



Article

Strength Decrease, Perceived Physical Exertion and Endurance Time for Backpacking Tasks

Kai Way Li ^{1,*}, Jenn Chun Chu ² and Ching Chung Chen ³

¹ Department of Industrial Management, Chung Hua University, Hsinchu 30012, Taiwan

² Ph.D. Program of Technology Management, Chung Hua University, Hsin-Chu 30012, Taiwan; d1043003@gmail.com

³ Department of Information Management, Hsing Wu University of Science & Technology, New Taipei 24452, Taiwan; 095165@mail.hwu.edu.tw

* Correspondence: kai@chu.edu.tw; Tel.: +886-3-5186583; Fax: +886-3-5186575

Received: 1 March 2019; Accepted: 9 April 2019; Published: 11 April 2019



Abstract: Manual material handling (MMH) tasks create a burden for workers which could result in musculoskeletal injuries. Assessments of the decrease of muscular strength and the maximum endurance time (MET) for MMH tasks are essential in studying the ergonomic risk of MMH tasks. A backpacking experiment was conducted for measuring the MET for MMH tasks. Human participants carried a load on their back and walked on a treadmill under various load, walking speed, and ramp angle conditions until they could no longer do so. It was found that the participants were able to walk for approximately 15 min to two hours before they needed to have a pause. Their back and leg strengths declined moderately due to performing the tasks. These tasks resulted in an increase in heart rate and elevated perceived physical exertion. The rating of perceived exertion (RPE)/heart rate ratio in our backpacking tasks was 31% higher than that in the literature, implying the calibration of the RPE may be required for such tasks. A MET model incorporating the f_{MVC_back} , body weight, walking speed, and ramp angle was established. This model may be used to determine the work/rest allowance for backpacking tasks under conditions similar to this study.

Keywords: manual material handling; manual operation; muscular fatigue; maximum endurance time

1. Introduction

Body pain and discomfort due to undesirable conditions such as overexertion and unnatural postures are common at work. Based on labor insurance claim data, reported injuries in the neck, shoulder, and upper extremity of workers in Taiwan increased 5.2 times in a twelve-year period (2001–2013), while lower back injuries increased 1.7 times [1]. These musculoskeletal disorders have resulted in a huge burden to both workers and the society. Due to the widespread problems of musculoskeletal disorders, the government in Taiwan stated in 2013, in the Occupational Safety & Health Act that it is the responsibility of the employers to prevent the occurrence of these occupational injuries. Investigations of issues related to musculoskeletal injury are, therefore, urgent for maintaining a safe and healthy work environment [2].

Manual material handling (MMH) tasks are major contributors of musculoskeletal injuries in workplaces [3–5]. Determining the physical capability for workers is essential to the design of MMH tasks such as lifting, pushing, pulling, and carrying [6,7]. Physical capability may be determined by checking the muscular strength for a certain body segment or for a composite measure involving several body segments. Muscular strength decreases after the muscles have contracted for a period of time, resulting in the onset of muscular fatigue.

Muscular fatigue is a common phenomenon for physical activities. It may be defined as the reduction in the ability to exert muscle force or power [8–11], failure to maintain the required or expected force [12], or failure to continue working at a given exercise intensity [13]. Muscular fatigue may be assessed by measuring the reduction of maximum voluntary contraction (MVC) after performing a forceful exertion for a period of time [14]. The reduction of the MVC, or alternatively force or strength decrease, may be quantified. A certain mathematic function may be fitted as a model describing the developing of muscular fatigue [15]. Following such an approach, muscular fatigue models have been established for various task conditions [16–18].

Ma et al. [14] suggested that a fatigue rate (k) for an individual or for a certain population should be incorporated when predicting the progress of muscular fatigue. The reciprocal of this parameter, or $1/k$, was termed fatigue resistance [19]. Zhang et al. [20] assessed muscular fatigue for workers performing single arm push tasks and found that males had significantly ($p < 0.0001$) higher k than female participants. Muscular decrease models incorporating the concept of fatigue rate have also been employed in both one- and two-handed carrying tasks [21,22].

In addition to the study of muscular strength, assessment and modeling of maximum endurance time (MET) have also been beneficial to studying muscular fatigue. The MET represents the maximum time during which a static muscular load can be maintained [23]. It has been used in job assessment, especially to determine the acceptable duration of maintaining a static muscular contraction [24]. Establishment of MET models has been reported [14,19,25–33]. Model development involves establishing a mathematical function with the %MVC, or alternatively the relative force ($f_{MVC} = \%MVC/100$), as independent variable [23,34–37].

Most MET models in the literature were developed for static contractions. However, most tasks involving static contractions for certain body segments in industry are accompanied by dynamic or cyclic activities of other body parts. Li et al. [35] conducted a one-handed carrying study and established MET models considering body weight, walking speed, and f_{MVC} . Their results indicated that both body weight and walking speed were important parameters in predicting the MET when walking was considered, especially when the f_{MVC} was 0.3 or lower.

Muscular fatigue issues for one- and two-handed carrying tasks have been discussed [21,22,35]. Backpacking is also a common manual material handling tasks, being performed, for example, by school students [38], firefighters, polices, and military personnel [39]. Theoretically, backpacking tasks involve static muscular contraction on the trunk and cyclic activities on the lower extremities. It has been hypothesized that backpacking tasks result in a decrease in muscular strength on the back and the leg due to muscular fatigue. These muscular strength decreases are believed to be associated with elevated physiological and psychophysical indices such as heart rate and subjective rating of muscular strength. The objectives of this study were to test these hypotheses. The effects of task factors such as walking speed, load carried, and ramp angle of the walk on the heart rate, decrease of muscular strength, rating of perceived exertion, and the MET for backpacking tasks were also tested. In addition, a predictive MET model incorporating walking conditions is established and discussed.

2. Methods

A carrying experiment was performed in a laboratory. The temperature and relative humidity were $21.1 (\pm 2.4) ^\circ\text{C}$ and $65.1 (\pm 9.7)\%$, respectively.

