

Article **Cone Beam Computed Tomography Radiomics for Prostate Cancer: Favourable vs. Unfavourable Prognosis Prediction**

Bruno Mendes 1,2,* [,](https://orcid.org/0000-0002-7574-7630) Inês Domingues 1,3 [,](https://orcid.org/0000-0002-2334-7280) Filipe Dias [1](https://orcid.org/0000-0002-2992-5096) and João Santos 1,[4](https://orcid.org/0000-0003-2465-5143)

- ¹ Centro de Investigação do Instituto Português de Oncologia do Porto (CI-IPOP), Grupo de Física Médica, Radiobiologia e Protecção Radiológica, 4200-072 Porto, Portugal
- ² Faculdade de Engenharia da Universidade do Porto (FEUP), 4200-465 Porto, Portugal
- 3 Instituto Superior de Engenharia de Coimbra (ISEC), 3030-199 Coimbra, Portugal
- 4 Instituto de Ciências Biomédicas Abel Salazar (ICBAS), 4050-313 Porto, Portugal

***** Correspondence: bruno.mendes@ipoporto.min-saude.pt

Abstract: Silently asymptomatic at an early stage and often painless, requiring only active surveillance, Prostate Cancer (PCa) is traditionally diagnosed by a Digital Rectal Examination (DRE) and a Prostate Specific Antigen (PSA) blood test. A histological examination, searching for pattern irregularities on the prostate glandular tissue, is performed to quantify the aggressiveness of PCa. The assigned Gleason Score (GS), usually combined with Transrectal Ultrasound Guided Biopsy (TRUS), allows the stratification of patients according to their risk group. Intermediate-risk patients may have a favourable $(GS = 3 + 4)$ or unfavourable $(GS = 4 + 3)$ prognosis. This borderline is critical for defining treatments and possible outcomes, while External Beam Radiotherapy (EBRT) is a curative option for localised and locally advanced disease and as a palliative option for metastatic low-volume disease; active surveillance or watchful waiting can also be an option for patients with a favourable prognosis. With radiomics, quantifying phenotypic characteristics in medical imaging is now possible. In the EBRT workflow, there are several imaging modalities, such as Magnetic Ressonance Imaging (MRI), Computed Tomography (CT), Positron Emission Tomography (PET), Ultrasound and Cone Beam Computed Tomography (CBCT). Most radiomic PCa studies focused on MRI and addressed tumour staging, GS, PSA or Biochemical Recurrence (BCR). This study intends to use CBCT radiomics to distinguish between favourable and unfavourable cases, with the potential of evaluating an ongoing treatment. Seven of the most used feature selection methods, combined with 14 different classifiers, were evaluated in a total of 98 pipelines. From those, six stood out with Area Under the Receiver Operating Characteristic (AUROC) values \geq 0.79. To the best of our knowledge, this is the first work to evaluate a PCa favourable vs. unfavourable prognosis model based on CBCT radiomics.

Keywords: radiomics; CBCT; favourable; prognosis; risk group

1. Introduction

In 1853, John Adams, a surgeon at the London Hospital, diagnosed a cirrhosis of the prostate gland as an orphan disease, the first described case of Prostate Cancer (PCa). In 2020, the disease was responsible for 7.3% of all cancer deaths in men and was the second most frequent malignancy [\[1\]](#page-12-0). The prostate gland is about the size of a walnut and located in the pelvis surrounding the prostatic urethra and below the bladder. Usually, PCa originates from the peripheral zone of the prostate, adjacent to the rectum [\[2\]](#page-12-1). Silently asymptomatic in an early stage, PCa is usually diagnosed by a Digital Rectal Examination (DRE) and a Prostate Specific Antigen (PSA) blood test.

The aggressiveness of PCa is quantified by the Gleason Grading System [\[3\]](#page-12-2). Based on the glandular architecture of cells, the pathologist assigns a grade of 1 if prostate cells are uniformly packed, up to a grade of 5 depending on pattern irregularity. The most predominant pattern and the second most prevalent are identified and graded accordingly,

Citation: Mendes, B.; Domingues, I.; Dias, F.; Santos, J. Cone Beam Computed Tomography Radiomics for Prostate Cancer: Favourable vs. Unfavourable Prognosis Prediction. *Appl. Sci.* **2023**, *13*, 1378. [https://](https://doi.org/10.3390/app13031378) doi.org/10.3390/app13031378

Academic Editors: Pedro Couto and Vitor Filipe

Received: 30 November 2022 Revised: 13 January 2023 Accepted: 17 January 2023 Published: 20 January 2023

Copyright: © 2023 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license [\(https://](https://creativecommons.org/licenses/by/4.0/) [creativecommons.org/licenses/by/](https://creativecommons.org/licenses/by/4.0/) 4.0/).

and finally summed to obtain the [Gleason Score \(GS\),](#page-0-0) proportional to [PCa](#page-0-0) aggressiveness [\[4\]](#page-12-3). In 2014, Epstein et al. [\[5\]](#page-12-4) proposed a new Gleason grading system when several studies showed that a [GS](#page-0-0) $7 = 4 + 3$ had a worst prognosis than GS $7 = 3 + 4$. A deeper stratification by [Grade Group \(GG\)](#page-0-0) was then possible, including the most likely prognosis. The low/very low [Risk Group \(RG\)](#page-0-0) is assigned to patients with a $GS \leq 6$ $GS \leq 6$. The intermediate [RG](#page-0-0) includes patients classified with a [GS](#page-0-0) of 7, with both favourable (3+4) and unfavourable (4+3) prognosis. Finally, the high/very high [RG](#page-0-0) includes patients with a $GS > 7$ $GS > 7$.

[GS](#page-0-0) plays an important role in the determination of the type of treatment to follow. A low-grade cancer with a [GS](#page-0-0) 6, together with a low [PSA](#page-0-0) level and a small tumor may be an indication for active surveillance only. [PCa](#page-0-0) evaluation takes into account the [PSA](#page-0-0) levels, [GS,](#page-0-0) TNM, patient history and physical examinations in order to provide a decision baseline for proper treatment and success prediction. Current guidelines suggest [External Beam](#page-0-0) [Radiotherapy \(EBRT\)](#page-0-0) as a curative option for localised and locally advanced disease and as a palliative option for metastatic low-volume disease [\[6\]](#page-12-5). The effectiveness of the treatment usually relies on the monitoring of [PSA](#page-0-0) blood levels, the current reference biological test. Although a high value is associated with an increased risk of [PCa,](#page-0-0) it is not [PCa](#page-0-0) specific. High values of [PSA](#page-0-0) are also associated with [Benign Prostatic Hyperplasia \(BPH\),](#page-0-0) an enlarged prostate gland [\[7\]](#page-12-6). With the wide availability of [PSA](#page-0-0) tests and the known long-term effects of definitive therapy, overdiagnosis and overtreatment have become a major issue. [PCa](#page-0-0) treatments may cause sexual dysfunction, infertility, bowel and urinary problems [\[6\]](#page-12-5), and so more conservative approaches such as active surveillance or watchful waiting have been adopted [\[8\]](#page-12-7). These are valid options, even for intermediate risk patients with a favourable prognosis $(GS = 3 + 4)$ $(GS = 3 + 4)$.

