



# *Article* **KOC\_Net: Impact of the Synthetic Minority Over-Sampling Technique with Deep Learning Models for Classification of Knee Osteoarthritis Using Kellgren–Lawrence X-Ray Grade**

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**Abstract:** One of the most common diseases afflicting humans is knee osteoarthritis (KOA). KOA occurs when the knee joint cartilage breaks down, and knee bones start rubbing together. The diagnosis of KOA is a lengthy process, and missed diagnosis can have serious consequences. Therefore, the diagnosis of KOA at an initial stage is crucial which prevents the patients from Severe complications. KOA identification using deep learning (DL) algorithms has gained popularity during the past few years. By applying knee X-ray images and the Kellgren–Lawrence (KL) grading system, the objective of this study was to develop a DL model for detecting KOA. This study proposes a novel model based on CNN called knee osteoarthritis classification network (KOC\_Net). The KOC\_Net model contains 05 convolutional blocks, and each convolutional block has three components such as Convlotuioanl2D, ReLU, and MaxPooling 2D. The KOC\_Net model is evaluated on two publicly available benchmark datasets which consist of X-ray images of KOA based on the KL grading system. Additionally, we applied contrast-limited adaptive histogram equalization (CLAHE) methods to enhance the contrast of the images and utilized SMOTE Tomek to deal with the problem of minority classes. For the diagnosis of KOA, the classification performance of the proposed KOC\_Net model is compared with baseline deep networks, namely Dense Net-169, Vgg-19, Xception, and Inception-V3. The proposed KOC\_Net was able to classify KOA into 5 distinct groups (including Moderate, Minimal, Severe, Doubtful, and Healthy), with an AUC of 96.71%, accuracy of 96.51%, recall of 91.95%, precision of 90.25%, and F1-Score of 96.70%. Dense Net-169, Vgg-19, Xception, and Inception-V3 have relative accuracy rates of 84.97%, 81.08%, 87.06%, and 83.62%. As demonstrated by the results, the KOC\_Net model provides great assistance to orthopedics in making diagnoses of KOA.

**Keywords:** image processing; deep learning; KOA; X-ray; Kellgren–Lawrence

**JEL Classification:** 68T07

### **1. Introduction**

According to the World Health Organization (WHO), knee osteoarthritis (KOA) will affect one out of every three people in their lives [\[1,](#page-29-0)[2\]](#page-29-1). Over half of those over the age of 65 show symptoms of KOA, and it is not just in that one joint. By 2030, nearly one in four Americans will be at least 65 years old, putting them at increased risk of getting KOA [\[3\]](#page-29-2). The existence of KOA impacts the quality of life of older people. No medication has yet developed that can slow or prevent the progression of the degenerative structural changes that define KOA.



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KOA early detection and treatment carry some risks, but it also can improve patients' quality of life and delay the disease's growth. The main symptoms of KOA are joint space narrowing (JSN), subchondral sclerosis, and osteophyte formation. The MRI scans show the 3D structure of the knee joint. WHO standards eventually resulted in the development of the Kellgren and Lawrence (KL) severity grading system in 1961 [\[4\]](#page-29-3). According to the KL system, the degree of KOA is ranked from 0 to 4.

It is impossible to make an accurate diagnosis without the experience and care of a trained medical professional [\[5\]](#page-29-4). In addition to this, the KL grading system leaves a lot of space for individual interpretation. Osteophyte lipping and minimal risk of JSN are two of the criteria for KL Grade 1. The same doctor can assign multiple grades of knee flexibility to the same knee joint at different times. According to the findings of the study [\[5\]](#page-29-4), the inter-rater reliability for KL falls somewhere in the range of 0.67 and 0.73. According to [\[6\]](#page-29-5), the KL grade standard introduces a lack of clarity, which makes physicians' evaluations of the knee joint less accurate than they could be.

There is a potential for deliberately increasing the grade of a knee joint in four levels (Grade 1 to Grade 4). Mean absolute error (MAE) was used in evaluating the accuracy of age predictions and was an additional measure that can be used to categorize the degree of knee KL [\[7\]](#page-29-6). The growing incidence of KOA makes accurate diagnosis and assessment of its severity all the more important.

