

Article

Pyrophosphate-Enhanced Oxidase Activity of Cerium Oxide Nanoparticles for Colorimetric Detection of Nucleic Acids

Seokhwan Kim 1,†, Jinjoo Han 1,†, Heeseok Chung ¹ , Yong-Keun Choi ¹ [,](https://orcid.org/0000-0002-4535-8044) Ayemeh Bagheri Hashkavayi ¹ , Yu Zhou 2,* and Ki Soo Park 1,[*](https://orcid.org/0000-0002-0545-0970)

- ¹ Department of Biological Engineering, Konkuk University, Seoul 05029, Korea; mmm1605@konkuk.ac.kr (S.K.); jinjoo9665@konkuk.ac.kr (J.H.); jhs2562@konkuk.ac.kr (H.C.); dragonrt@konkuk.ac.kr (Y.-K.C.); elnazbagheri@konkuk.ac.kr (A.B.H.)
- ² College of Animal Sciences, Yangtze University, Jingzhou 434023, China
- ***** Correspondence: zhouyurunye@sina.com (Y.Z.); akdong486@konkuk.ac.kr (K.S.P.)
- † These authors contributed equally to this work.

Abstract: In recent years, cerium oxide (CeO²) nanoparticles (NPs) have drawn significant attention owing to their intrinsic enzyme mimetic properties, which make them powerful tools for biomolecular detection. In this work, we evaluated the effect of pyrophosphate (PPi) on the oxidase activity of $CeO₂$ NPs. The presence of PPi was found to enhance the oxidase activity of $CeO₂$ NPs, with enhanced colorimetric signals. This particular effect was then used for the colorimetric detection of target nucleic acids. Overall, the PPi-enhanced colorimetric signals of $CeO₂$ NPs oxidase activity were suppressed by the presence of the target nucleic acids. Compared with previous studies using CeO² NPs only, our proposed system significantly improved the signal change (ca. 200%), leading to more sensitive and reproducible colorimetric analysis of target nucleic acids. As a proof-ofconcept study, the proposed system was successfully applied to the highly selective and sensitive detection of polymerase chain reaction products derived from *Klebsiella pneumoniae.* Our findings will benefit the rapid detection of nucleic acid biomarkers (e.g., pathogenic bacterial DNA or RNA) in point-of-care settings.

Keywords: cerium oxide; colorimetry; nucleic acid; oxidase activity; pyrophosphate

1. Introduction

Fast, robust, and ultrasensitive detection of target nucleic acids has important applications in molecular diagnostics for the detection of pathogens and viruses [\[1](#page-7-0)[,2\]](#page-7-1). The gold standard for the detection of specific nucleic acid involves the exponential amplification of a target DNA fragment using polymerase chain reaction (PCR) followed by gel electrophoresis [\[3\]](#page-7-2). However, gel-based assay is not only time consuming but also requires user expertise. In recent years, real-time PCR, which can amplify DNA in real time, has been widely utilized as a promising alternative [\[4,](#page-7-3)[5\]](#page-7-4). However, despite its high accuracy, real-time PCR requires expensive reagents (fluorescence-labeled probes or DNA binding dyes) and bulky equipment. These shortcomings become more problematic for point-of-care testing (POCT) applications [\[6\]](#page-7-5).

In this regard, colorimetric strategies, whose results can be identified even with the naked eye, are a good option for POCT applications or facility-limited settings. Several assays are available for the rapid and sensitive colorimetric detection of target nucleic acids and other various target biomolecules [\[7\]](#page-7-6). The representative examples rely on metal nanomaterials (gold [\[8](#page-7-7)[–12\]](#page-7-8) and silver [\[13](#page-7-9)[–15\]](#page-7-10)) that exhibit distinct, size-dependent color changes and enzyme-mimicking activities. For example, the peroxidase-mimicking activity of magnetic nanoparticles (Fe₃O₄ NPs) [\[16\]](#page-7-11) and the oxidase-mimicking activity of cerium oxide nanoparticles ($CeO₂$ NPs) [\[17,](#page-7-12)[18\]](#page-7-13) catalyze the conversion of transparent substrates (e.g., 3,3',5,5'-tetramethylbenzidine [TMB]) into colorimetric products. These catalytic