2.1. Human Participants

A total of 16 adults (10 males and 6 females) participated in the experiment. The participants were healthy without self-reported history of musculoskeletal disorders within a year. Their age, stature, and body weight (BW) were $21.7 (\pm 2.6)$ years, $169.5 (\pm 5.6)$ cm, and $63.0 (\pm 11.4)$ kg, respectively. Signed informed consent was obtained from every participant before participating in the study. The participants were compensated 150 NTD per hour for their participation in the experiment.

This study has been reviewed and approved by an external IRB (National Tsing Hua University, 10607EE061).

2.2. Apparatus

A treadmill which allows adjustment of inclination was used. In addition, an isometric strength measurement unit was adopted. This unit contains a platform, a chain with a handle, and a loadcell. It allows measurements of isometric back strength and isometric leg strength. This unit had been adopted in previous studies [21,22]. A Borg rating of perceived exertion (RPE) scale (6–20) was prepared to measure the perceived physical exertion of the body after a backpacking trial [40,41]. A backpack allowing to be carried with both shoulders was also prepared. The sizes of the backpack were 41 cm × 33 cm × 14 cm. The width and thickness of the shoulder straps were 7.5 cm and 0.5 cm, respectively.

2.3. Experimental Conditions

2.3.1. Load Carried

Carrying a load weighing 25% of their BW is common for firefighters, police officers in special missions [39], and even for school children [38]. Three load levels were tested: 0%, 12.5%, and 25% of BW. The load in the experiment was comprised with steel blocks. The load was in the backpack prepared. The participants carried the backpack on both shoulders during the trial.

2.3.2. Walking Speed

Three walking speeds were tested, including 2 km/h, 4 km/h, and 6 km/h. The walking speed was controlled by the settings on the treadmill.

2.3.3. Ramp Angle

The inclination of the treadmill can be adjusted. Two levels of treadmill inclination were tested. The first one was flat or a 0° ramp angle condition. The second was a 10° uphill condition.

2.4. Procedure

Before the trial, the isometric back, and leg strengths were measured. For these measurements, the participant stood on a platform and pulled a handle connected to the platform upward. A loadcell was hooked between the handle and the platform to measure the force. The participant applied his/her maximum force for 4 to 6 seconds. The peak force was displayed and recorded. For isometric back strength, the participant stood and bent his/her waist to grasp the handle 38 cm above the platform and pulled upward with maximum force (see Figure 1). This force was the maximum voluntary contraction of the back muscles or MVC_{back} . For the isometric leg strength, the participant bent his/her knee with upper body straight to grasp the handle 38 cm above the platform and pulled upward with maximum force. This force was the MVC_{leg} . The procedure performing these strengths measurements followed those in Ayoub and Mital [42]. The participant took a break for at least five minutes after taking a strength measurement so as to avoid the effects of muscular fatigue on the next measurement.

In the experiment, the participant was requested to carry a backpack with a predetermined weight and walk on the treadmill under a predetermined ramp angle and walking speed (see Figure 2). The order of the weight carried, ramp angle, and walking speed was randomly arranged in advance. The participant kept on walking until he or she could not walk any longer. Drinking and listening to music were not allowed during the trial. The heart rates of the participant before (HR_b) and immediately after the walk (HR_a) were recorded. The time of walking was recorded as the maximum endurance time (MET). After the walk, the participant's RPE was immediately recorded. He or she then unloaded the backpack and was tested for his/her isometric back and leg strengths. These back

and leg strengths were termed MVC_{backa} and MVC_{lega} , respectively. The participant joined the test only once per day to avoid the effects of fatigue.



Figure 1. Measurement of isometric back strength.



Figure 2. Walking with a backpack on a treadmill.

2.5. MET Modeling

Backpacking tasks involve both load carrying and walking. Load carrying on the back requires static contraction mainly on the back. Walking, on the other hand, involves dynamic contractions especially on the lower limbs. For static muscular contraction, the MET is dependent on the f_{MVC} [14,31,36,37]. For walking, task factors which contribute to physical burdens should be incorporated. Both BW and walking speed were found to be major factors affecting energy expenditure required for walking [43–45]. They should be incorporated into the MET models for backpacking tasks. In addition, walking uphill requires more physical energy than walking on a level surface. Ramp angle should also be included. The MET may, then, be represented as a function of f_{MVC} , BW, walking speed, and ramp angle:

$$MET = F(f_{MVC}, BW, v, \theta) \quad (1)$$

where v is walking speed (km/h) and θ is ramp angle (degree).

Both power and exponential functions have been proposed in MET modeling [19,23,28,36,37,46,47]. Body weight and walking speed were reported to have multiplication effects on the increment of energy expenditure for walking [45]. Equation (1) may be formulated adopting an exponential function of f_{MVC} considering ramp angle and multiplicative effects of BW and walking speed, as in Equation (2):

$$MET = e^{\beta_1 f_{MVC_back}} \times BW^{\beta_2} \times \beta_3^v \times (\cos\theta)^{\beta_4} \quad (2)$$

where f_{MVC_back} is the f_{MVC} on back muscles; β_1 , β_2 , β_3 , and β_4 are coefficients to be determined.

Equation (2) may be converted to a linear equation by taking natural logarithm on both sides:

$$\ln(MET) = \beta_1 f_{MVC_back} + \beta_2 \ln(BW) + \ln(\beta_3)v + \beta_4 \ln(\cos\theta) \quad (3)$$

2.6. Experiment Design and Data Analysis

There was a total of 288 trials (16 participants \times 2 inclined angles \times 3 walking speeds \times 3 load conditions). The f_{MVC_back} was calculated by dividing the weight carried by the MVC_{back} . The following equations were adopted to calculate the decline (%) of isometric back and leg strengths:

$$\text{Back strength decline (\%)} = (MVC_{back} - MVC_{backa}) / MVC_{back} \times 100\% \quad (4)$$

$$\text{Leg strength decline (\%)} = (MVC_{leg} - MVC_{lega}) / MVC_{leg} \times 100\% \quad (5)$$

Descriptive statistics and analyses of variance (ANOVA) were performed for the HR_a , MET, RPE, and declines of both back and leg strengths. Regression analysis was performed to determine the regression coefficients in Equation (3). The statistical analyses were performed using the SAS 9.4 software (SAS Institute Inc., Cary, NC, USA).