Automatic knee severity assessment maintains accuracy over time and may provide more objective and trustworthy estimates than human experts. The severity of KOA can be predicted using knee joint X-rays alone, but only if the knee joint is first recognized and then classified into one of five KL groups. KL grade classification and knee joint recognition algorithms have been developed in recent years. For the most accurate identification of knee joints, the study [\[8\]](#page-29-7) utilizes a sliding window strategy in conjunction with a templatematching technique. After being overlaid on the existing X-ray image, a total of 20 images of the knee joint, each consisting of  $15 \times 15$  pixels, are measured for their Euclidean distances from one another. When one looks out the window, the Euclidean distance to the knee joint that is the shortest that is possible found  $[9,10]$  $[9,10]$  uses a linear support vector machine (SVM) to identify knee joints by looking at features found in Sobel vertical image gradients. These gradients are made by the horizontal edges in images of knee joints [\[11\]](#page-29-10).

First, the identification of the knee joint region is offered in a study [\[12\]](#page-29-11). They experience a peak intensity at the patella, followed by a sharp drop down at the femur and tibia. A linear SVM classifier employing a Histogram of Oriented Gradients (HOG) features [\[13\]](#page-29-12) is given the knee joint predictions. An innovative deep neural network (DNN)-based method for knee joint identification is described by [\[14\]](#page-29-13). The method achieves state-of-the-art standards in terms of performance [\[8,](#page-29-7)[15\]](#page-29-14). According to the findings presented in [\[15\]](#page-29-14), the assignment of KL grades is observed as a challenging regression task. The BVLC\_Net has been optimized for knee KL grade categorization using the mean squared loss. Moreover, a novel CNN model with improved accuracy by including cross-entropy and mean-squared losses [\[16\]](#page-29-15), they designed a CNN technique known as deep siamese. This tool was designed to isolate certain areas around the knee and combine their predictions.

Deep learning (DL) algorithms are capable of obtaining a wide variety of visual tasks, including object detection, segmentation, and classification [\[17\]](#page-30-0). DL models have been utilized for a wide range of medical image analysis. These tasks include cell detection and segmentation [\[18\]](#page-30-1), mitosis detection [\[19\]](#page-30-2), white matter lesion detection [\[17](#page-30-0)[–19\]](#page-30-2), and retinal blood vessel recognition and segmentation [\[20\]](#page-30-3).

The Severe complications of KOA are on the rise, patients have an approx. 95% chance of recovering if they are recognized and treated quickly. This motivates us to develop an automatic KOA identification model at an initial stage. Therefore, this study introduces a novel CNN model for the classification of KOA using a knee severity grading system named the knee osteoarthritis classification network (KOC\_Net). This KOC\_Net classifies cases of KOA according to the KL severity grading system, which includes five grades (ranging from Healthy, Doubtful, Minimal, Moderate, and Severe): 0, 1, 2, 3, and 4. Several studies [\[8,](#page-29-7)[15\]](#page-29-14) used artificial intelligence approaches for the identification of KOA. However, no study has been found that identifies the subtypes of KOA based on the X-rays of the KL severity grading system. Four baseline classifiers, including Vgg-19, Dens-Net 169, Xception, and Inception-V3, were also compared to KOC\_Net. The primary contributions of this study are given below:

- 1. The novel KOC\_Net model is developed to classify the five different types of KOA, i.e., Healthy, Doubtful, Minimal, Moderate, and Severe using X-rays of the KL severity grading system. Additionally, the KOC\_Net extracts the dominant features from the X-rays of KOA which makes the model significant in classifying the KOA based on knee severity.
- 2. The proposed KOC\_Net model reduces the complexity of the model by limiting the number of trainable parameters.
- 3. For this work, the SMOTE Tomek method is used to resolve the problem of the imbalance number of KOA images.
- 4. The proposed model also highlights the part of the knee affected by KOA using Grad-CAM heat-map methodology.
- 5. The performance of the KOC\_Net model was compared with four baseline classifiers such as Vgg-19, DenseNet 169, Xception, and Inception-V3. The proposed model achieves the highest classification accuracy of 96.51% which is superior to the other four baseline models.
- 6. In addition, the outcomes of the KOC\_Net model surpassed modern state-of-theart classifiers.

This study is broken down into the following sections: The literature review is presented in Section [2.](#page-2-0) In Section [3,](#page-5-0) we discuss the dataset description, SMOTE Tomek, proposed model, and performance evaluation metrics. The results obtained by using the proposed model and four baseline models are comprehensively discussed in Section [4.](#page-14-0) The conclusion and future work of the study is presented in Section [5.](#page-28-0)

#### <span id="page-2-0"></span>**2. Related Work**

The goal of the significant study on KOA diagnosis help doctors in the early identification of the disease [\[21,](#page-30-4)[22\]](#page-30-5). Meanwhile, current research is focused on improving the diagnosis procedure for multiple stages of KOA through the use of intelligent algorithms [\[23,](#page-30-6)[24\]](#page-30-7). Table [1](#page-5-1) provides an overview of the recent literature on KOA diagnosis using DL models.