During the [EBRT](#page-0-0) workflow, many imaging modalities are available. The [Computed](#page-0-0) [Tomography \(CT\)](#page-0-0) provides the [Hounsfield Unit \(HU\)](#page-0-0) values critical for dose estimations. For [PCa,](#page-0-0) [Magnetic Ressonance Imaging \(MRI\),](#page-0-0) providing superior soft-tissue resolution, is used for volume delineation. [Positron Emission Tomography \(PET\)](#page-0-0) provides tumour cells' metabolic insights and finally, the [Cone Beam Computed Tomography \(CBCT\),](#page-0-0) acquired during [EBRT](#page-0-0) sessions, is used for patient positioning and setup verifications. Quantitative analysis of medical images may have a similar prognosis power to phenotypes and gene protein signatures [\[9\]](#page-12-8). This is the hypothesis behind radiomics (the extraction of features from radiographic images using data-characterization algorithms). As an emerging field in medicine, radiomics provides the quantification of phenotypic characteristics in medical imaging [\[10\]](#page-12-9). Traditionally, image analysis and characterization of shape, texture or patterns is performed by highly trained human observers, but radiomics can provide quantitative image analysis without inter/intra observer variability.

Radiomic studies have recently triggered the interest of the research community, and for [PCa](#page-0-0) are mainly focused on several predictive outcomes such as staging, grading, detection, [Biochemical Recurrence \(BCR\)](#page-0-0) or aggressiveness. Furthermore, the most used imaging modality is [MRI,](#page-0-0) which is usually performed in the initial stages and is critical for volume delineation. With the predictive and phenotypic power of radiomics, other imaging modalities besides [MRI](#page-0-0) may provide valuable insights. Mendes et al. [\[11\]](#page-12-10) evaluated [CT](#page-0-0) based radiomics to predict [PCa](#page-0-0) aggressiveness with promising results. In a novel attempt, Bosetti et al. [\[12\]](#page-13-0) evaluated the use of [CBCT](#page-0-0) radiomics to address tumour staging, [GS,](#page-0-0) [PSA,](#page-0-0) [RG](#page-0-0) and [BCR.](#page-0-0) Monitoring and classifying the outcome prognosis during treatment may help to avoid extra-invasive procedures or another [MRI.](#page-0-0) This work intends to evaluate a model in borderline favourable vs. unfavourable (3+4 vs. 4+3) [PCa](#page-0-0) cases, providing a tool that may trigger a more conservative approach, avoiding over-treatment and reducing the side effects of radiation exposure.

Following this introductory section is a summary of some of the work done in [PCa](#page-0-0) radiomics using multiple imaging modalities. The idea is to gather information on the most-used feature selection and classification techniques. Section [3](#page-3-0) describes the dataset and the methods used to build the evaluated pipelines. Section [4](#page-6-0) presents the obtained results, highlighting the six best pipelines (from 98 evaluated). Finally, Section [5](#page-10-0) presents the main conclusions drawn.

2. Related Work

Radiomics, the extraction of quantitative features from medical images using data characterization algorithms, has the potential to provide more relevant information, improve decision outcomes and avoid overdiagnosis and overtreatment. A full radiomic study follows a pipeline initially proposed by Lambin et al. [\[13\]](#page-13-1) involving several steps, as exemplified in Figure [1.](#page-2-0)

Figure 1. Radiomic studies pipeline.

Many imaging modalities are of great value in screening [PCa](#page-0-0) and improving diagnosis and prognosis outcomes [\[14\]](#page-13-2). [MRI](#page-0-0) provides superior soft-tissue contrast resolution when compared to other imaging modalities. It is the selected imaging modality by [Prostate](#page-0-0) [Imaging Reporting and Data System \(PIRADS\).](#page-0-0) Most radiomic studies are focused on [MRI](#page-0-0) with the [PCa](#page-0-0) clinical significance as a model endpoint [\[15–](#page-13-3)[21\]](#page-13-4). The combination of T1 and T2 weighted sequences [\(multi-parametric Magnetic Ressonance Imaging \(mpMRI\)\)](#page-0-0) allows us to overcome the poor correlation between [MRI](#page-0-0) signal intensities and tissue properties. With this in mind, several authors evaluated the use of [MRI](#page-0-0) for [PCa](#page-0-0) patient stratification with promising results [\[16](#page-13-5)[–19\]](#page-13-6), although the introduction of clinical outcomes such as [PSA](#page-0-0) or [GS](#page-0-0) introduced some issues [\[20\]](#page-13-7). Abraham and Nair [\[22\]](#page-13-8) topped the PROSTATEx-2 2017 challenge with a quadratic-weighted kappa score of 0.2772, developing a new feature selection method for [PCa](#page-0-0) aggressiveness assessment. Algohary et al. [\[23\]](#page-13-9) sought a model to evaluate [Intensity Modulated Radiation Therapy \(IMRT\)](#page-0-0) [PCa](#page-0-0) treatment responses using T2w and [Apparent Diffusion Coefficient \(ADC\)](#page-0-0) maps in an attempt to personalize the [PCa](#page-0-0) treatment evaluation framework.

[PET](#page-0-0) provides insights into the pathological responses to some types of cancers with the addition of a radio-tracer and a viable tool for diagnosing, staging and grading. For radiomic [PCa](#page-0-0) studies, researchers focused on evaluating lymph node involvement, metastasis, [GS](#page-0-0) and extra-capsular extension [\[24\]](#page-13-10). Alongi et al. [\[25\]](#page-13-11) evaluated tumour heterogeneity with 18F-Cho[-PET/CT](#page-0-0) radiomics and introduced a novel feature selection method (a mixed descriptive-inferential sequential approach).

[CT](#page-0-0) seems to be a poor candidate for radiomic studies since it lacks metabolic manifestation and soft-tissue contrast. However, the spatial distribution provided by the [CT](#page-0-0) could be used as a virtual biopsy for patient risk stratification [\[26\]](#page-13-12). In a recent work, Mendes et al. [\[11\]](#page-12-10) evaluated the use of [CT](#page-0-0) based radiomics for [PCa](#page-0-0) aggressiveness assessment. With a dataset of 44 [PCa](#page-0-0) patients, Mendes et al. [\[11\]](#page-12-10) extracted features using pyradiomics [\[10\]](#page-12-9) and [Local Image Features Extraction \(LIFEx\)](#page-0-0) [\[27\]](#page-13-13). Unable to find a radiomic signature for [RG](#page-0-0) stratification, they used [Principal Component Analysis \(PCA\)](#page-0-0) and evaluated several kernels to build a model with a [Support Vector Machine \(SVM\).](#page-0-0) The best results were obtained with pyradiomics with a maximum [Area Under the Receiver](#page-0-0) [Operating Characteristic \(AUROC\)](#page-0-0) value of 0.88 for both low/very low and high/very high [RG.](#page-0-0)

[CBCT](#page-0-0) is used for patient positioning verification procedures before [EBRT](#page-0-0) treatment and therefore is freely available. Bosetti et al. [\[12\]](#page-13-0) were the first to study the use of [CBCT](#page-0-0) radiomics to build models predicting tumour staging, [GS,](#page-0-0) [PSA](#page-0-0) levels, risk category and biochemical recurrence with promising results. In this work, we intend to evaluate the use of [CBCT](#page-0-0) radiomics to distinguish between favourable and unfavourable [PCa](#page-0-0) cases. An unevaluated scenario that may provide an [EBRT](#page-0-0) treatment effectiveness monitoring tool is used.

