

## Online Supplement

### Physiological Roles of the $K^+$ Current, $I_{Kr}$ , in Adult Mouse Heart Primary Pacemaker Activity

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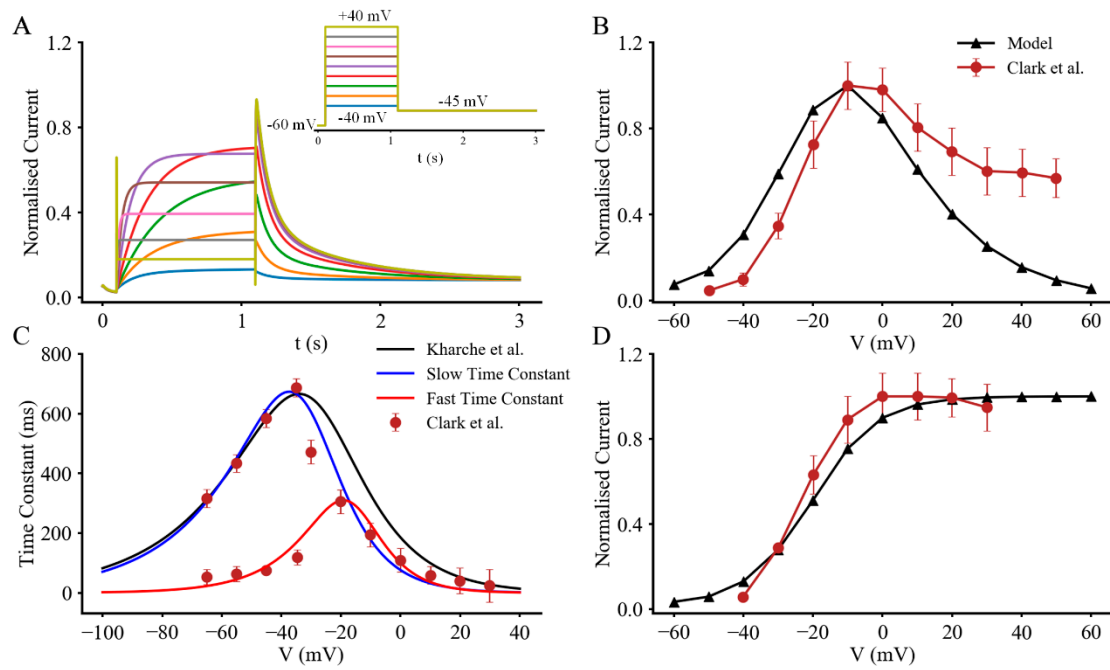
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#### 1. Updated $I_{Kr}$ equation and validation

To update the equations for the rapidly activating delayed rectifier  $K^+$  current,  $I_{Kr}$ , we modified the  $I_{Kr}$  formulations in our previously published Kharche et al. model [1] for mouse SAN myocyte action potentials. In the updated  $I_{Kr}$  model, the parameters for the steady-state voltage dependence of fast and slow activation variables ( $p_{a,f\infty}$ ,  $p_{a,s\infty}$ ), voltage-dependent time constants,  $\tau_{p,af}$  and  $\tau_{p,as}$ , the fractional ratio between the slow and fast components of  $K^+$  fluxes that generate the macroscopic  $I_{Kr}$  ( $f_v$ ), were derived by fitting the model equations to our previously published experimental data in Clark et al. [2]. During the model development and validation, the same voltage clamp protocol as used as was used in the experiments published by Clark et al. [2] was implemented to simulate  $I_{Kr}$  records (Figure S1A). These records were also used to obtain the I-V relationships for  $I_{Kr}$ . Measurements were made at the end of the test pulse (Figure S1B) for the isochronal I-V relationships; and at the peak of each tail current (panel D of Figure S1) to generate activation curve data.



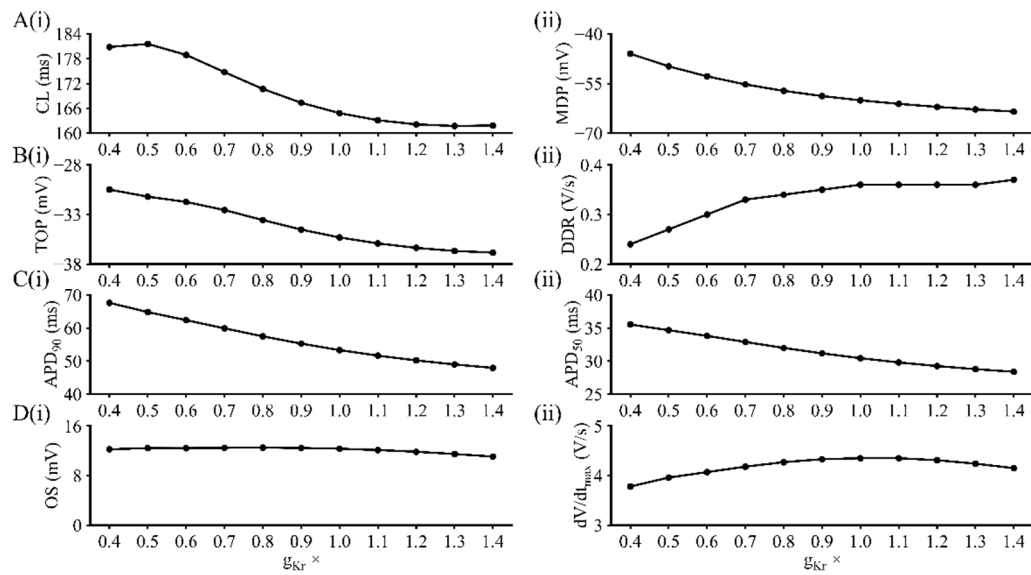
**Figure S1. Development and validation of the updated  $I_{Kr}$  model.**