Jiang et al. [\[25\]](#page-30-8) designed a CNN-based model for the classification of KOA using X-rays. They compared the classification performance of their proposed CNN model with musculoskeletal radiologists. They used data augmentation methods before training the proposed CNN model. The Osteoarthritis Initiative (OAI) dataset was used in their work, which contains a total of 40,000 images. Their proposed model achieved an F1 score and accuracy of 70.00% and 71.00%, respectively.

Thomas et al. [\[11\]](#page-29-10) proposed an ordinal regression module (ORM) with neural networks, to classify the KOA by using the KL grading system. They compared the outcomes of their proposed model with neural network approaches. The OAI dataset used included 8260 knee radiographs total, with this number being split evenly between validation, test, and training sets. It was stated that DenseNet-161 had an accuracy of 88.09% after being trained on ORM, with a Quadratic Weighted Kappa of 0.8609. Despite the positive results of their method, the model occasionally failed to correctly label KOA images with KL ratings of 0 and 1.

Overfitting has been a problem in the KOA datasets. This issue was resolved by Yong et al. [\[26\]](#page-30-9) by combining the GCN with the concept of decreasing intrinsic dimension, which was driven by the non-Euclidean structure of form space. They compared the output of the classifier to the results obtained from an additional extrinsic technique. The OAI was responsible for the construction of the dataset that was utilized, which consisted of 201 general representations. Images received a score of 0 if they did not contain any

osteophytes, 1 if they contained some osteophytes, and 2 if they contained numerous osteophytes. When contrasted with the result obtained by the Euclidean technique, which had an accuracy of 58.62%, the accuracy that was achieved using their internal model was 64.64%.

Von et al. [\[27\]](#page-30-10) developed a model with the combination of InceptionNet-v2 with SVM for the categorization of KOA. In their study, 728 knee scans in total, including images of 364 distinct patients, were taken from a Seoul hospital's database with permission from the Institutional Review Board (IRB) of the university. The outcome of this attempt was an F1 score of 0.71, along with sensitivity and accuracy values of 0.70 and 0.76. The gait characteristics that were recovered in this investigation were shown to be substantially correlated with the severity of the radiological KOA photos. The study's findings suggest that the restored features have been related to the degree of radiological KOA images.

Kwon et al. [\[28\]](#page-30-11) were able to detect knee osteoarthritis (KOA) in its early stages by analyzing the geometric anomalies found in knee X-rays and applying Hu's invariant moments to the analysis. The suggested approach started with gathering images for classification, which were subsequently classified using K-NN and decision tree models after superimposing irrelevant sections, isolating the cartilage area, and computing Hu's invariant moments. To create their dataset, two medical professionals assessed two thousand images manually using the KL grading method. All of these experts' predictions were almost exactly right—99.23% of the time.

Gornale et al. [\[29\]](#page-30-12) used ML techniques for KOA diagnosis and prognosis. Numerous specialized domains were examined, including segmentation, best practices for post-treatment planning, classification, regression analysis, and predictions. Based on the data, most diagnostic algorithms that attempted to predict KOA had an accuracy between 76.1% and 92.2%.

A technique for determining if a patient has osteoarthritis based on the joint space width (JSW) was provided by Kokkotis et al. [\[30\]](#page-30-13). They preprocessed the KOA images, selected areas of interest (ROIs), computed edges, and assessed the joint space width as part of their methodology. Two radiologists and two orthopedic surgeons collaborated to determine the extent of the damage seen in the 140 images that were taken into consideration. The suggested method achieved an accuracy rate of 97.14% and a score of 98.4% on the F1 scale, successfully classifying KOA.

Saleem et al. [\[31\]](#page-30-14), used an ML-based computer-aided design (CAD) system. Before applying a multivariate linear regression-based normalization approach, the X-ray images underwent preprocessing. The aim was to achieve maximum uniformity in the appearance of osteoarthritic and Healthy knees. First, the features are extracted using an independent component analysis. Next, they are classified using a random forest (RF) in conjunction with a Naive Bayes (NB) model. The researchers' methodology was based on 1024 distinct OAI knee X-ray images. Their method has an 82.98% accuracy rate, an 80.65% specificity rate, and an 87.15% sensitivity rate.