3. Materials and Methods

This work is a retrospective piece of research that uses treatment plans available at [Instituto Português de Oncologia do Porto Francisco Gentil \(IPO-PORTO\).](#page-0-0) All patients had an initial [CT](#page-0-0) scan, required for dose estimation and volume delineations, and [CBCT](#page-0-0) of the first [EBRT](#page-0-0) treatment session, used for patient positioning setup verification. The full analysis was performed on an Intel(R) Core(TM) i7-6500U CPU@2.50GHz 2.60 GHzz, with 16 Gb of RAM and an Nvidia GeForce 930M (2Gb DDR3).

3.1. Study Population

This study includes a subset of patients from a dataset containing [CT](#page-0-0) and [CBCT](#page-0-0) images from 70 patients. All studies ranged from 2019 to 2021 with curative intent, and patients were between 51 and 89 years old. [CT](#page-0-0) images were acquired in a 16 slice [CT](#page-0-0) scanner from General Electric, GE Optima 580 available at the [IPO-PORTO](#page-0-0) for [EBRT,](#page-0-0) acquired at 120 kVp, with 2.500 mm of slice thickness, automatic tube current modulation, a pixel spacing of 0.976×0.976 and 16 bits of pixel depth. For the same patients [CBCT](#page-0-0) images were acquired from the on-board imaging devices installed in NOVALIS, TRUEBEAM and TRILOGY [Medical Linear Accelerators \(LINACs\)](#page-0-0) from Varian. Acquisition settings depend on the [LINAC](#page-0-0) and are shown on Table [1.](#page-3-1)

Table 1. Acquisition settings for CBCT.

Clinical information such as the [GS,](#page-0-0) [PSA](#page-0-0) levels, TNM and also staging, when available, was collected. The dataset was grouped following a 3-fold [GS](#page-0-0) risk group stratification as proposed by Epstein et al. [\[5\]](#page-12-4). The selected subset included only patients classified as intermediate risk. The idea was to develop a tool capable of distinguishing favourable and unfavourable clinical outcomes and also a baseline for a [EBRT](#page-0-0) effectiveness assessment. Following these criteria, this study included 22 patients with a favourable outcome $(GS = 3 + 4$ $(GS = 3 + 4$ and $GG = 2)$ $GG = 2)$ and 24 patients with an unfavourable outcome $(GS = 4 + 3$ and $GG = 3$ $GG = 3$, as shown in Table [2](#page-3-2) (in bold font).

Table 2. Patients Stratification.

GS RG		GG # of Cases	
$3+3$ Low/very low			
3+4 Intermediate (favourable)		22	
4+3 Intermediate (unfavourable)		24	
$4+4$ High		14	
$4+5/5+4$ Very high	5		

3.2. Image Registration

In [EBRT,](#page-0-0) in the treatment planning stage, tumor and tissue related volumes are defined by the [International Commission on Radiation Units and Measurements \(ICRU\).](#page-0-0) The [Gross](#page-0-0) [Tumor Volume \(GTV\)](#page-0-0) is the gross demonstrable extent and location of the tumor which may also include metastatic regional nodes and distant metastasis if they are indistinguishable from the primary tumor. The [Clinical Target Volume \(CTV\)](#page-0-0) is a volume that contains a [GTV](#page-0-0) and a margin that reflects the probability of subclinical disease occurrence. The prescribed dose must be delivered to the [CTV,](#page-0-0) plus a clinically acceptable margin that may include organ motion and setup variations [\[28\]](#page-13-14).

The initial [CT](#page-0-0) scan is essential for the [EBRT](#page-0-0) planning systems to provide a baseline for volume delineation and the [HU](#page-0-0) values needed for dose estimations. For [PCa,](#page-0-0) an [MRI](#page-0-0) or [PET](#page-0-0) can also be considered in this task. All the volumes were drawn manually, or using semi-automatic tools from the available [EBRT](#page-0-0) planning system at the institution, by medical experts. During the treatment, a [CBCT](#page-0-0) is usually acquired for patient positioning verification. In other words, to verify that the prostate is within the [CTV.](#page-0-0) This visual inspection is validated by a medical doctor. In this work, the included [CBCT](#page-0-0) was the one from the first treatment session.

To transpose the structures defined in the [CT](#page-0-0) to the [CBCT,](#page-0-0) an elastic registration was performed using the Elastix toolbox [\[29](#page-13-15)[,30\]](#page-13-16) available as an extension from 3DSlicer [\[31\]](#page-13-17). The fixed volume was the [CT,](#page-0-0) while the moving volume was the [CBCT.](#page-0-0) The extension computed the displacement field which is then applied to the [CBCT](#page-0-0) to transform the volume. Figure [2a](#page-4-0) shows an example [CT](#page-0-0) image, and Figure [2b](#page-4-0) the registered [CBCT](#page-0-0) and the manually defined [CTV](#page-0-0) structure on both.

Figure 2. Initial [CT](#page-0-0) scan with manually drawn prostate (yellow) and registered [CBCT.](#page-0-0) (**a**) Initial [CT](#page-0-0) scan. (**b**) First [EBRT](#page-0-0) session [CBCT.](#page-0-0)

3.3. Feature Extraction

The extraction of radiomic features from the [CTV](#page-0-0) was performed using the python library pyradiomics [\[10\]](#page-12-9), a highly tested and maintained open-source platform and also available as an extension from 3DSlicer. Most PyRadiomics features are in compliance with the [Image Biomarker Standardisation Initiative \(IBSI\),](#page-0-0) an independent international collaboration that aims at standardizing the extraction of image biomarkers for highthroughput quantitative image analysis (radiomics) [\[32\]](#page-13-18). A total of 107 features were extracted volume-wise with the default settings: only the original images (no filter applied), minimum [Region Of Interest \(ROI\)](#page-0-0) dimensions of 2, a pad distance of 5, a bin width of 25 and a cubic voxel size of 1 mm, since the voxel size will vary as it depends on the acquisition settings of each [LINAC,](#page-0-0) as shown in Table [1.](#page-3-1) Table [3](#page-4-1) shows the radiomic feature classes extracted from the dataset.

Table 3. Extracted radiomics feature classes.

The extracted features were then saved to a tab-separated values file for later processing in a python environment.