3. Results

3.1. Descriptive Statistics

Walking and carrying depletes our energy. Theoretically, the energy expenditure for such an activity results in increase of heart rate and decrease of muscular strength. Sixteen participants joined our backpacking experiment. Their anthropometric characteristics are shown in Table 1. Our results indicated that the heart rate of the participants increased 9.1% to 62.7% depending on the weight carried, walking speed, and ramp angle. The HR_b and HR_a were 85.5 (± 10.3) bpm and 112.3 (± 21.1) bpm, respectively. The difference between these two was statistically significant ($p < 0.0001$). This corresponds to an increase of 26.8 bpm on average. Figure 3 shows the heart rate after trial under the experimental conditions.

Table 1. Anthropometric characteristics of the participants.

Basic Characteristics	Male (n = 10)	Female (n = 6)
Age (years)	21.3 (1.7)	22.3 (3.4)
Stature (cm)	172.5 (5.3)	166.8 (3.8)
Body weight (kg)	67.4 (11.8)	55.7 (3.3)
Heart rate at rest (bpm)	82.5 (10.4)	90.5 (8.0)
Isometric leg strength (kgf)	62.8 (15.8)	52.7 (9.3)
Isometric back strength (kgf)	61.8 (17.2)	50.4 (7.1)

Number in parentheses are standard deviations.

The RPE values averaged for each weight carried, walking speed, and ramp angle were between 11.9 and 17.6, with an overall average of 15.1 (± 2.9). An RPE of 15 corresponds to “hard” on the RPE scale. Figure 4 shows the RPE of the participants upon completing the backpacking tasks.

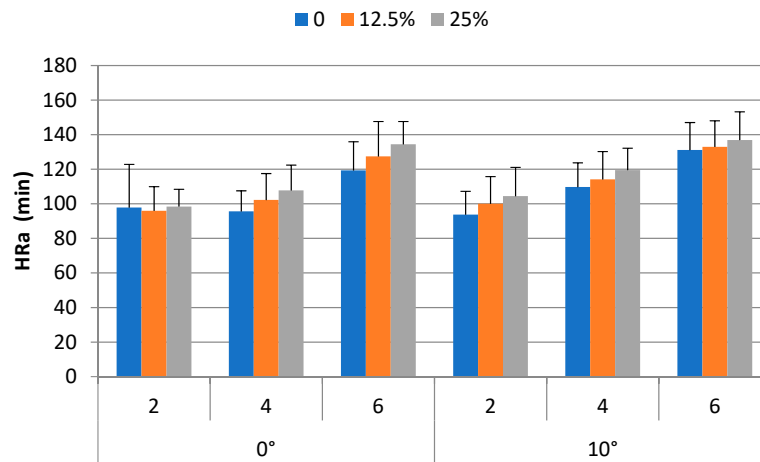


Figure 3. Heart rate after trial under experimental conditions.

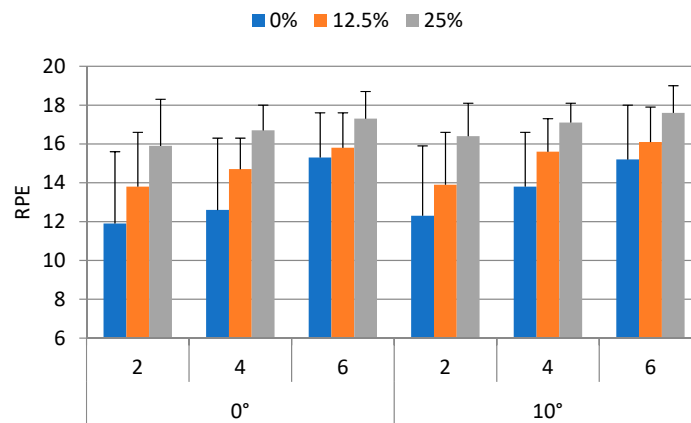


Figure 4. RPE under experimental conditions.

The decreases of the back strengths, averaged over each weight carried, walking speed, and ramp angle condition were between -1.1% and 9.9% . The corresponding leg strength decreases were between -1.7% and 9.1% . The strength decreases (%) on the back and the leg for performing the backpacking tasks are shown in Figures 5 and 6, respectively.

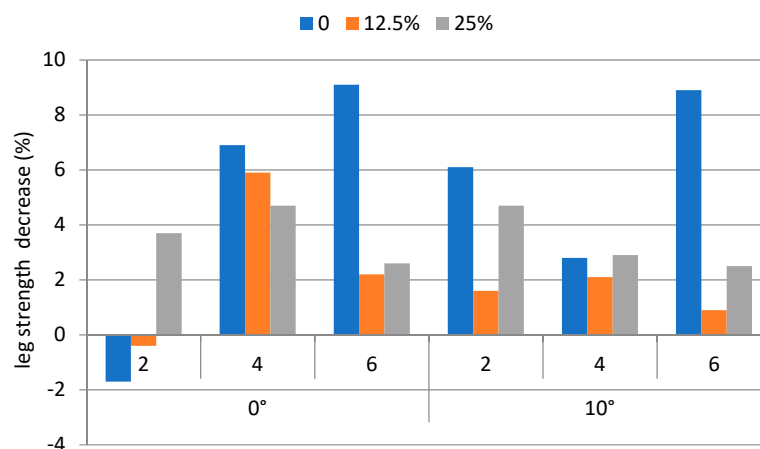


Figure 5. Leg strength decrease under experimental conditions.

