

*Supplementary Materials*

# Scalable Functionalization of Polyaniline-Grafted rGO Field-Effect Transistors for a Highly Sensitive Enzymatic Acetylcholine Biosensor

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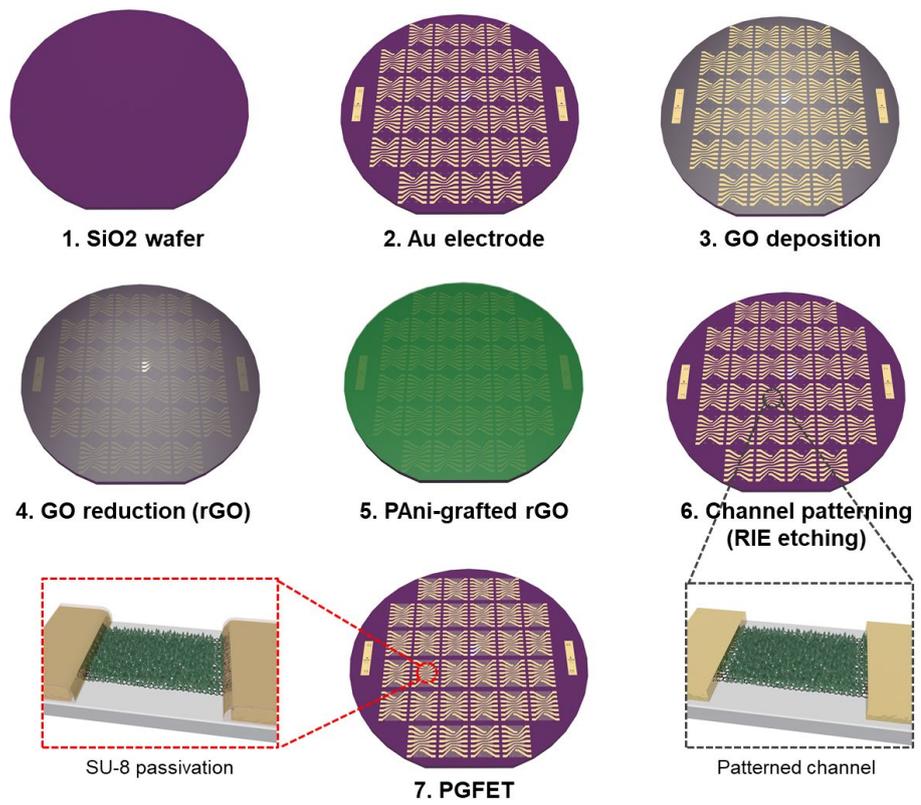
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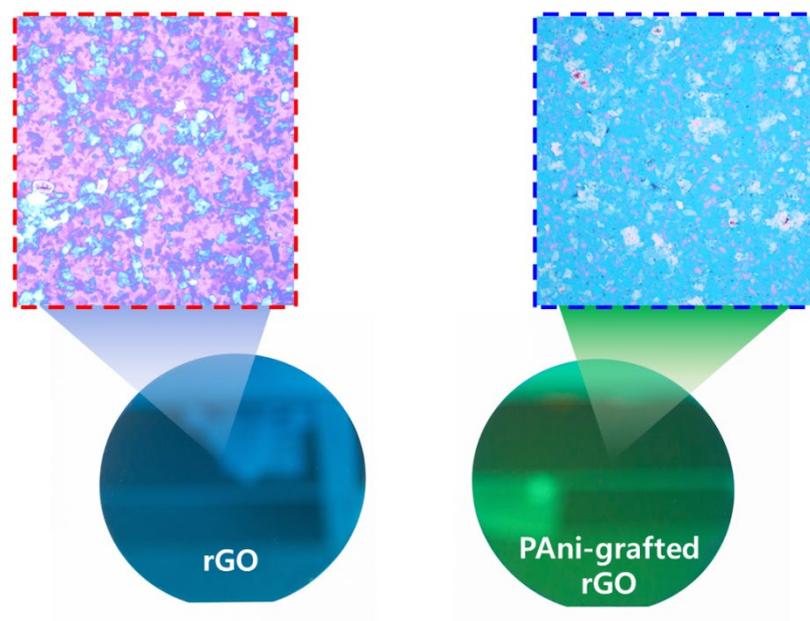
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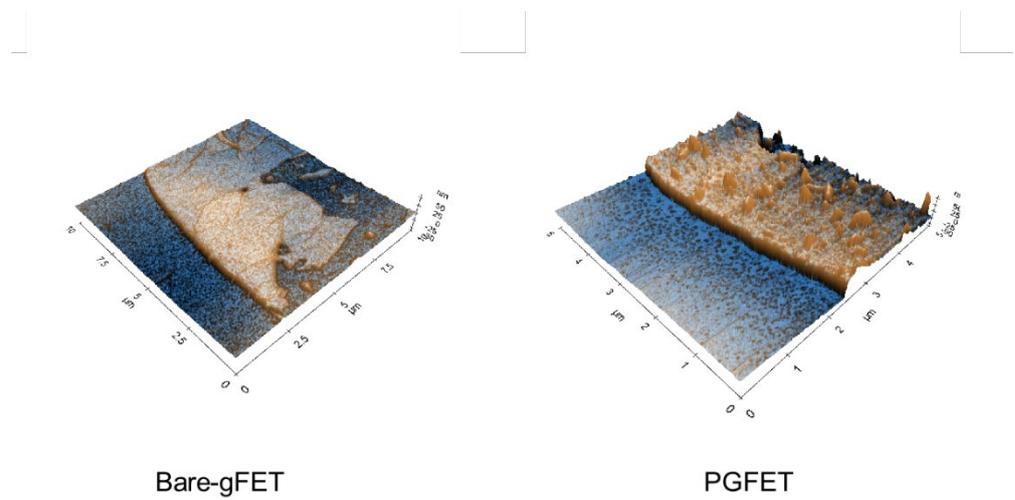
† These authors contributed equally to this work.