Roth et al. [\[17\]](#page-30-0) use a discriminative regularized autoencoder to elucidate the crucial and discriminative components that improve the detection process. To guarantee that the final model has all of the required discriminative data, the training conditions were changed to include discriminative loss. In total, 3900 knee X-rays that were taken from the OAI's open-access database were analyzed by the researchers. By contrasting their results with those of other DL approaches, they were able to demonstrate an accuracy of 82.53%. Their results are fascinating, especially considering that their technique outperformed other sophisticated DL techniques in terms of accuracy.

Nasser et al. [\[32\]](#page-30-15) used a DCNN for the identification of KOA. The Korean National Health and Nutrition Examination Survey (KNHANES) was conducted in 2015 and 2016 to gather the data for this study. The proposed method used DCNNs and scaled principal component analysis (PCA) to automatically obtain key features for assessing risk factors associated with KOA. They concluded that their classification model had an accuracy of 71.97% and a sensitivity level of 66.67%.

Brahim et al. [\[33\]](#page-30-16) used YOLOv2 for the identification of KOA using KL severity grading. The suggested approach begins by identifying knee joints in the X-rays by employing a customized YOLOv2 network. The KL system was used to grade knee images, and the results were reliably classified into severity levels. This was accomplished via fine-tuning variants of DenseNet, VGG, ResNet, and InceptionV3. With a mean Jaccard index of 0.858 and recall of 92.2%, their knee joint recognition approach performed well, but the calibrated VGG-19 [\[13\]](#page-29-12) model was only 69.7% effective in predicting the severity of knee osteoarthritis [\[34](#page-30-17)[,35\]](#page-30-18).

The procedure for obtaining LBP features from 3D images of radiographs is described in [\[36\]](#page-30-19). Through the use of deep feature extraction, Dark-net-53, and Alex-Net, 90.6% accuracy in the KOA image classification was found. In the proposed localization method, an open exchange neural network (ONNX) is combined with YOLOv2 to achieve a mean absolute precision of 0.98. These images were taken from the OAI dataset and divided in half, one for training and the other for testing.

Yunus et al. [\[37\]](#page-30-20) proposed automatic image classification for KOA. Preprocessing is the initial stage of the two-part classification process that KOA images go through. A first extraction from the VGG network concentrates on the knee joint center. Subsequently, the images are provided to the ResNet-50 network for classification. To rebalance the data, the authors employed a SMOTE method and they were able to achieve a classification accuracy of 81.41%. Wang et al. [\[38\]](#page-30-21) proposed a DL classification method based on contrast knee images from patients who underwent total knee replacement. The KL-based grading categories were divided using a cross-validation method trained on ResNet34. 4796 OAI X-rays in total were included in the dataset utilized for this investigation. Their suggested model's accuracy was 72.7%. Given the tiny size of their dataset and their use of transfer learning, it is plausible that their model's performance was not as good.

Leung et al. [\[39\]](#page-30-22) proposed a hybrid model that combines elements of a deep and traditional model to increase the accuracy of early KOA detection. The traditional model made use of logistic regression, ANNs, and RF. The deep learning model used CNNs to classify KOA images. The subjects for the OAI dataset comprised 3285 individuals without KOA and 1389 individuals with KOA. Their proposed hybrid model yielded an AUC of 0.807, sensitivities of 72.3%, and specificities of 80.9%.

Gaun et al. [\[40\]](#page-30-23) proposed a CNN model for the classification of KOA using the KL grading system. They achieve remarkable results by employing a deep Siamese CNN. After using data from the multicenter osteoarthritis research to train their model, they used 5960 OAI knee images for validation to ensure their work was accurate. Their model's overall classification accuracy was 66.71%, and in the quadratic range, its Kappa value was 0.83. Furthermore, they focus on emphasizing the significant visual elements related to the proposed model's conclusion. The study [\[41\]](#page-30-24) used ML methods to identify the fundamental features of KOA. The researchers used a combination of distance-weighted discrimination and k-means clustering to identify patterns of similarity among patient phenotypes. The dataset was obtained by researchers at the National Institutes of Health from the Osteoarthritis Biomarkers Consortium Foundation. The collected dataset contains 600 patients with 76 distinct variables. The difference between those who had improved and those who had not across all assessments was indicated by a z-score of 10.1.