3.4. Feature Selection

For high-dimensional datasets, feature selection plays a crucial role, improving performance and estimators accuracy scores [\[33\]](#page-13-19). Current radiomic studies use several feature selection methods for model building. In this study, seven of the most used methods found in the literature were selected to build a classification pipeline for radiomics in [CBCT.](#page-0-0)

The variance threshold provides a baseline approach by removing all zero-variance features. Univariate methods were also used by several authors such as Bernatz et al. [\[18\]](#page-13-20), Li et al. [\[19\]](#page-13-6), Bleker et al. [\[21\]](#page-13-4), Bourbonne et al. [\[34\]](#page-14-0). Cysouw et al. [\[24\]](#page-13-10), Chen et al. [\[35\]](#page-14-1), who also used [Analysis Of Variance \(ANOVA\)](#page-0-0) method with good results. Another one is the [Recursive Feature Elimination \(RFE\)](#page-0-0) with an [SVM](#page-0-0) estimator [\[16,](#page-13-5)[36\]](#page-14-2). The goal of [RFE](#page-0-0) is to select features by recursively considering smaller and smaller sets [\[33\]](#page-13-19). An approach also evaluated is the introduction of cross-validation in the [RFE.](#page-0-0) A different approach is to select the features that maximize an estimator's metric (selected from the model). Wildeboer et al. [\[37\]](#page-14-3) considered an [SVM](#page-0-0) and Abdollahi et al. [\[38\]](#page-14-4) a [Linear Regression \(LR\)](#page-0-0) model. The selected feature selection methods and used parameters during training are shown in Table [4.](#page-5-0)

Table 4. Evaluated feature selection methods.

To implement these methods, scikit-learn library was used [\[33\]](#page-13-19) and the chosen parameters are the default ones. Each of the feature selection methods was evaluated with different classifiers (see Section [3.5\)](#page-5-1) in multiple pipelines. The idea is not to evaluate the best feature selection method or classifier but the pipeline or pipelines that best suit this particular dataset and the task of distinguishing favourable/unfavourable prognoses for [EBRT](#page-0-0) [PCa](#page-0-0) patients from [CBCT](#page-0-0) images. Furthermore, no parameter optimization was performed but that will be considered for future work.

3.5. Model Building

The number of extracted features can increase dramatically in radiomics and can even surpass the number of samples, thereby reducing effectiveness and increasing the probability of an overfitting scenario. Thus, feature selection is critical, but once features are chosen or recombined, the classifier or prediction model is ready to be developed.

The most used methods are [SVM](#page-0-0) [\[16–](#page-13-5)[18](#page-13-20)[,20](#page-13-7)[,37,](#page-14-3)[39](#page-14-5)[–43\]](#page-14-6) and [LR](#page-0-0) [\[12,](#page-13-0)[15](#page-13-3)[,17,](#page-13-21)[19](#page-13-6)[,35,](#page-14-1)[36](#page-14-2)[,41,](#page-14-7) [42](#page-14-8)[,44](#page-14-9)[,45\]](#page-14-10), followed by [Random Forest \(RF\)](#page-0-0) [\[17,](#page-13-21)[18,](#page-13-20)[21,](#page-13-4)[35,](#page-14-1)[38,](#page-14-4)[40,](#page-14-11)[41,](#page-14-7)[43\]](#page-14-6). Castillo T et al. [\[41\]](#page-14-7), Stanzione et al. [\[43\]](#page-14-6) also included [Bayesian Network \(BN\)](#page-0-0) estimators while Woźnicki et al. [\[17\]](#page-13-21), Bleker et al. [\[21\]](#page-13-4) used [Extreme Gradient Boosting \(XGB\).](#page-0-0) Finally, Abdollahi et al. [\[38\]](#page-14-4), Stanzione et al. [\[43\]](#page-14-6) used [Tree Based \(TB\)](#page-0-0) and [K-nearest Neighbors \(KNN\)](#page-0-0) classifiers, and the only approach using a [Neural Network \(NN\)](#page-0-0) was from Bernatz et al. [\[18\]](#page-13-20). In order to add more diversity, a bagging strategy was applied with a [Support Vector Classifier](#page-0-0) [\(SVC\)](#page-0-0) and a [TB](#page-0-0) estimator (bagging fits the base classifier on random subsets and aggregates predictions [\[33\]](#page-13-19)). Table [5](#page-6-1) shows the evaluated 14 estimators considered.

Table 5. Evaluated Classifiers.

The chosen parameters are the default ones provided by the scikit-learn library. To build the pipelines, features were first standardized (removing the mean and scaling to unit variance calculated on the training dataset). Each of the seven feature selection methods was combined with each of the 14 classifiers for a total of 98 classification pipelines. For comparison, the [AUROC,](#page-0-0) accuracy scores and corresponding standard deviations were computed following a stratified (in order to preserve class distribution) 5-fold cross validation scheme and a training/validation split of 0.75/0.25. Figure [3](#page-6-2) summarizes the followed methodology.

Figure 3. Pipeline evaluation flowchart.

4. Results and Discussion

The evaluation of the 98 pipelines was performed in a python environment, computing the [AUROC](#page-0-0) and accuracy scores. Figure [4](#page-7-0) shows the obtained [AUROC.](#page-0-0) Figure [5](#page-7-1) shows the obtained accuracy scores, and both present the corresponding mean standard deviations for the five fold cross-validation scheme (lighter colors mean a higher [AUROC](#page-0-0) value as indicated in the color bar scale).

The pipelines were built with a very specific subset and goal - to distinguish favourable and unfavourable cases from [PCa](#page-0-0) patients classified as intermediate risk. The specificity of this approach may provide [EBRT](#page-0-0) with a tool capable of monitoring the true effectiveness of the treatment. An initial unfavourable outcome may become, during treatment, a favourable case, possibly leading to adjustments in the treatment workflow.

From the obtained results, a few pipelines do present good performance. In radiomic studies, there is always an issue with the reproducibility of the features. In the future, other [CBCTs](#page-0-0) of each patient will be included in order to overcome this issue, as already performed by Bosetti et al. [\[12\]](#page-13-0).

Figure 4. ROC values with a five fold-CV.

Still, results seem to suggest that some classifiers are not suited to this particular task. The HistGradientBoosting obtained an [AUROC](#page-0-0) of 0.50 for every feature selection method. From the evaluated feature selection methods, the KBest (ANOVA) and RFECV (SVR) provided poor performances. On the other hand, the percentile feature selection method seems to have an overall decent performance, obtaining its best results when combined with an AdaBoost classifier with an [AUROC](#page-0-0) of 0.79 ± 0.27 and its worst when combined with an [LR](#page-0-0) classifier with an [AUROC](#page-0-0) of 0.72 ± 0.25 .

Considering a threshold value of [AUROC](#page-0-0) of 0.79, six pipelines were capable of obtaining good performance. Selecting features from an [LR](#page-0-0) model and combining it with a Bagging (SVC) classifier or GaussianNB provided a pipeline with an [AUROC](#page-0-0) value of 0.82 ± 0.18 and 0.79 ± 0.17 , respectively. Furthermore, the univariate selection method combined with an SVC obtained an [AUROC](#page-0-0) of 0.80 ± 0.13 and, with an ExtraTrees, of 0.79 ± 0.21 . The Adaboost classifier combined with the baseline feature selection method, the variance threshold, provided an [AUROC](#page-0-0) of 0.80 ± 0.14 , and when combined with the percentile feature selection method, an [AUROC](#page-0-0) of 0.79 ± 0.27 . Table [6](#page-8-0) highlights the selected pipelines obtained results.