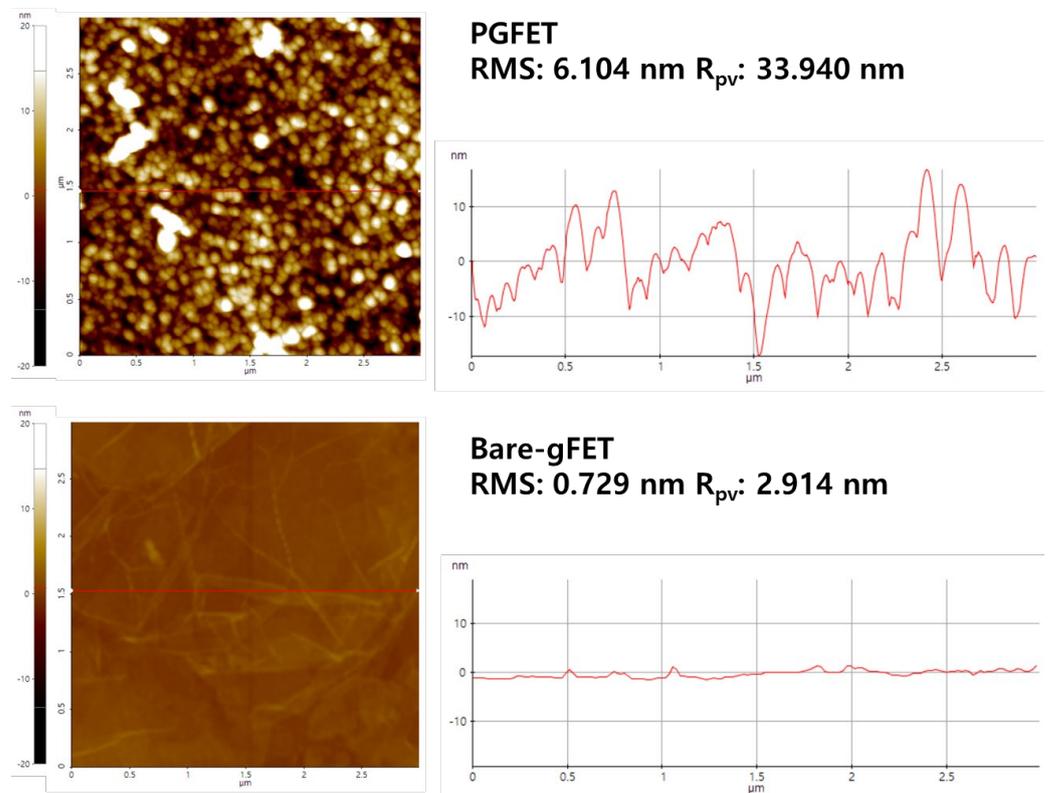
**Figure S1.** The wafer-scale fabrication procedure of PGFET.