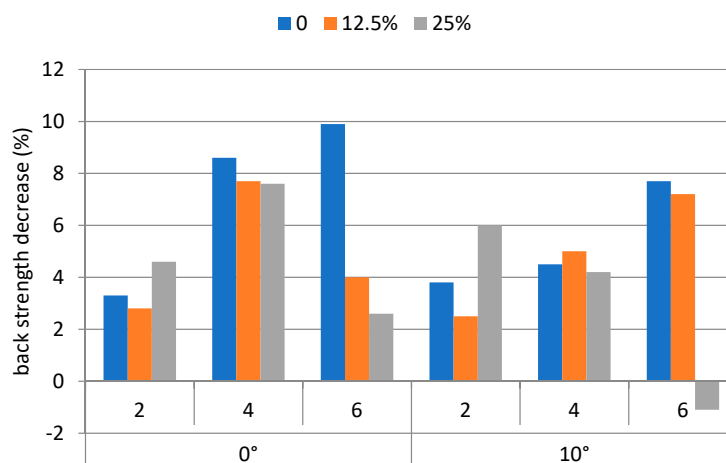


Figure 6. Back strength decrease under experimental conditions.

Figure 7 shows the MET under experimental conditions. The MET averaged over each weight carried, walking speed, and ramp angle condition ranged from 14.8 min to 125.5 min with an overall mean (\pm std) of 67.3 (\pm 48.3) min. The minimum and maximum values occurred at the least (the 0° ramp \times no weight \times 2 km/h) and most (10° ramp \times 25% body weight \times 6 km/h) strenuous conditions, respectively.

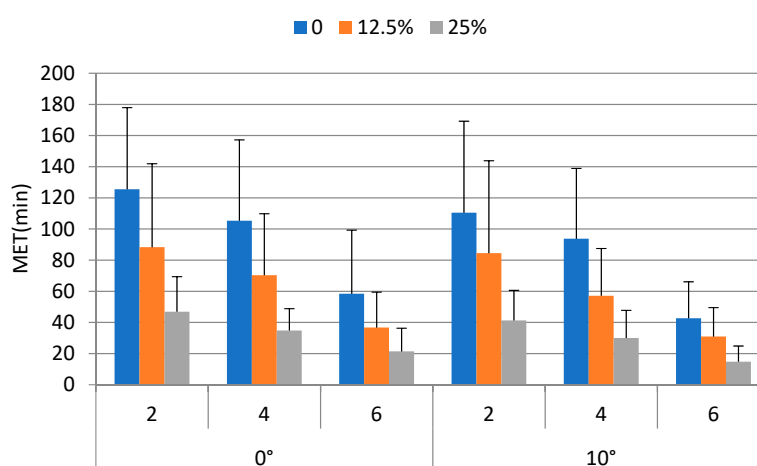


Figure 7. MET under experimental conditions.

3.2. ANOVA Results

The ANOVA results indicated that the MET were significantly affected by the weight carried ($p < 0.0001$), ramp angle ($p < 0.05$), and walking speed ($p < 0.0001$). The effects of gender were not statistically significant. The mean MET values for the 0, 12.5% and 25% BW conditions were 89.3, 61.3, and 31.6 mins, respectively. The Duncan's multiple range test results indicated that the MET without load carrying was significantly ($p < 0.05$) higher than those of the carrying 12.5% and 25% BW conditions. The MET of the 12.5% BW condition was significantly ($p < 0.05$) higher than that of the 25% BW conditions. The MET decreased when the walking speed increased. The mean MET values for the 2, 4, and 6 km/h walking speed were 82.8, 65.2, and 34.2 mins, respectively. The MET of the 2 km/h was significantly ($p < 0.05$) higher than those of the 4 and 6 km/h conditions. The MET of the 4 km/h was significantly ($p < 0.05$) higher than that of the 6 km/h condition. In addition, the MET for the 0° and 10° ramp conditions were 65.3 and 56.2 mins, respectively. They were significantly ($p < 0.05$) different.

The ANOVA results indicated that HR_a were significantly affected by the weight carried ($p < 0.001$), walking speed ($p < 0.0001$) and ramp angle ($p < 0.001$). The Duncan's multiple range test results indicated that HR_a of the 25%BW condition (116.9 bpm) was significantly ($p < 0.05$) higher than those of the 12.5%BW (112.1 bpm) and 0%BW (107.9 bpm) conditions. The HR_a of the 12.5%BW condition and that of the 0%BW were not significantly different. The HR_a for the 2 km/h (98.4 bpm) condition was significantly ($p < 0.05$) lower than those of the 4 km/h (108.1 bpm) and 6 km/h (130.3 bpm) conditions. The HR_a for the 4 km/h condition was significantly ($p < 0.05$) lower than that of the 6 km/h conditions. The HR_a of the 0° ramp angle condition (108.7 bpm) was significantly ($p < 0.05$) lower than that of the 10° condition (115.8 bpm).

The ANOVA results indicated that both the decrease (%) of the back and leg strengths were insignificant to the weight carrying condition, walking speed, and the ramp angle of the treadmill. A pairwise t -test results indicated that back strength decrease was significantly ($p < 0.05$) higher than that of leg strength decrease. Table 2 shows the Pearson's correlation coefficients between variables.

Table 2. Pearson's correlation coefficients.

Variable	MET	RPE	HR Increase
Weight carried	−0.49 *	0.47 *	-
Walking speed	−0.41 *	0.31 *	0.62 *
HR_a	−0.46 *	0.30 *	

* $p < 0.0001$.

The ANOVA results indicated that the RPE were significantly affected by the weight carried ($p < 0.0001$) and walking speed ($p < 0.0001$). The Duncan's multiple range test results indicated that the RPE without load carrying (13.5) was significantly ($p < 0.05$) lower than those of the 12.5% (15.0) and 25% (16.8) BW conditions. The RPE for the 12.5% BW condition was significantly ($p < 0.05$) lower than that of the 25% BW condition. The RPE when walked at 2 km/h (14.0) was significantly ($p < 0.05$) lower than those of the 4 km/h (15.1) and 6 km/h (16.2) conditions. The RPE for the 4 km/h condition was significantly ($p < 0.05$) lower than that of the 6 km/h conditions. The effects of ramp angle on RPE were not significant.