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reactions are suppressed by the presence of the target nucleic acids, thus leading to the development of facile colorimetric assay. These procedures are simple, and their results can be quickly analyzed without the need for expensive instruments. However, in the case of AuNPs, several factors (e.g., salt) can cause AuNPs to aggregate regardless of the presence of target nucleic acids, leading to unexpected false-positive or false-negative results [\[19\]](#page-7-14). In the case of Fe₃O₄ NPs, it requires a relatively long reaction time (ca. 30–90 min) [\[16,](#page-7-11)[20,](#page-7-15)[21\]](#page-7-16) to generate the colorimetric signal and there are hydrogen peroxide (H_2O_2)-related toxicity issues [\[21,](#page-7-16)[22\]](#page-8-0). Furthermore, the signal change caused by the presence of target nucleic acids is not strong enough to achieve reproducible results. On the other hand, CeO_2 NPs with oxidase activity effectively catalyze the colorimetric reaction within a few minutes and do not involve H_2O_2 [\[23\]](#page-8-1), which is more desirable for POCT application.

In the current study, we aimed to devise an advanced method to enhance the colori-In the current study, we aimed to devise an advanced method to enhance the colorimetric signal change caused by CeO² NPs by improving their oxidase-mimicking activity. metric signal change caused by CeO2 NPs by improving their oxidase-mimicking activity. Specifically, we evaluated PPi as an effective enhancer molecule of CeO₂ NP-catalyzed oxidation reactions in an effort to amplify the signal changes caused by the presence of target nucleic acids. We then developed the colorimetric system for the detection of target target nucleic acids. We then developed the colorimetric system for the detection of target nucleic acids. As described in Figur[e 1](#page-1-0)a, when negatively charged nucleic acids are present, it binds to the positively charged $CeO₂$ NPs through electrostatic interaction, reducing the effective surface area for the interaction with PPi and TMB substrate. As a result, the the effective surface area for the interaction with PPi and TMB substrate. As a result, the sample with target nucleic acids exhibits a suppressed colorimetric signal as compared with the one without target nucleic acids. Importantly, $CeO₂$ NPs that are known to possess phosphatase-like activity as well [\[24](#page-8-2)[–26\]](#page-8-3) can release energy by hydrolyzing phosphate ester bonds in PPi, which thereby can contribute to the enhancement of colorimetric signal change (Figure 1b) [\[27\]](#page-8-4). In the effort described below, we successfully determined the target nucleic acids originated from *Klebsiella pneumoniae* with high selectivity. Results from the study may benefit the development of a molecular diagnostic system that can be used in POCT settings.

Figure 1. (a) Schematic illustration of the proposed CeO₂ NPs-based colorimetric detection of target DNA using pyrophosphate (PPi) as an enhancer. (b) Reaction mechanism for the hydrolysis of phosphate ester bonds in PPi by CeO₂ NPs.

2. Materials and Methods 2. Materials and Methods

2.1. Reagents 2.1. Reagents

Cerium (IV) oxide nanoparticles (CeO₂ NPs) were purchased from Sigma-Aldrich (St. Louis, MO, USA). Sodium acetate, sodium phosphate, and sodium pyrophosphate were purchased from Samchun Chemical (Seoul, Korea); SYBR Green II and TMB were purchased from Thermo Fisher Scientific (Waltham, MA, USA). Deoxynucleoside triphosphate (dNTPs) and ribonucleoside triphosphate (rNTPs) were purchased from Enzynomics (Seoul, Korea). All DNA oligonucleotides were synthesized by Integrated DNA Technologies (Coralville, IA, USA). Ultrapure DNase/RNase-free distilled water from Bioneer (Daejeon, Korea) was used in all experiments. All chemicals used in this study were of analytical grade.