A feature extraction method was devised by Nelson et al. [\[42\]](#page-30-25) to help radiologists diagnose KOA. Furthermore, a method based on ML was introduced to identify KOA automatically from the gathered data. They used the SVM and KNN algorithms to categorize knee X-rays. Based on the OAI data, knee radiographs were categorized as KOA-progressors or non-progressors. By using the SVM technique, they were able to achieve a classification accuracy of 74.07%.



<span id="page-5-1"></span>**Table 1.** Recent studies that use artificial intelligence (AI) models for the classification of KOA using different medical images.

Several limitations have been observed in the majority of recent research studies [\[43–](#page-31-0)[46,](#page-31-3)[49,](#page-31-6)[54,](#page-31-11)[55\]](#page-31-12); (1) no data preprocessing techniques were applied; (2) the images in KOA datasets contain low contrast. No image enhancement method was used by prior studies; thus, it might affect the performance of the model; (3) imbalance classes; and (4) no study works on the KOA classification based on the knee severity grading. Therefore, this study fulfills this gap by addressing these aforementioned problems.

#### <span id="page-5-0"></span>**3. Materials and Methods**

This section presents a comprehensive description of the datasets, image enhancement, data generative methods, and the proposed KOC\_Net model. KOA, the main cause of which is the increase in articular cartilage degeneration, often appears in old age [\[47](#page-31-4)[–49\]](#page-31-6). To detect the KOA, the researchers use an X-ray image widely. Applying DL algorithms to improve the diagnostic accuracy of the grading of KOA in each of the 0–4 categories: Minimal, Doubtful, Moderate, Severe, and Healthy [\[13,](#page-29-12)[56,](#page-31-13)[57\]](#page-31-14). Moreover, early diagnosis of KOA provides doctors with a greater chance to prevent the progression of the disease and to initiate treatment [\[58\]](#page-31-15). Advances in technology related to image processing and AI have greatly involved the medical domain such as skin cancer [\[59\]](#page-31-16), genetic disorders [\[60\]](#page-31-17), lung cancer [\[61\]](#page-31-18), etc. Smart automated systems depend largely on the research community for their improvements to ensure the evaluation process is even quicker and with even more accuracy. We have designed a novel KOC\_Net model in this study, which aims to identify five different types of KOA using KOA Grading images. The KOC\_Net model is trained and tested on two publicly available KOA datasets. The KOA images are resized to 150  $\times$  150 pixels before training the proposed model. After this, we improved the contrast of the KOA images by applying the Contrast-Limited Adaptive histogram equalization (CLAHE) technique. The Synthetic Minority Over-Sampling Technique (SMOTE) Tomek method was adopted to resolve the unbalanced dataset problem and keep the size of samples in each class balanced [\[62,](#page-31-19)[63\]](#page-31-20). The KOC\_Net model and four baseline classifiers such as Vgg-19 [\[64\]](#page-31-21), DenseNet 169 [\[65\]](#page-31-22), Xception [\[14\]](#page-29-13), and Inception-V3 were executed up to 30 epochs. The Grad-CAM heat-map technique has been applied to visualize the discriminating properties of KOA and to highlight the input features that affect the classification of KOA. These features were employed to highlight the determinants of KOA diagnosis. Figure [1](#page-6-0) depicts the workflow of the proposed KOC\_Net model.

<span id="page-6-0"></span>



**Figure 1.** Proposed study framework for the identification of KOA using KL grading system. **Figure 1.** Proposed study framework for the identification of KOA using KL grading system.

## *3.1. Description of Datasets 3.1. Description of Datasets*

For this study, two publicly available benchmark datasets such as KOA datasets with For this study, two publicly available benchmark datasets such as KOA datasets with severity grading [\[14\]](#page-29-13) and Digital Knee X-ray Images [\[66\]](#page-31-23) are used. Two medical experts severity grading [14] and Digital Knee X-ray Images [66] are used. Two medical experts discuss each radiographic knee X-ray using the KL grading system. Based on KL grading, discuss each radiographic knee X-ray using the KL grading system. Based on KL grading, the dataset is divided into five different grades such as Grade 0 (Healthy), Grade 1 (Doubt-the dataset is divided into five different grades such as Grade 0 (Healthy), Grade 1 (Doubtful), Grade 2 (Minimal), Grade 3 (Moderate), and Grade 4 (Severe). The dataset-1 [14] contains a total of 1629 KOA images including 693 images of Grade 0, 296 images of Grade 1, 447 images of Grade 2, 223 images of Grade 3, and 51 images of Grade 4. The dataset-2 [\[66\]](#page-31-23) contains a total of 1650 of which 514 images are of Grade 0, 477 images of Grade 1, 232 images of Grade 2, 221 images of Grade 3, and 206 images of Grade 4. A detailed description of the KOA dataset is presented in Table 2. Additi[ona](#page-7-0)lly, Figure 2 presents a few original samples of KOA.