3.3. MET Modeling

The following equation was obtained in the regression analysis:

$$\ln(\text{MET}) = -4.423f_{MVC_{back}} + 1.283 \ln(\text{BW}) - 0.229v + 11.836 \ln(\cos\theta) \quad (6)$$

This equation was statistically significant ($p < 0.0001$) with an $R_{adj}^2 = 0.97$. Equation (6) may be converted to Equation (7):

$$\text{MET} = e^{-4.423f_{MVC_{back}}} \times \text{BW}^{1.283} \times 0.795^v \times (\cos\theta)^{11.836} \quad (7)$$

A mean absolute deviation (MAD) was calculated using the following equation to compare the actual MET and predicted MET:

$$\text{MAD} = \frac{1}{n} \sum_{i=1}^n (\text{actual MET} - \text{predicted MET}) \quad (8)$$

The MAD of Equation (8) in estimating the MET in our backpacking tasks were 29.7 (mins).

4. Discussion

Muscular strength decrease has been adopted to quantify the progress of muscular fatigue [10,36,37]. Analyzing the decrease of muscular strength in a single muscle is less complicated but is of little

practical use in resolving industrial problems. Assessing the muscular strength in performing a certain task is common. The task-specific assessment of muscular strength, however, involves contractions of multiple muscles. Both the isometric back and leg strengths were measured by having the participants pull a handle 38 cm above the platform, following the protocol in the literature [42]. It should be noted that the fixed handle height could lead to variations in body posture for participants with different body dimensions. It was likely that the MVC values measured using this protocol might be lower than the real MVCs of the participants, especially the taller ones.

It was hypothesized that the strengths of the back and leg would decrease upon performing the backpacking tasks. However, both the back and leg strengths decreased only moderately (<10%). In addition, to our further surprise, the decreases of these two strengths after the trial were not affected by any of the three factors tested. An explanation of these phenomena may be that muscular strength decrease due to performing physical tasks is more likely to occur under static muscular contraction conditions. Muscular contractions on the leg were dynamic. Such dynamic contractions facilitate blood circulation, and hence slow down the onset of muscular fatigue. On the other hand, back muscle contractions were required to support the backpacking tasks. These muscles might; however, provide only partial contributions to the tasks. Many other muscles in the trunk, such as those in abdomen and shoulders, might also play a role. Unfortunately, muscular strength for those muscles could not be measured due to technical difficulties and the limitations of our apparatus. Decrease of both of the back and leg strengths were, therefore, less prominent than what we had expected. Strength decrease in the back was significantly ($p < 0.05$) higher than that on the leg, as back muscles experienced less dynamic contractions than those of the leg muscles.

For prolonged physical activities, heart rate is one of the most appropriate physiological parameters for indicating physiological strain. The perceived physical exertion is also believed to be “the single best indicator of the degree of physical strain” [40]. It is well known that the RPE was developed based on heart rate. Even though the results indicated that walking with load carriage resulted in increased heart rate and elevated RPE ratings, the Pearson’s correlation coefficient between our RPE and HR_a was only 0.3. This was much lower than those reported in the literature [41]. In addition, the RPE, averaged over all experimental conditions, at the end of the trial was 15.1. According to Borg [40], this value corresponded to a heart rate of 151 for adults aged between 30 and 50 years. Our HR_a , averaged over all experimental conditions, was only 112. This might be attributed to factors other than physiological strain such as age and the type of physical exertion. Our participants were college students with a mean age of 21.7 years old. Their maximum heart rates were higher than those of the adults in Borg’s study. They might give higher RPE scores than what have been anticipated based on the literature [40]. A linear regression analysis without intercept has been performed using the RPE as the dependent variable and the HR_a as the independent variable. The following equation was obtained with an R^2 of 0.95 and $p < 0.0001$:

$$RPE = 0.131 \times HR_a \quad (9)$$

The regression coefficient of 0.131 was 31% higher than the 0.1 suggested in the literature [36]. As the participants might walk up to approximately 3 hours in some trials, they could give relatively high RPE because of thirst, as the participants were not allowed to drink during the trial. In addition to age, feelings of boredom, discomfort on the shoulder due to the pressure of the strap of the pack on the local muscles, and some other reasons might also have affected the RPE reported by the participants.

It is well known that f_{MVC} has nonlinear effects on MET and both power and exponential functions have been adopted in the modeling of MET [36,37,46,47]. The early literature [31,32] indicated an indefinite exertion period for low f_{MVC} . The so-called “indefinite exertion period” has been challenged for f_{MVC} as low as 0.05 [48]. A power model of the f_{MVC} was not considered in the current study, because it is undefined when the f_{MVC} is equal to 0. An undefined MET function implies an indefinite MET. This is not reasonable in our backpacking tasks even there was no external load on the back. Exponential model (Equation (2)) was then fitted. In Equation (8), predictive MET was established

considering f_{MVC_back} , BW, ramp angle, and walking speed. The f_{MVC_back} , ramp angle, and walking speed were associated with physical burdens or job demand of the tasks. Figures 8 and 9 show the predicted MET using Equation (8) for ramp angles of 0° and 10° , respectively. The predicted MET values in these two figures were calculated using the average BW (63 kg) of the participants. For both ramp angles, the difference between the predicted MET values for any two walking speeds tested was becoming smaller when the f_{MVC_back} was getting higher. The effects of walking speed on the MET were more prominent at low f_{MVC_back} than were at a high one. This was consistent with the findings in the literature [35]. The MET model established in the current study may be used to determine the work/rest allowance for backpacking tasks similar to ours.