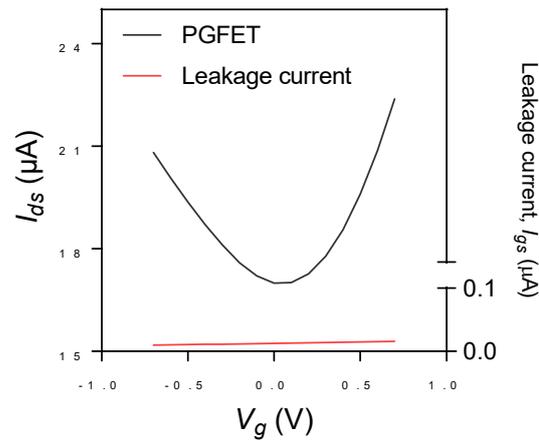
**Figure S2.** The photographic images of rGO and PANi-grafted rGO deposited on 4 in. wafers. The magnified images of rGO (red) and PANi-grafted rGO showing completely covered the rGO surface.



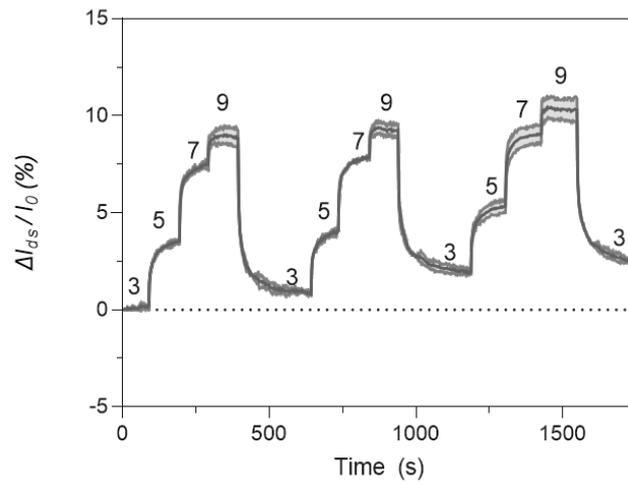
**Figure S3.** Three-dimensional AFM images of bare-gFET and PGFET.



**Figure S4.** Comparison of morphologies of PGFET and bare-gFET. AFM image and surface roughness of PGFET and bare-gFET. (RMS, rms surface roughness,  $R_{pv}$ , peak-to-valley roughness).



**Figure S5.** Comparison between leakage current and the source-drain current of PGFET with varying the gate voltage ( $V_g$ ), representing that leakage current is negligible ( $\sim 27$  nA).



**Figure S6.** The real-time output responses of bare-gFETs for three pH cycles.

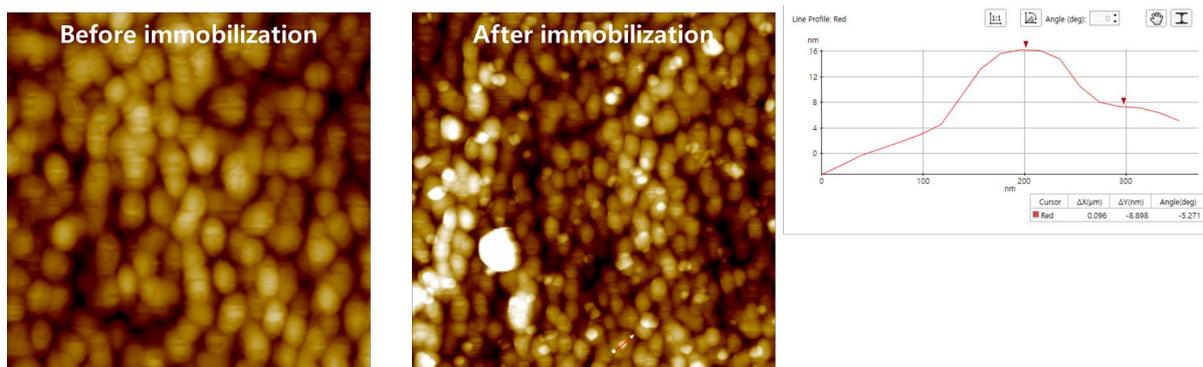


Figure S7. The AFM images of before and after AchE immobilization on PGFET surface.