2.2. Confirmation of DNA Binding to CeO² NP by Fluorescence Microscope

20 µL of 10 µM synthetic DNA (5'-AGT TCG AGCAGC AAG CTA TAT TTC CTT AAC AA-3', 32 nt) were added to 2.7 μ L of a CeO₂ NP stock solution (2.5 wt.% colloidal dispersion in 0.4 M sodium acetate buffer), and to this solution, 22.3 μ L of 0.4 M sodium acetate buffer (pH 3.7) and 41 μ L of deionized water were added. After incubation for 5 min , $4 \mu L$ of 10 mM PPi was added and incubated for 30 min. Finally, images were obtained using fluorescence microscopy (KI-2000F; Korea Lab Tech, Gyeonggi-do, Korea) with filter cube (excitation: 450–480 nm; barrier: 515 nm) after adding 10 μ L of 10 \times SYBR Green II, a staining dye specific for single-stranded DNA.

2.3. Bacteria Cultivation and Genomic DNA Isolation

Klebsiella pneumoniae (ATCC 700603), *Pseudomonas aeruginosa* (ATCC 27853), *Escherichia coli* (ATCC 25922), and *Enterobacter cloacae* (KCTC 2519) were grown in Luria-Bertani (LB) medium (BD, Franklin Lakes, NJ, USA) at 37 ◦C with constant shaking for 18–20 h. After the cultures were centrifuged at $5000 \times g$ for 5 min, the supernatant was carefully discarded, and the cell pellet was resuspended in 200 μ L of the TCL buffer supplied with the Total DNA Extraction S&V Kit (Bionics, Seoul, Korea). The cells were then lysed by mixing with Proteinase K and heating for 1 h at 56 °C. Finally, genomic DNA (gDNA) was isolated according to the instructions of the gDNA extraction kit. The purity and concentration of the extracted gDNA were evaluated using a Nanodrop Spectrometer (Spectramax iD5 multi-mode microplate reader; Molecular Devices, San Jose, CA, USA) prior to storage of the gDNA at -20 °C until use.

2.4. PCR Amplification

Bacterial gDNA was amplified by PCR. The total reaction solution of 20 μ L that contained 1 µL of bacterial gDNA, 0.5 µM of each primer, and 10 µL Topreal qRCR $2\times$ PreMIX (SYBR Green with low ROX) (Enzynomics, Daejeon, Korea), was heat-denatured at 95 °C for 10 min, followed by 25 cycles of 95 °C for 20 s, 64 °C for 30 s, and 72 °C for 60 s. For the specific amplification of *K. pneumoniae*, *wabG* gene (GenBank accession number KX842082) was targeted, and the following primers were used for PCR amplification: forward, 5'-ACC ATC GGC CAT TTG ATA GA-3' and reverse, 5'-CGG ACT GGC AGA TCC ATA TC-3'. After amplification, the PCR products were purified with NucleoSpin Gel & PCR Clean-up kit (Takara Bio, Kusatsu, Japan) according to the manufacturer's protocol. The length and concentration of the PCR products were determined by agarose gel electrophoresis and Nanodrop Spectrometer (Spectramax iD5 multi-mode; Molecular Devices), respectively.

2.5. CeO² NP-Based Colorimetric Detection Using PPi as an Enhancer

First, 20 µL of 10 µM synthetic DNA, PCR products or gDNA at different concentrations were added to 2.7 μ L of a CeO₂ NP stock solution (2.5 wt.% colloidal dispersion in 0.4 M sodium acetate buffer), and to this solution, 22.3 μ L of 0.4 M sodium acetate buffer (pH 3.7) and 1 μ L of deionized water were added. After incubation for 5 min, to the solution was added 50 μ L of 1 \times TMB substrate solution and 4 μ L of 10 mM PPi, which was then incubated for 30 min to develop the colorimetric signal. Not only PPi, but also other substances such as dNTP and rNTPs $(4 \mu L, 10 \text{ mM})$ were tested to evaluate their enhancement effect on the $CeO₂$ NP-catalyzed oxidation reactions. After centrifugation at 5900 \times *g* for 30 s to separate CeO₂ NPs from the reaction solution, the colorimetric signal

of the supernatant was measured at a wavelength of 650 nm using a microplate reader (Spectramax iD5 multi-mode; Molecular Devices).