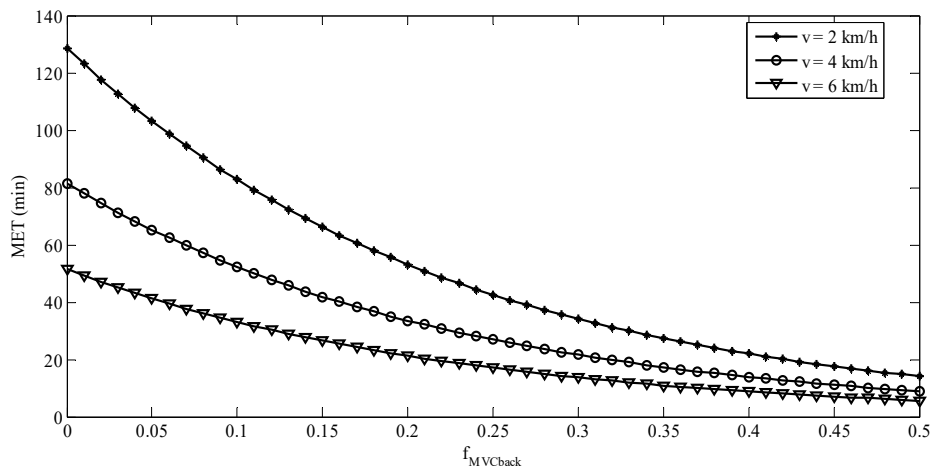


Figure 8. Predicted MET when $\theta = 0^\circ$ and BW = 63 kg.

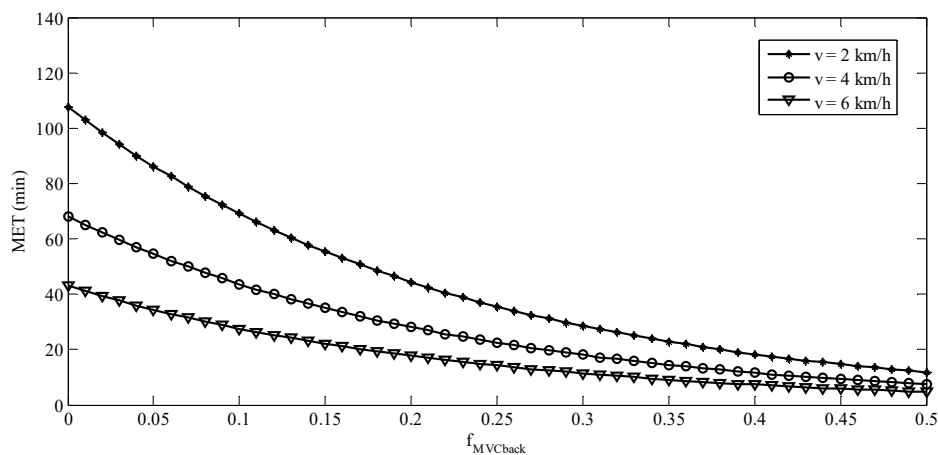


Figure 9. Predicted MET when $\theta = 10^\circ$ and BW = 63 kg.

There were limitations in the study. First of all, the participants were not allowed to drink or listen to music. Instead of being physically exhausted, they might have given up walking because of thirst, boredom, or some other reasons. In other words, their MET values could be higher than what were recorded if they were allowed to replenish water when they were thirsty or if they were allowed to listen to their favorite music. Replenishment of water and music listening may be important factors affecting the decrease of muscular strength, RPE, and MET. Effects of such factors will be interesting topics in the future. Secondly, the experiment was conducted in the laboratory where the temperature and relative humidity were controlled at $21.1 (\pm 2.4)^\circ\text{C}$ and $65.1 (\pm 9.7)\%$, respectively. It is well known that temperature and humidity do affect the physiological strain of people performing physical tasks. We believe that the MET should be lower than our prediction if the task was performed in an environment with higher temperature or humidity than ours. Thirdly, age was not considered in

the modeling of MET due to the nature of our participants. Our MET model may not be applicable to people in other age groups, especially school-aged children. This is because the ranges of the body weight and walking speed of our participants are much higher than those of children. Other MET models should be established for backpacking for school-aged children in the future. Finally, the sample size of this study was not large. This was due to our budget constraint. However, a sample size of 16 was believed to be acceptable as it was larger than some of the studies in the literature [28,49].

5. Conclusions

The participants carried a backpack and walked until they could no longer do so. The endurance time for the backpacking tasks under different weight carried, walking speed, and ramp angle conditions ranged from approximately 15 min to more than two hours. These tasks resulted in an increase of heart rate and elevated perceived exertion. Our data support the hypotheses that both the MET and heart rate are affected by the weight carried, walking speed, and ramp angle. The RPE was also affected by the weight carried and walking speed significantly. The effects of ramp angle were not significant on RPE. The RPE/heart rate ratio for our backpacking tasks was 31% higher than that in the literature [40] implying the calibration of the RPE may be required for such tasks. Factors affecting the pause of backpacking tasks are very complicated. Muscular strength decreases on the back and leg might not be the predominant ones as these strengths declined only moderately at the end of the tasks. A MET model incorporating the f_{MVC_back} , body weight, walking speed, and ramp angle was established. This model may be used to determine the work/rest allowance for backpacking tasks under conditions similar to this study.

Author Contributions: Conceptualization, K.W.L. and J.C.C.; Methodology, K.W.L.; Data Collection, J.C.C. and C.C.C.; Formal Analysis, K.W.L., J.C.C.; Resources, K.W.L.; Writing—Original Draft Preparation, K.W.L.; Writing—Review & Editing, J.C.C. and C.C.C.

Funding: This research was financially supported by a grant from the Ministry of Science & Technology (MOST) of the Republic of China (ROC) under contract 106-2221-E-216-008-MY3.