(A) Simulated time traces of  $I_{Kr}$  during the voltage-clamp protocol as shown in the inset. (B) Simulated I-V relationship obtained at the end of testing potentials (black) are compared to experimental data of Clark et al. [2]. (C) Comparison between simulated slow (blue) and fast (red) time constants of the activation variable of the  $I_{Kr}$  model and experimental data of Clark et al. [2] (solid circles with error bars). The time constant of activation variable in original Kharche et al. [1] model is also shown for comparison (black). (D) Simulated activation curve obtained at the tail current (black) are compared to experimental data of Clark et al. [2].

Successful incorporation of the updated  $I_{Kr}$  formulations into the parent Kharche et al. model, required some additional relatively small changes in other model parameters. The L-type  $Ca^{2+}$  channel maximal conductance was reduced scale by a factor of 0.5; the T-type  $Ca^{2+}$  channel conductance was increased by a factor of 1.1; and the maximal electrogenic current generated by the  $Na^+-K^+$  pump was scaled by a factor 0.74. These changes were made to make it possible for the characteristics or biomarkers of the simulated pacemaker action potentials (e.g. pacemaking cycle length, maximal diastolic potential, AP overshoot and AP maximal upstroke velocity) generated by the updated model to closely approximate those from the original Kharche et al. model.

## 2. Modulation of pacemaker action potentials by $I_{Kr}$

In these simulations, the parameter  $g_{Kr}$  was modified or scaled in a range including: a 60% reduction, i.e., ( $g_{Kr} \times 0.4$ ) to a 40% increase i.e., ( $g_{Kr} \times 1.4$ ) as indicated by the labels on the abscissa on each panel in Figure S2. Note that changes in  $g_{Kr}$  in the range of (0.5 – 1.4), resulted in corresponding, monotonic increases in cycle length (CL) as shown in panel Ai of Figure S2. These changes were accompanied by a depolarized MDP (panel Aii in Figure S2); an increased threshold for firing or take off potential (TOP) (panel Bi in Figure S2); a reduced rate of the spontaneous pacemaker depolarization (DDR) (panel Bii in Figure S2); and increased AP durations measured at both APD<sub>90</sub> (panel Ci in Figure S2) and APD<sub>50</sub> (panel Cii in Figure S2). There was little if any change in the maximum depolarization or overshoot (OS) of the AP as shown in panel Di of Figure S2. However, a small bi-phasic change in the  $dV/dt_{max}$  was observed (panel Dii in Figure S2). In contrast, when  $g_{Kr}$  was reduced by more than 50%, the computed CL decreased progressively; in part, this was because the MDP moved in the depolarizing direction and thus was closer to the threshold for AP firing that is strongly dependent on two transient inward currents:  $I_{Na}$  and  $I_{CaL}$ .



**Figure S2. Summary of the effects of systematic scaling of the maximal conductance of  $I_{Kr}$ , ( $g_{Kr}$ ) on action potential descriptors**

Effect of a systematic scaling of the maximal channel conductance of  $I_{Kr}$  ( $g_{Kr}$ ) from a 60% reduction ( $g_{Kr} \times 0.4$ ) to 40% augmentation ( $g_{Kr} \times 1.4$ ) on the characteristics of the pacemaking action potentials. In the scaling range of (0.5 – 1.4), a decrease of  $g_{Kr}$  caused a monotonic increase of the CL, which is accompanied by an elevated MDP, increased TOP, reduced DDR, increased APD<sub>90</sub> and APD<sub>50</sub>, but unnoticed change in the OS, and a bi-phasic change in the  $dV/dt_{max}$ . When  $g_{Kr}$  is reduced more than 50% (i.e.,  $x < 0.5$ ), the computed CL starts to decrease as the MDP is getting closer to the TOP. (Ai) CL; (Aii): MDP; (Bi) TOP; (Bii) DDR; (Ci) APD<sub>90</sub>; (Cii) APD<sub>50</sub>; (Di) OS; and (Dii)  $dV/dt_{max}$ .

## References

1. Kharche, S.; Yu, J.; Lei, M.; Zhang, H., A mathematical model of action potentials of mouse sinoatrial node cells with molecular bases. American Journal of Physiology-Heart and circulatory physiology 2011, 301, (3), H945-H963.
2. Clark, R. B.; Mangoni, M. E.; Lueger, A.; Couette, B.; Nargeot, J.; Giles, W. R., A rapidly activating delayed rectifier K<sup>+</sup> current regulates pacemaker activity in adult mouse sinoatrial node cells. American Journal of Physiology-Heart and Circulatory Physiology 2004, 286, (5), H1757-H1766.