3. Results and Discussion charged CeO2 NPs more effectively than dNTP and rNTP. In addition, the energy released

3.1. Selection of the Best Enhancer for CeO₂ NPs Oxidase Activity

First, we investigated the effect of phosphate ester bonds using different substances, such as dNTP, rNTP, and PPi, on the oxidase activity of CeO $_2$ NPs during a CeO $_2$ NPscatalyzed oxidation reaction. As shown in Figure 2a, PPi substantially increased the catalytic activity of CeO₂ NPs and induced the highest signal change in the presence of nucleic acids. We assumed that PPi without sugar and bases can interact with the positively charged CeO $_2$ NPs more effectively than dNTP and rNTP. In addition, the energy released after PPi is cleaved by CeO₂ NPs boosted the oxidase activity of CeO₂ NPs, resulting in substantial colorimetric signal change.

Figure 2. Selection of the best enhancer for CeO₂ NPs oxidase activity. (a) Relative signal change (%) of dNTPs (0.4 mM), rNTPs (0.4 mM), and PPi (0.4 mM). Relative signal change (%) was calculated of dNTPs (0.4 mM), rNTPs (0.4 mM), and PPi (0.4 mM). Relative signal change (%) was calculated as the DNA-induced signal change in the presence of dNTPs and rNTPs divided by that in the presence ence of PPi and multiplied by 100 (%). (**b**) Absorbance signal at 650 nm (A650) in the absence (−) and of PPi and multiplied by 100 (%). (**b**) Absorbance signal at 650 nm (A₆₅₀) in the absence (−) and presence (+) of PPi (0.4 mM). Black and gray bars indicate the absence and presence of synthetic DNA, respectively.

3.2. Confirmation of DNA Binding to CeO2 NPs and Reaction Optimization DNA. Figure [2b](#page-3-0) shows that the presence of DNA suppressed the oxidase activity of CeO₂ NPs , as evidenced by the low colorimetric signal at 650 nm, the maximum absorbance of oxidized TMB, regardless of the presence or absence of PPi. In contrast, the oxidase activity of CeO_2 NPs in the absence of DNA was increased by the presence of PPi, thereby increasing the signal difference between reactions with and without DNA. Taken together, Next, using PPi as the best enhancer, we evaluated the detection feasibility of target these results indicate that PPi is the key factor for the enhanced signal change in the presence of DNA.

3.2. Confirmation of DNA Binding to CeO² NPs and Reaction Optimization

As shown in Figure [1,](#page-1-0) the binding between the DNA and $CeO₂$ NPs was assumed to drive the suppression of catalytic activity of $CeO₂$ NPs. To confirm this, we investigated the adsorption of DNA onto $CeO₂$ NPs using fluorescence microscopy after preparing the samples containing $CeO₂$ NPs, DNA, and SYBR Green II, a staining dye specific for single-stranded DNA. Figure [3](#page-4-0) shows that $CeO₂$ NPs displayed a high fluorescence signal when the DNA was present with $CeO₂$ NPs, whereas a negligible fluorescence signal was observed when the DNA was absent. This clearly confirms that the DNA binds to $CeO₂$ NPs to inhibit the catalytic reaction of $CeO₂$ NPs. We also optimized the reaction conditions, including the concentrations of $CeO₂$ NPs and PPi, for the efficient analysis of DNA by comparing the absorbance signals in the absence and presence of [DN](#page-4-1)A. Figure 4 shows that 0.07 wt.% of $CeO₂$ NPs and 0.4 mM of PPi were ideal to achieve the highest signal $\frac{1}{2}$ change, which were thus used for further experiments. \overline{C}

Figure 3. Fluorescence microscope images obtained in the presence (a) and absence (b) of DNA. Optical images, (2) fluorescent images, (3) merged images. (1) Optical images, (2) fluorescent images, (3) merged images. Optical images, (2) fluorescent images, (3) merged images.