Acknowledgments: The authors thank Ying Chen, a graduate student in safety engineering at Xian University of Science & Technology, and Yi-Hong Tang, an undergraduate student in industrial management at Chung Hua University, Lu Peng, a Ph.D. student with the System Engineering & Engineering Management Department at City University of Hong Kong, and Yu-Shan Jiang, a graduate student with National Taiwan University, for their assistance in the study.

Conflicts of Interest: The authors declare no conflict of interest.

References

1. Institute for Labor and Occupational Safety and Health (ILOSH). *Local Study on Ergonomic and Musculoskeletal Health Assessments*; Technical Report 2014, ILOSH103-3083; ILOSH: Taipei, Taiwan, 2014. (In Chinese)
2. Institute for Labor and Occupational Safety and Health (ILOSH). *Ergonomic Risk Assessments for Specific Occupation*; Technical Report 2015, ILOSH103-H308; ILOSH: Taipei, Taiwan, 2014. (In Chinese)
3. Snook, S.H. The design of manual handling tasks. *Ergonomics* **1978**, *21*, 963–985. [[CrossRef](#)] [[PubMed](#)]
4. Dempsey, P.G.; Hashemi, L. Analysis of workers' compensation claims associated with manual materials handling. *Ergonomics* **1999**, *42*, 183–195. [[CrossRef](#)] [[PubMed](#)]
5. Waters, T.R.; Dick, R.B.; Davis-Barkley, J.; Krieg, E.F. A cross-sectional study of risk factors for musculoskeletal symptoms in the workplace using data from the General Social Survey (GSS). *J. Occup. Environ. Med.* **2007**, *49*, 172–184. [[CrossRef](#)]
6. Chaffin, D.B.; Andres, R.O.; Garg, A. Volitional postures during maximal push/pull exertions in the sagittal plane. *Hum. Factors* **1983**, *25*, 541–550. [[CrossRef](#)] [[PubMed](#)]
7. Mamansari, D.U.; Salokhe, V.M. Static strength and physical work capacity of agricultural labourers in the central plain of Thailand. *Appl. Ergon.* **1996**, *27*, 53–60. [[CrossRef](#)]
8. Bigland-Ritchie, B.; Woods, J.J. Changes in muscle contractile properties and neural control during human muscular fatigue. *Muscle Nerve* **1984**, *7*, 691–699. [[CrossRef](#)] [[PubMed](#)]

9. Enoka, R.M.; Duchateau, J. Muscle fatigue: What, why and how it influences muscle function. *J. Physiol.* **2008**, *586*, 11–23. [[CrossRef](#)]
10. Ma, L.; Zhang, W.; Hu, B.; Chablat, D.; Bennis, F.; Guillaume, F. Determination of subject-specific muscle fatigue rates under static fatiguing operations. *Ergonomics* **2013**, *56*, 1889–1900. [[CrossRef](#)]
11. Vøllestad, N. Measurement of human muscle fatigue. *J. Neurosci. Methods* **1997**, *74*, 219–227. [[CrossRef](#)]
12. Edwards, R.H. Human muscle function and fatigue. *Ciba Found. Symp.* **1981**, *82*, 1–18. [[PubMed](#)]
13. Booth, F.W.; Thomason, D.B. Molecular and cellular adaptation of muscle in response to exercise: Perspectives of various models. *Physiol. Rev.* **1991**, *71*, 541–585. [[CrossRef](#)]
14. Ma, L.; Chablat, D.; Bennis, F.; Zhang, W. A new simple dynamic muscle fatigue model and its validation. *Int. J. Ind. Ergon.* **2009**, *39*, 211–220. [[CrossRef](#)]
15. Roman-Liu, D.; Tokarski, T.; Kowalewski, R. Decrease of force capabilities as an index of upper limb fatigue. *Ergonomics* **2005**, *48*, 930–948. [[CrossRef](#)]
16. Roman-Liu, D.; Tokarski, T.; Wojcik, K. Quantitative assessment of upper limb muscle fatigue depending on the conditions of repetitive task load. *J. Electromyogr. Kinesiol.* **2004**, *14*, 671–682. [[CrossRef](#)]
17. Iridiastadi, H.; Nussbaum, M. Muscle fatigue and endurance during repetitive intermittent static efforts: development of prediction models. *Ergonomics* **2006**, *49*, 344–360. [[CrossRef](#)]
18. Wood, D.; Fisher, D.; Andres, R. Minimizing fatigue during repetitive jobs: Optimal work-rest schedules. *Hum. Factors* **1997**, *39*, 83–101. [[CrossRef](#)]
19. Ma, L.; Chablat, D.; Bennis, F.; Zhang, W.; Hu, B.; Guillaume, F. A novel approach for determining fatigue resistances of different muscle groups in static cases. *Int. J. Ind. Ergon.* **2011**, *41*, 10–18. [[CrossRef](#)]
20. Zhang, Z.; Li, K.W.; Zhang, W.; Ma, L.; Chen, Z. Muscular fatigue and maximum endurance time assessment for male and female industrial workers. *Int. J. Ind. Ergon.* **2014**, *44*, 292–297. [[CrossRef](#)]
21. Li, K.W.; Wang, C.W.; Yu, R. Modeling of Predictive Muscular Strength for Sustained One-Handed Carrying Task. *Work* **2015**, *52*, 911–919. [[CrossRef](#)]
22. Li, K.W.; Chiu, W.-S. Isometric Arm Strength and Subjective Rating of Upper Limb Fatigue in Two-Handed Carrying Tasks. *PLoS ONE* **2015**, *10*, e0119550. [[CrossRef](#)]
23. El Ahrache, K.; Imbeau, D.; Farbos, B. Percentile values for determining maximum endurance times for static muscular work. *Int. J. Ind. Ergon.* **2006**, *36*, 99–108. [[CrossRef](#)]
24. Kahn, J.F.; Monod, H. Fatigue induced by static work. *Ergonomics* **1989**, *32*, 839–846. [[CrossRef](#)]
25. Avin, K.G.; Naughton, M.R.; Ford, B.W.; Moore, H.E.; Monitto-Webber, M.N.; Stark, A.M.; Gentile, A.J.; Frey Law, L.A. Sex differences in fatigue resistance are muscle group dependent. *Med. Sci. Sports Exerc.* **2010**, *42*, 1943–1950. [[CrossRef](#)]
26. Bishu, R.; Kim, B.; Klute, G. Force-endurance relationship: Does it matter if gloves are donned? *Appl. Ergon.* **1995**, *26*, 179–185. [[CrossRef](#)]
27. Frey Law, L.A.; Avin, K.G. Endurance time is joint-specific: A modelling and meta-analysis investigation. *Ergonomics* **2010**, *53*, 109–129. [[CrossRef](#)]
28. Garg, A.; Hegmann, K.T.; Schwoerer, B.J.; Kapellusch, J.M. The effect of maximum voluntary contraction on endurance times for the shoulder girdle. *Int. J. Ind. Ergon.* **2002**, *30*, 103–113. [[CrossRef](#)]
29. Manenica, I. A technique for postural load assessment. In *The Ergonomics of Working Postures*; Corlett, N., Wilson, J., Manenica, I., Eds.; Taylor & Francis: London, UK, 1986; pp. 270–277.
30. Mathiassen, S.E.; Ahsberg, E. Prediction of shoulder flexion endurance from personal factors. *Int. J. Ind. Ergon.* **1999**, *24*, 315–329. [[CrossRef](#)]
31. Rohmert, W. Problems in determining rest allowances Part 1: Use of modern methods to evaluate stress and strain in static muscular work. *Appl. Ergon.* **1973**, *4*, 91–95. [[CrossRef](#)]
32. Rohmert, W.; Wangenheim, M.; Mainzer, J.; Zipp, P.; Lesser, W. A study stressing the need for a static postural force model for work analysis. *Ergonomics* **1986**, *29*, 1235–1249. [[CrossRef](#)]
33. Rose, L.; Ericsson, M.; Glimskar, B.; Nordgren, B.; Ortengren, R. Ergo-Index. Development of a model to determine pause needs after fatigue and pain reactions during work. In *Computer Application in Ergonomics, Occupational Safety and Health*; Mattila, M., Karwowski, W., Eds.; Elsevier Science Publishers: Amsterdam, The Netherlands, 1992; pp. 461–468.
34. Van Dieen, J.H.; Oude Vrielink, H.H.E. The use of the relation between relative force and endurance time. *Ergonomics* **1994**, *37*, 231–243. [[CrossRef](#)]