Table 6. Selected pipelines results ordered by [AUROC.](#page-0-0)

The presented values are the mean values obtained for the five folds in the crossvalidation. For these six pipelines, a deeper analysis was performed in order to evaluate the performance of each. Figure [6](#page-8-1) presents the [AUROC](#page-0-0) curves and corresponding values for each fold as well as the mean value. Furthermore, in grey, are the ± 1 standard deviation curves and, in dashed red, the 0.5 [AUROC](#page-0-0) line.

Figure 6. ROC curves obtained for the selected pipelines.

In binary classification models, other metrics may provide valuable information on the performance of a classifier. The precision is defined as a ratio of the number of true positives divided by the sum of true positives and false positives. It is also referred to as the positive predictive power, this is, the ability of the model to predict true positives, which in this work, are the unfavourable cases $(GG = 3)$ $(GG = 3)$. The recall (sensitivity) is calculated as the ratio of the number of true positives divided by the sum of true positives and false negatives. The f1-score is the harmonic mean of the precision and recall, while the support is the number of occurrences of each class in the ground truth labels [\[33\]](#page-13-19). Table [7](#page-9-0) presents these parameters for the selected pipelines and the mean number of features selected in each fold in the cross-validation.

Selector	Classifier	Class	Precision	Recall	f1-Score	Support	Features
Model (LR)	Bagging (SVC)	2	$0.90 + 0.20$	$0.64 + 0.16$	$0.73 + 0.16$	4.40 ± 0.49	43
		3	$0.74 + 0.10$	$0.92 + 0.16$	$0.82 + 0.12$	4.80 ± 0.40	
Univariate	SVC	2	$0.68 + 0.17$	$0.64 + 0.24$	0.65 ± 0.20	$4.40 + 0.49$	20
		3	$0.71 + 0.17$	0.75 ± 0.08	$0.73 + 0.12$	$4.80 + 0.40$	
Variance threshold	AdaBoost	2	$0.70 + 0.22$	$0.64 + 0.24$	$0.65 + 0.20$	$4.40 + 0.49$	107
		3	$0.72 + 0.16$	$0.76 + 0.15$	$0.73 + 0.12$	$4.80 + 0.40$	
Model (LR)	Gaussian NB	2	$0.81 + 0.19$	$0.64 + 0.16$	$0.70 + 0.14$	$4.40 + 0.49$	43
		3	$0.72 + 0.09$	$0.83 + 0.15$	$0.77 + 0.10$	$4.80 + 0.40$	
Univariate	ExtraTrees	2	$0.85 + 0.20$	$0.64 + 0.16$	$0.71 + 0.15$	$4.40 + 0.49$	20
		3	$0.73 + 0.10$	$0.88 + 0.16$	$0.79 + 0.11$	$4.80 + 0.40$	
	AdaBoost	2	$0.80 + 0.22$	$0.82 + 0.22$	$0.79 + 0.19$	4.40 ± 0.49	11
Percentile		3	0.84 ± 0.20	$0.80 + 0.22$	$0.81 + 0.19$	4.80 ± 0.40	

Table 7. Best pipelines' performance parameters.

The threshold $= 0$, in the variance threshold method, is not enough to perform any feature selection because the preprocessing standardization removes the mean and scales features to unit variance. The AdaBoost classifier fits additional copies on the same dataset and re-adjusts the weights accordingly. This behaviour may overcome the lack of feature selection when both are combined. Besides the percentile–Adaboost combination, most pipelines present a low recall value for Class 2 (favourable), returning very few results. Themodel (LR)-bagging (SVC) pipeline has a high precision for Class 3 (unfavourable), suggesting those few results are well classified. This combination, however, has the opposite behaviour for Class 3. A high recall returns many results, but a low precision means those results are poorly classified.

The bagging (SVC) classifier aggregates the predictions of several [SVCs,](#page-0-0) reducing the variance of the final output and improving accuracy. When using an [SVC](#page-0-0) classifier, we obtained an accuracy of 0.0 ± 0.15 , but with a bagging strategy of 0.78 ± 0.14 . The GaussianNB classifier assumes a Gaussian likelihood with a naive assumption of pair-wise features' conditional independence. By reducing the number of features to 43, we are also eliminating highly correlated features, a factor that degrades the classifier performance. The decision tree creates a piecewise constant approximation to the decision curve, but when using the entire feature set, the set is known to provide some overfitting. The ExtraTrees introduces randomized decision trees on several subsets allowing control of the overfitting and increasing accuracy [\[33\]](#page-13-19).

percentile feature selection method with an AdaBoost classifier, the obtained results seem to be satisfactory, with relatively high values of precision and recall for both classes. The main advantage of this model is that the number of features used for classification is reduced to 11. This may be a step further in providing explainability and interpretability. In fact, the selected features in each fold of the cross-validation varies, although some are frequently selected. Figure [7](#page-10-1) shows the features that were more frequently selected.

Figure 7. Selected features frequency.

All evaluated feature selection methods select the skewness. Complexity features are selected using a univariate or percentile approach, while the zone variance, business and surface to volume ratio are selected when learning from an [LR](#page-0-0) model. The percentile-AdaBoost pipeline is used the complexity and skewness features in the cross-validation. Increasing the number of folds in the cross-validation scheme may provide more valuable insights.

5. Conclusions

For [PCa,](#page-0-0) [EBRT](#page-0-0) is a curative option for localized and locally advanced disease and a palliative option for metastatic low-volume disease [\[6\]](#page-12-5). Currently, the only triggers for recurrence or treatment effectiveness monitoring are the [PSA](#page-0-0) blood test or redoing a [Transrectal Ultrasound Guided Biopsy \(TRUS\).](#page-0-0) With radiomics, a quantitative analysis of medical images may have similar prognostic power to phenotypes and gene protein signatures $[9]$. Interest in radiomics has been increasing and for [PCa,](#page-0-0) it has been mainly focused on [MRI](#page-0-0) in the initial staging and grading. However, during the [EBRT,](#page-0-0) [CBCTs](#page-0-0) are freely available, as they are used for patient positioning and setup verifications.

The value of [CBCT-](#page-0-0)based radiomics was evaluated to distinguish between favourable and unfavourable prognosis for patients initially classified as intermediate risk. Such a tool may provide added value to monitor and trigger possible changes in [EBRT](#page-0-0) outcomes. Following the current methods of feature selection and classification for [PCa](#page-0-0) radiomics, 98 pipelines were evaluated. The results seem to suggest that selecting features from an [LR](#page-0-0) model, combined with a bagging (SVC) classifier, provided good performance. Although using 43 features, it lacks the potential to offer explainability. In this sense, a better approach seems to be using a percentile feature selection method and an AdaBoost classifier. This pipeline presents an [AUROC](#page-0-0) of 0.79 ± 0.27 and an accuracy of 0.80 ± 0.19 and high values of precision and recall, being the most balanced of the evaluated pipelines.