Figure 4. Optimization of the proposed colorimetric system. (a) $CeO₂$ NP concentration. (b) PPi concentration. Change in absorbance signal (ΔA_{650}) was calculated by subtracting A_{650} in the presence of DNA from that in the absence of DNA.

3.3. Analytical Performance of the Proposed System 3.3. Analytical Performance of the Proposed System 3.3. Analytical Performance of the Proposed System

Under the optimized conditions, we demonstrated the detection feasibility of target nucleic acids originating from pathogenic bacteria. As proof of concept, we selected present using the target pathogen and designed the specific primers by targeting wables and ℓ K. pneumoniae as the target pathogen and designed the specific primers by targeting wabG shown in Figure 5a, gDNA extracted from *K. pneumoniae* generated a PCR product with a shown in Figure [5a](#page-5-0), gDNA extracted from *K. pneumoniae* generated a PCR product with a
since 6.683 has welt these adiations title of from that formed in the change of cDNA. Next *K. pneumoniae*. First, we verified the PCR amplification with the designed primers. As in *K. pneumoniae*. First, we verified the PCR amplification with the designed primers. As size of 683 bp, which was distinguished from that formed in the absence of gDNA. Next, we detected the PCR product using the proposed colorimetric system, which was compared to its counterpart without using PPi. Figure [5b](#page-5-0) shows that the presence of the PCR product suppressed the colorimetric signal both without and with PPi; however, signal change (ΔA_{650}) was more evident in the presence of PPi. These results were consistent with those using a synthetic target DNA (Figure [2b](#page-3-0)), demonstrating that our proposed system with PPi as enhancer is more suitable for the sensitive and selective colorimetric detection of target nucleic acids. of target nucleic acids. change (\overline{X} 650) was more evident in the presence of PPI. The presence of PPI. These results with with with with with with with \overline{X} those using a symmetric target DNA (Figure 2b), demonstrating that our proposed system whi

pared to its counterpart without using PPi. Figure 5b shows that the presence of the PCR

Figure 5. Detection of PCR products from *K. pneumoniae*. (a) PCR amplification curves in the absence (black) and presence (red) of gDNA from *K. pneumoniae* $(1.6 \times 10^3 \text{ copies/}\mu\text{L})$. Inset shows the corresponding gel electrophoresis results. Lanes 1 and 2 indicate the samples obtained after PCR in the absence and presence of gDNA, respectively. RFU: relative fluorescence unit. (**b**) ∆A₆₅₀ in $s = \frac{1}{4}$ and presence (and presence of $\frac{1}{4}$) of PPi. Change in a boundary subtraction by subtraction $\frac{1}{4}$ and $\frac{1}{4}$ the absence (−) and presence (+) of PPi. Change in absorbance signal (ΔA_{650}) was calculated by subtracting A_{650} in the presence of target DNA from that in the absence of target DNA.

Next, we evaluated the selectivity and sensitivity of the proposed detection system. Next, we evaluated the selectivity and sensitivity of the proposed detection system. Because the primers were designed specifically for *K. pneumoniae*, the highest signal Because the primers were designed specifically for *K. pneumoniae*, the highest signal change change (ΔA650) was obtained only in the presence of *K. pneumoniae*, whereas the presence (∆A650) was obtained only in the presence of *K. pneumoniae*, whereas the presence of other car 650) was obtained only in the presence of *n*: *predimendal*, whereas the presence of other
control bacteria, including *Pseudomonas aeruginosa*, *Escherichia coli*, and *Enterobacter cloacae*, *ter cloacae*, did not generate any PCR product and exhibited a negligible signal change, did not generate any PCR product and exhibited a negligible signal change, indicating the and not generate any 1 EX product and exhibited a negagible signal enarge, matedanity are high specificity of the proposed system (Figure [6a](#page-6-0)). In addition, we measured the colori-metric signal in the presence of PCR products at different concentrations. Figure [6b](#page-6-0) shows metric signal in the presence of PCR products at different concentrations. Figure 6b shows that as the concentration of PCR products increased, the colorimetric signal decreased with that as the concentration of PCR products increased, the colorimetric signal decreased with a limit of detection (LOD) of 1.04 nM (3σ/S, where σ and S are the standard deviation of standard deviation of the blank and the slope). It should be noted that the LOD obtained the blank and the slope). It should be noted that the LOD obtained in this assay is good in this assay is good enough to be used in various areas for the detection of pathogens and enough to be used in various areas for the detection of pathogens and viruses because viruses because the general concentration of PCR products ranges from 10 to 100 nM [28]. the general concentration of PCR products ranges from 10 to 100 nM [\[28\]](#page-8-5). Furthermore, Furthermore, the proposed system was applied to the detection of extracted gDNA from the proposed system was applied to the detection of extracted gDNA from *K. pneumoniae*. *K. pneumoniae*. The results in Figure 7 show that the presence of gDNA led to the signal The results in Figure [7](#page-6-1) show that the presence of gDNA led to the signal change (∆A650), change (α 650), proving the direction feasibility of extracted gDNA extra suither the direction feasibility of extracted gDNA extra suither the formulation in proving the direct detection feasibility of extracted gDNA even without PCR amplification.