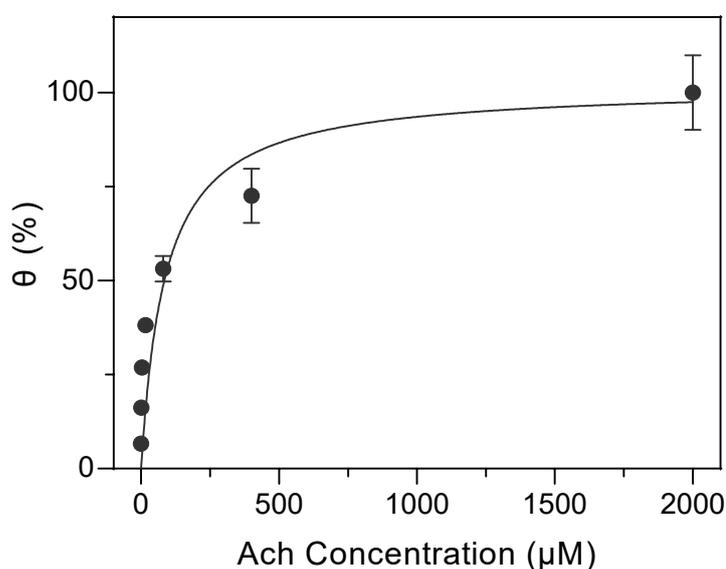


Figure S8. Fitting of the AchE activity to a Michaelis-Menten kinetics model.

The changes in  $\Delta I_{ds}/I_0$  were also fitted to a thermodynamic model to investigate the enzymatic kinetics of AchE immobilized on the PGFET. The Hill equation is as follows:

$$\theta = \frac{[S]^n}{(K_D)^n + [S]^n}$$

where  $K_D$  is the dissociation constant,  $S$  is the substrate concentration, and  $n$  is the Hill coefficient, which describes the fractional saturation of the process. When  $n=1$ , the Hill equation equals Michaelis–Menten kinetics, the most well-known model for enzymatic reactions, and  $K_D$  equals the Michaelis–Menten constant ( $K_M$ ), which is the concentration of substrate providing half of enzyme maximal activity. The quantified enzymatic responses of PGFET were fitted to Michaelis-Menten kinetics between  $\theta$  and the concentration of Ach.

**Table S1.** Comparison of the analytical parameters of the PGFET and other recently reported biosensors for Ach detection.

Sensor type	Detection range ( $\mu\text{M}$ )	LOD ( $\mu\text{M}$ )	Sensitivity	Measurement setup	Comments	Ref.
rGO-FET	1-10000	1	13.9 mV/Ach dec	$V_{ds} = 10\text{mV}$ , $V_g = 1.0$ to $-1.0$ V	Dirac point shift, static conditions	[1]
rGO-FET	100-10000	100	1.06 ( $\Delta G/G_{min}$ )/Ach dec	$V_{ds} = 100$ mV, $V_g = -200$ mV	Flow conditions	[2]
rGO-FET	5-1000	2.3	$-850 \mu\text{A}/\text{cm}^2$ Ach dec	$V_{ds} = 100$ mV, $V_g = -200$ mV	Flow conditions	[3]
Organic electrochemical transistor	5-14	5	4.1 A/M $\text{cm}^2$	$V_{ds} = -200$ mV, $V_g = 400$ mV	Flow conditions	[4]
rGO-FET	0.108-2000	0.0723	1.34%/Ach dec (The relative changes in the source-drain current)	$V_{ds} = 100$ mV, $V_g = -300$ mV	Thermostatic, flow conditions	This work

## References

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