35. Li, K.W.; Peng, L.; Yi, C. Modeling of maximum endurance time for one-handed carrying tasks. *Hum. Factors Man.* **2019**, in press. [[CrossRef](#)]
36. Liu, B.; Ma, L.; Chen, C.; Zhang, Z. Experimental validation of a subject-specific maximum endurance time model. *Ergonomics* **2018**, *61*, 806–817. [[CrossRef](#)]
37. Liu, B.; Ma, L.; Zhang, W.; Zhang, Z. Subject-specific hand grip fatigability indicator determined using parameter identification technique. *Hum. Factors Man.* **2019**, *29*, 86–94. [[CrossRef](#)]
38. Perrone, M.; Orr, R.; Hing, W.; Milne, N.; Pope, R. The impact of backpack loads on school children: A critical narrative review. *Int. J. Environ. Res. Public Health* **2018**, *15*, 2529. [[CrossRef](#)]
39. Joseph, A.; Wiley, A.; Orr, R.; Schram, B.; Dawes, J.J. The impact of load carriage on measures of power and agility in tactical occupations: A critical review. *Int. J. Environ. Res. Public Health* **2018**, *15*, 88. [[CrossRef](#)]
40. Borg, G. Psychophysical bases of perceived exertion. *Med. Sci. Sports Exerc.* **1982**, *14*, 377–381. [[CrossRef](#)]
41. Borg, G. Psychophysical scaling with applications in physical work and the perception of exertion. *Scan. J. Work Environ. Health* **1990**, *16*, 55–58. [[CrossRef](#)]
42. Ayoub, M.M.; Mital, A. *Manual Materials Handling*; Taylor & Francis: London, UK, 1989; pp. 229–233.
43. Brooks, A.G.; Gunn, S.M.; Withers, R.T.; Gore, C.J.; Plummer, J.L. Predicting Walking METs and Energy Expenditure from Speed or Accelerometry. *Med. Sci. Sports Exerc.* **2005**, *37*, 1216–1223. [[CrossRef](#)]
44. Haisman, M.F. Determinants of load carrying ability. *Appl. Ergon.* **1988**, *19*, 111–121. [[CrossRef](#)]
45. Garg, A.; Chaffin, D.B.; Herrin, G.D. Prediction of metabolic rates for manual materials handling jobs. *Am. Ind. Hyg. Assoc. J.* **1978**, *39*, 661–674. [[CrossRef](#)]
46. Yi, C.; Tang, F.; Peng, L.; Li, K.W.; Ma, L.; Hu, H. Modeling of Maximum Endurance Time for Static Pulling Tasks. *Work* **2018**, *60*, 455–463. [[CrossRef](#)]
47. Yi, C.; Li, K.W.; Tang, F.; Ma, L.; Hu, H.; Zuo, H. Modeling of Maximum endurance time for two-handed truck pulling tasks. *PLoS ONE* **2018**, *13*, e0207283.
48. Jorgensen, K.; Fallentin, N.; Krogh-Lund, C.; Jensen, B. Electromyography and fatigue during prolonged, low-level static contractions. *Eur. J. Appl. Physiol.* **1988**, *57*, 316–321. [[CrossRef](#)]
49. Rose, L.; Ericsson, M.; Ortengren, R. Endurance time, pain and resumption in passive loading of the elbow joint. *Ergonomics* **2000**, *43*, 405–420. [[CrossRef](#)]



© 2019 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<http://creativecommons.org/licenses/by/4.0/>).