Figure 6. Detection selectivity (a) and sensitivity (b,c) of the proposed system. (a) Change in absorbance signal (ΔA_{650}) was calculated by subtracting A_{650} in the presence of target DNA from that in the absence of target DNA. Inset shows a photographic image of each sample containing PCR products. 1: the absence of target DNA; 2: Pseudomonas aeruginosa; 3: Enterobacter cloacae; 4: Escherichia coli; 5: Klebsiella pneumoniae. (b) Absorbance spectra in the presence of PCR products concentrations and images of a control sample without PCR products and a sample contained by the products. (*c*) at different concentrations and images of a control sample without PCR products and a sample containing 40 nM PCR products. (**c**) Linear relationship between ΔA₆₅₀ and PCR concentration (2.5–40 nM). probacter clouds of each sample collision of Products. The products at different in the products at different products at different in the products at different in the products at different in the products at different in

Figure 7. Direct detection of gDNA extracted from Klebsiella pneumoniae. (a) Absorbance spectra and (b) ΔA_{650} in the presence of extracted gDNA at different concentrations. Change in absorbance signal (ΔA_{650}) was calculated by subtracting A_{650} in the presence of extracted gDNA from that in the absence of extracted gDNA. p value is indicated by stars, **** $p < 0.0001$. Inset shows a photographic image of each sample containing extracted gDNAs at different concentrations.

4. Conclusions 4. Conclusions 4. Conclusions

We developed a simple, colorimetric assay for the detection of target nucleic acids $\frac{1}{2}$ the oxidase activity of CCO₂ NPs and PPI as an enhancer to improve the oxidase activity of CeO_2 NPs, leading to more evident colorimetric signal change. Using the proposed posed system, PCR products from the pathogenic bacteria, *K. pneumoniae,* were quantita t_{max} and σ_{max} and σ_{max} is addition, in addition, it can directly analyze gDNA extracted with σ_{max} $\frac{1}{2}$ to the continue that the may pave the way for the way for the reproduction of the reproduction of $\frac{1}{2}$ methods, such as isothermal nucleic acid amplification. Overall, our proposed system methods, such as isothermal nucleic acid amplification. Overall, our proposed system system provides rapid colorine rapid coloring rapid coloring PCT and continuous the need for a complication and expenditure in PCT and in PCT and in the need for and for and for a complication of PCT and PCT and PCT instrument and can thus be used in POCT applications and facility-limited settings. using the oxidase activity of CeO_2 NPs and PPi as an enhancer to improve the oxidase acsystem, PCR products from the pathogenic bacteria, *K. pneumoniae*, were quantitatively analyzed with high selectivity. In addition, it can directly analyze gDNA extracted from target bacteria. Our findings may pave the way for the reproducible detection of various target molecules and can be used in combination with various nucleic acid amplification
target molecules and can be used much is said amplification. Organization and can be used with provides rapid colorimetric results without the need for a complicated and expensive
instrument and see thus has used in POCT explications and facility limited esttings.

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