The skewness seems to be the most frequently selected feature, considering each fold in the cross-validation scheme. Although its true importance is yet to be evaluated, the fact it was selected in every fold of every feature selection method suggests it may provide some insights. Furthermore, the fact that only one [CBCT](#page-0-0) was considered for each patient did not allow the evaluation of features reproducibility.

Although the obtained results are promising, some improvements need to be made for a deeper evaluation. A grid-search cross-validation may provide fine-tuning of parameters and improved results. Furthermore, the used subset is quite small, and may benefit in the future from the inclusion of high-risk patients and the assessment of other models.

[CBCT-](#page-0-0)based radiomics may provide a baseline for an [EBRT](#page-0-0) effectiveness assessment framework on ongoing treatment, improving outcomes and lowering recurrence rates regardless of the several limitations.

Author Contributions: Conceptualization, B.M.; methodology, B.M. and I.D.; software, B.M.; validation, B.M., I.D. and J.S.; formal analysis, B.M.; investigation, B.M.; resources, B.M., I.D., F.D. and J.S.; data curation, B.M. and F.D.; writing—original draft preparation, B.M.; writing—review and editing, B.M., I.D., F.D. and J.S.; supervision, I.D. and J.S. All authors have read and agreed to the published version of the manuscript.

Funding: This research received no external funding.

Institutional Review Board Statement: The study was conducted according to the guidelines of the Declaration of Helsinki. The study was approved by IPO Porto Healthcare Ethics Committee (protocol code CES.274/020 and date of approval 1 October 2020.

Informed Consent Statement: Informed consent was obtained from all subjects involved in the study.

Data Availability Statement: No new data were created or analyzed in this study. Data sharing is not applicable to this article.

Conflicts of Interest: The authors declare no conflict of interest.

Abbreviations

The following abbreviations are used in this manuscript:

References

- 1. Sung, H.; Ferlay, J.; Siegel, R.L.; Laversanne, M.; Soerjomataram, I.; Jemal, A.; Bray, F. Global Cancer Statistics 2020: GLOBOCAN Estimates of Incidence and Mortality Worldwide for 36 Cancers in 185 Countries. *CA A Cancer J. Clin.* **2021**, *71*, 209–249. [\[CrossRef\]](http://doi.org/10.3322/caac.21660) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/33538338)
- 2. Singh, V. *Textbook of Anatomy: Abdomen and Lower Limb*; 3rd Updated Edition-EBook; Elsevier: New Delhi, India, 2020; Volume 2.
- 3. Humphrey, P.A. Histopathology of prostate cancer. *Cold Spring Harb. Perspect. Med.* **2017**, *7*, a030411. [\[CrossRef\]](http://dx.doi.org/10.1101/cshperspect.a030411) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/28389514)
- 4. DeMarzo, A.M.; Nelson, W.G.; Isaacs, W.B.; Epstein, J.I. Pathological and molecular aspects of prostate cancer. *Lancet* **2003**, *361*, 955–964. [\[CrossRef\]](http://dx.doi.org/10.1016/S0140-6736(03)12779-1) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/12648986)
- 5. Epstein, J.I.; Egevad, L.; Amin, M.B.; Delahunt, B.; Srigley, J.R.; Humphrey, P.A. The 2014 International Society of Urological Pathology (ISUP) consensus conference on Gleason grading of prostatic carcinoma. *Am. J. Surg. Pathol.* **2016**, *40*, 244–252. [\[CrossRef\]](http://dx.doi.org/10.1097/PAS.0000000000000530)
- 6. Parker, C.; Castro, E.; Fizazi, K.; Heidenreich, A.; Ost, P.; Procopio, G.; Tombal, B.; Gillessen, S. Prostate cancer: ESMO Clinical Practice Guidelines for diagnosis, treatment and follow-up. *Ann. Oncol.* **2020**, *31*, 1119–1134. . [\[CrossRef\]](http://dx.doi.org/10.1016/j.annonc.2020.06.011)
- 7. Schröder, F.H.; Kruger, A.B.; Rietbergen, J.; Kranse, R.; Maas, P.v.d.; Beemsterboer, P.; Hoedemaeker, R. Evaluation of the digital rectal examination as a screening test for prostate cancer. *J. Natl. Cancer Inst.* **1998**, *90*, 1817–1823. [\[CrossRef\]](http://dx.doi.org/10.1093/jnci/90.23.1817)
- 8. Klotz, L. Active surveillance for prostate cancer: For whom? *J. Clin. Oncol.* **2005**, *23*, 8165–8169. . [\[CrossRef\]](http://dx.doi.org/10.1200/JCO.2005.03.3134)
- 9. Gillies, R.J.; Kinahan, P.E.; Hricak, H. Radiomics: Images are more than pictures, they are data. *Radiology* **2016**, *278*, 563–577. [\[CrossRef\]](http://dx.doi.org/10.1148/radiol.2015151169)
- 10. Van Griethuysen, J.J.; Fedorov, A.; Parmar, C.; Hosny, A.; Aucoin, N.; Narayan, V.; Beets-Tan, R.G.; Fillion-Robin, J.C.; Pieper, S.; Aerts, H.J. Computational radiomics system to decode the radiographic phenotype. *Cancer Res.* **2017**, *77*, e104–e107. [\[CrossRef\]](http://dx.doi.org/10.1158/0008-5472.CAN-17-0339)
- 11. Mendes, B.; Domingues, I.; Silva, A.; Santos, J. Prostate Cancer Aggressiveness Prediction Using CT Images. *Life* **2021**, *11*, 1164. [\[CrossRef\]](http://dx.doi.org/10.3390/life11111164)
- 12. Bosetti, D.G.; Ruinelli, L.; Piliero, M.A.; van der Gaag, L.C.; Pesce, G.A.; Valli, M.; Bosetti, M.; Presilla, S.; Richetti, A.; Deantonio, L. Cone-beam computed tomography-based radiomics in prostate cancer: A mono-institutional study. *Strahlenther. Und Onkol.* **2020**, *196*, 943–951. [\[CrossRef\]](http://dx.doi.org/10.1007/s00066-020-01677-x)
- 13. Lambin, P.; Rios-Velazquez, E.; Leijenaar, R.; Carvalho, S.; Van Stiphout, R.G.; Granton, P.; Zegers, C.M.; Gillies, R.; Boellard, R.; Dekker, A.; et al. Radiomics: Extracting more information from medical images using advanced feature analysis. *Eur. J. Cancer* **2012**, *48*, 441–446. [\[CrossRef\]](http://dx.doi.org/10.1016/j.ejca.2011.11.036)
- 14. Yao, S.; Jiang, H.; Song, B. Radiomics in prostate cancer: Basic concepts and current state-of-the-art. *Chin. J. Acad. Radiol.* **2020**, *2*, 47–55. [\[CrossRef\]](http://dx.doi.org/10.1007/s42058-019-00020-3)
- 15. Min, X.; Li, M.; Dong, D.; Feng, Z.; Zhang, P.; Ke, Z.; You, H.; Han, F.; Ma, H.; Tian, J.; et al. Multi-parametric MRI-based radiomics signature for discriminating between clinically significant and insignificant prostate cancer: Cross-validation of a machine learning method. *Eur. J. Radiol.* **2019**, *115*, 16–21. [\[CrossRef\]](http://dx.doi.org/10.1016/j.ejrad.2019.03.010)
- 16. Hou, Y.; Bao, M.L.; Wu, C.J.; Zhang, J.; Zhang, Y.D.; Shi, H.B. A radiomics machine learning-based redefining score robustly identifies clinically significant prostate cancer in equivocal PI-RADS score 3 lesions. *Abdom. Radiol.* **2020**, *45*, 4223–4234. [\[CrossRef\]](http://dx.doi.org/10.1007/s00261-020-02678-1)
- 17. Woźnicki, P.; Westhoff, N.; Huber, T.; Riffel, P.; Froelich, M.F.; Gresser, E.; von Hardenberg, J.; Mühlberg, A.; Michel, M.S.; Schoenberg, S.O.; et al. Multiparametric MRI for prostate cancer characterization: Combined use of radiomics model with PI-RADS and clinical parameters. *Cancers* **2020**, *12*, 1767. [\[CrossRef\]](http://dx.doi.org/10.3390/cancers12071767)
- 18. Bernatz, S.; Ackermann, J.; Mandel, P.; Kaltenbach, B.; Zhdanovich, Y.; Harter, P.N.; Döring, C.; Hammerstingl, R.; Bodelle, B.; Smith, K.; et al. Comparison of machine learning algorithms to predict clinically significant prostate cancer of the peripheral zone with multiparametric MRI using clinical assessment categories and radiomic features. *Eur. Radiol.* **2020**, *30*, 6757–6769. [\[CrossRef\]](http://dx.doi.org/10.1007/s00330-020-07064-5)
- 19. Li, M.; Chen, T.; Zhao, W.; Wei, C.; Li, X.; Duan, S.; Ji, L.; Lu, Z.; Shen, J. Radiomics prediction model for the improved diagnosis of clinically significant prostate cancer on biparametric MRI. *Quant. Imaging Med. Surg.* **2020**, *10*, 368. [\[CrossRef\]](http://dx.doi.org/10.21037/qims.2019.12.06)
- 20. Bevilacqua, A.; Mottola, M.; Ferroni, F.; Rossi, A.; Gavelli, G.; Barone, D. The Primacy of High B-Value 3T-DWI Radiomics in the Prediction of Clinically Significant Prostate Cancer. *Diagnostics* **2021**, *11*, 739. [\[CrossRef\]](http://dx.doi.org/10.3390/diagnostics11050739)
- 21. Bleker, J.; Kwee, T.C.; Dierckx, R.A.; de Jong, I.J.; Huisman, H.; Yakar, D. Multiparametric MRI and auto-fixed volume of interest-based radiomics signature for clinically significant peripheral zone prostate cancer. *Eur. Radiol.* **2020**, *30*, 1313–1324. [\[CrossRef\]](http://dx.doi.org/10.1007/s00330-019-06488-y)
- 22. Abraham, B.; Nair, M.S. Computer-aided classification of prostate cancer grade groups from MRI images using texture features and stacked sparse autoencoder. *Comput. Med. Imaging Graph.* **2018**, *69*, 60–68. [\[CrossRef\]](http://dx.doi.org/10.1016/j.compmedimag.2018.08.006) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/30205334)
- 23. Algohary, A.; Shiradkar, R.; Pahwa, S.; Purysko, A.; Verma, S.; Moses, D.; Shnier, R.; Haynes, A.M.; Delprado, W.; Thompson, J.; et al. Combination of peri-tumoral and intra-tumoral radiomic features on bi-parametric MRI accurately stratifies prostate cancer risk: A multi-site study. *Cancers* **2020**, *12*, 2200. [\[CrossRef\]](http://dx.doi.org/10.3390/cancers12082200) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/32781640)
- 24. Cysouw, M.C.; Jansen, B.H.; van de Brug, T.; Oprea-Lager, D.E.; Pfaehler, E.; de Vries, B.M.; van Moorselaar, R.J.; Hoekstra, O.S.; Vis, A.N.; Boellaard, R. Machine learning-based analysis of [18 F] DCFPyL PET radiomics for risk stratification in primary prostate cancer. *Eur. J. Nucl. Med. Mol. Imaging* **2021**, *48*, 340–349. [\[CrossRef\]](http://dx.doi.org/10.1007/s00259-020-04971-z) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/32737518)
- 25. Alongi, P.; Stefano, A.; Comelli, A.; Laudicella, R.; Scalisi, S.; Arnone, G.; Barone, S.; Spada, M.; Purpura, P.; Bartolotta, T.V.; et al. Radiomics analysis of 18F-Choline PET/CT in the prediction of disease outcome in high-risk prostate cancer: An explorative study on machine learning feature classification in 94 patients. *Eur. Radiol.* **2021**, *31*, 4595–4605. [\[CrossRef\]](http://dx.doi.org/10.1007/s00330-020-07617-8) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/33443602)
- 26. Osman, S.O.; Leijenaar, R.T.; Cole, A.J.; Lyons, C.A.; Hounsell, A.R.; Prise, K.M.; O'Sullivan, J.M.; Lambin, P.; McGarry, C.K.; Jain, S. Computed tomography-based radiomics for risk stratification in prostate cancer. *Int. J. Radiat. Oncol. Biol. Phys.* **2019**, *105*, 448–456. [\[CrossRef\]](http://dx.doi.org/10.1016/j.ijrobp.2019.06.2504)
- 27. Nioche, C.; Orlhac, F.; Boughdad, S.; Reuzé, S.; Goya-Outi, J.; Robert, C.; Pellot-Barakat, C.; Soussan, M.; Frouin, F.; Buvat, I. LIFEx: A freeware for radiomic feature calculation in multimodality imaging to accelerate advances in the characterization of tumor heterogeneity. *Cancer Res.* **2018**, *78*, 4786–4789. [\[CrossRef\]](http://dx.doi.org/10.1158/0008-5472.CAN-18-0125)
- 28. ICRU. Prescribing, recording, and reporting photon-beam intensity-modulated radiation therapy (IMRT). *J. Int. Comm. Radiat. Units Meas. (JICRU)* **2010**, *10*, 41–53.
- 29. Klein, S.; Staring, M.; Murphy, K.; Viergever, M.A.; Pluim, J.P. Elastix: A toolbox for intensity-based medical image registration. *IEEE Trans. Med. Imaging* **2009**, *29*, 196–205. [\[CrossRef\]](http://dx.doi.org/10.1109/TMI.2009.2035616)
- 30. Shamonin, D.P.; Bron, E.E.; Lelieveldt, B.P.; Smits, M.; Klein, S.; Staring, M.; Initiative, A.D.N. Fast parallel image registration on CPU and GPU for diagnostic classification of Alzheimer's disease. *Front. Neuroinform.* **2014**, *7*, 50. [\[CrossRef\]](http://dx.doi.org/10.3389/fninf.2013.00050)
- 31. Fedorov, A.; Beichel, R.; Kalpathy-Cramer, J.; Finet, J.; Fillion-Robin, J.C.; Pujol, S.; Bauer, C.; Jennings, D.; Fennessy, F.; Sonka, M.; et al. 3D Slicer as an image computing platform for the Quantitative Imaging Network. *Magn. Reson. Imaging* **2012**, *30*, 1323–1341. [\[CrossRef\]](http://dx.doi.org/10.1016/j.mri.2012.05.001)
- 32. Zwanenburg, A.; Vallières, M.; Abdalah, M.A.; Aerts, H.J.; Andrearczyk, V.; Apte, A.; Ashrafinia, S.; Bakas, S.; Beukinga, R.J.; Boellaard, R.; et al. The image biomarker standardization initiative: Standardized quantitative radiomics for high-throughput image-based phenotyping. *Radiology* **2020**, *295*, 328. [\[CrossRef\]](http://dx.doi.org/10.1148/radiol.2020191145)
- 33. Pedregosa, F.; Varoquaux, G.; Gramfort, A.; Michel, V.; Thirion, B.; Grisel, O.; Blondel, M.; Prettenhofer, P.; Weiss, R.; Dubourg, V.; et al. Scikit-learn: Machine Learning in Python. *J. Mach. Learn. Res.* **2011**, *12*, 2825–2830. [\[CrossRef\]](http://dx.doi.org/10.48550/arXiv.1201.0490)
- 34. Bourbonne, V.; Fournier, G.; Vallières, M.; Lucia, F.; Doucet, L.; Tissot, V.; Cuvelier, G.; Hue, S.; Le Penn Du, H.; Perdriel, L.; et al. External validation of an MRI-derived radiomics model to predict biochemical recurrence after surgery for high-risk prostate cancer. *Cancers* **2020**, *12*, 814. [\[CrossRef\]](http://dx.doi.org/10.3390/cancers12040814)
- 35. Chen, A.; Zhu, L.; Zang, H.; Ding, Z.; Zhan, S. Computer-aided diagnosis and decision-making system for medical data analysis: A case study on prostate MR images. *J. Manag. Sci. Eng.* **2019**, *4*, 266–278. [\[CrossRef\]](http://dx.doi.org/10.1016/j.jmse.2020.01.002)
- 36. Toivonen, J.; Montoya Perez, I.; Movahedi, P.; Merisaari, H.; Pesola, M.; Taimen, P.; Boström, P.J.; Pohjankukka, J.; Kiviniemi, A.; Pahikkala, T.; et al. Radiomics and machine learning of multisequence multiparametric prostate MRI: Towards improved non-invasive prostate cancer characterization. *PLoS ONE* **2019**, *14*, e0217702. [\[CrossRef\]](http://dx.doi.org/10.1371/journal.pone.0217702)
- 37. Wildeboer, R.R.; van Sloun, R.J.; Huang, P.; Wijkstra, H.; Mischi, M. 3-D multi-parametric contrast-enhanced ultrasound for the prediction of prostate cancer. *Ultrasound Med. Biol.* **2019**, *45*, 2713–2724. [\[CrossRef\]](http://dx.doi.org/10.1016/j.ultrasmedbio.2019.05.017)
- 38. Abdollahi, H.; Mofid, B.; Shiri, I.; Razzaghdoust, A.; Saadipoor, A.; Mahdavi, A.; Galandooz, H.M.; Mahdavi, S.R. Machine learning-based radiomic models to predict intensity-modulated radiation therapy response, Gleason score and stage in prostate cancer. *La Radiol. Medica* **2019**, *124*, 555–567. [\[CrossRef\]](http://dx.doi.org/10.1007/s11547-018-0966-4)
- 39. Cuocolo, R.; Stanzione, A.; Faletti, R.; Gatti, M.; Calleris, G.; Fornari, A.; Gentile, F.; Motta, A.; Dell'Aversana, S.; Creta, M.; et al. MRI index lesion radiomics and machine learning for detection of extraprostatic extension of disease: A multicenter study. *Eur. Radiol.* **2021**, *31*, 7575–7583. [\[CrossRef\]](http://dx.doi.org/10.1007/s00330-021-07856-3)
- 40. Shiradkar, R.; Ghose, S.; Jambor, I.; Taimen, P.; Ettala, O.; Purysko, A.S.; Madabhushi, A. Radiomic features from pretreatment biparametric MRI predict prostate cancer biochemical recurrence: Preliminary findings. *J. Magn. Reson. Imaging* **2018**, *48*, 1626–1636. [\[CrossRef\]](http://dx.doi.org/10.1002/jmri.26178)
- 41. Castillo T, J.M.; Starmans, M.P.; Arif, M.; Niessen, W.J.; Klein, S.; Bangma, C.H.; Schoots, I.G.; Veenland, J.F. A multi-center, multi-vendor study to evaluate the generalizability of a radiomics model for classifying prostate cancer: High grade vs. low grade. *Diagnostics* **2021**, *11*, 369. [\[CrossRef\]](http://dx.doi.org/10.3390/diagnostics11020369)
- 42. Murakami, Y.; Magome, T.; Mizutani, T.; Sato, T.; Yoshioka, Y.; Oguchi, M. Potential of Radiomic Feature Related to Prostatic Calcifications for the Machine Learning-Based Prediction of Biochemical Recurrence in Prostate Cancer Patient. *Int. J. Radiat. Oncol. Biol. Phys.* **2019**, *105*, E137. [\[CrossRef\]](http://dx.doi.org/10.1016/j.ijrobp.2019.06.2176)
- 43. Stanzione, A.; Cuocolo, R.; Cocozza, S.; Romeo, V.; Persico, F.; Fusco, F.; Longo, N.; Brunetti, A.; Imbriaco, M. Detection of extraprostatic extension of cancer on biparametric MRI combining texture analysis and machine learning: Preliminary results. *Acad. Radiol.* **2019**, *26*, 1338–1344. [\[CrossRef\]](http://dx.doi.org/10.1016/j.acra.2018.12.025) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/30655050)
- 44. Xu, M.; Fang, M.; Zou, J.; Yang, S.; Yu, D.; Zhong, L.; Hu, C.; Zang, Y.; Dong, D.; Tian, J.; et al. Using biparametric MRI radiomics signature to differentiate between benign and malignant prostate lesions. *Eur. J. Radiol.* **2019**, *114*, 38–44. [\[CrossRef\]](http://dx.doi.org/10.1016/j.ejrad.2019.02.032) [\[PubMed\]](http://www.ncbi.nlm.nih.gov/pubmed/31005174)
- 45. Liang, L.; Zhi, X.; Sun, Y.; Li, H.; Wang, J.; Xu, J.; Guo, J. A Nomogram Based on a Multiparametric Ultrasound Radiomics Model for Discrimination between Malignant and Benign Prostate Lesions. *Front. Oncol.* **2021**, *11*, 290. [\[CrossRef\]](http://dx.doi.org/10.3389/fonc.2021.610785)

Disclaimer/Publisher's Note: The statements, opinions and data contained in all publications are solely those of the individual author(s) and contributor(s) and not of MDPI and/or the editor(s). MDPI and/or the editor(s) disclaim responsibility for any injury to people or property resulting from any ideas, methods, instructions or products referred to in the content.