<span id="page-6-1"></span>

Figure 2. Image Samples of KOA; (a) KOA images with marked abnormalities, while, (b) show raw samples of KOA. samples of KOA.



<span id="page-7-0"></span>**Table 2.** A detailed summary of the KOA dataset.

### *3.2. KOA Image Data Preprocessing 3.2. KOA Image Data Preprocessing*

<span id="page-7-1"></span>As discussed in the above section, this study uses two KOA datasets. The KOA images of the datasets are further separated into five different grades. For better training of the proposed model, several data-preprocessing methods are used to enhance the KOA dataset. The steps for conducting data processing are depicted i[n F](#page-7-1)igure 3.



**Figure 3.** Steps of conducting pre-processing to enhance the KOA dataset. **Figure 3.** Steps of conducting pre-processing to enhance the KOA dataset.

The dataset is symbolized as  $X_1$ , each KOA image is symbolized as  $x_1(v) \in X_1$ ,  $v = 1, 2, \dots |X| = 6400$ . We have  $X_1 = [x_1(1), x_1(2), \dots, x_1(v), \dots, x_1(|X|)]$ . The size of each KOA image is  $[X_1(v)] = W_1 \times H_1 \times C_1$ . Here,  $W_1 = H_1 = 512$ ,  $C_1 = 3$ . The raw KOA images are not appropriate for training CNN due to several issues, including (i) having duplicate data in three color channels, (ii) uneven contrast, (iii) including background and duplicate data in three color channels, (ii) uneven contrast, (iii) including background and text information, and (iv) high-resolution KOA images. The first step  $X_1$  was to transform the color images into grayscale as shown in Equation (1). the color images into grayscale as shown in Equation (1).

$$
X_2 = G(X_1) = \{x_2(1), x_2(2), \dots, x_2(v), \dots, x_2(|X|)\}\
$$
 (1)

where *G* means the grayscale operation. After converting the images into grayscale images, the dataset becomes  $[X_2(v)] = W_2 \times H_2 \times C_2$  which represents the  $W_2 = H_2 = 512$ ,  $C_2 = 3$ . Now, the contrast-limited adaptive histogram equalization (CLAHE) method was used to method was used to enhance the contrast of KOA images. CLAHE is used to enhance the enhance the contrast of KOA images. CLAHE is used to enhance the contrast of digital images. For *v*th image  $X_3(v)$ ,  $v = 1, 2, \dots, |X|$ , we first calculate their minimum grayscale mages. For earling  $\mathcal{L}_{12}$  (e)  $\mathcal{L}_{23}$  (e)  $\mathcal{L}_{33}$  (e)  $\mathcal{L}_{34}$  (see the maximum grayscale value  $\mathcal{L}_{34}$  (z) by using Equations (2) and (3) value  $\chi_{min}(v)$  and maximum grayscale value  $\chi_{max}(v)$  by using Equations (2) and (3).

$$
\chi_{min}(v) = min_{a=1}^{W1} \times max_{b=1}^{W1} \times x_2(v|a, b)
$$
 (2)

$$
\chi_{max}(v) = min_{a=1}^{W1} \times max_{b=1}^{W1} \times x_2(v|a, b)
$$
\n(3)

Here, (*a*, *b*) means the coordinates of the pixel of the image. The new CLAHE image Here, (*a*, *b*) means the coordinates of the pixel of the image. The new CLAHE image  $X_3(v)$  is obtained by using Equation (4).

 $\mathcal{L} = \sum_{i=1}^n \mathcal{L}_i$ 

$$
x_3(v) = \frac{x_2(v) - \chi_{min}(v)}{\chi_{max}(v) - \chi_{min}(v)}
$$
(4)

 $\mathcal{L}(\mathcal{L}^{\mathcal{L}})$  (see Fig. ). The set of the set o

In all, we obtain the CLAHE image set  $X_3 = \text{CHALE}(H_2) = \{x_3(1), x_3(2), \ldots, x_3(v), \ldots, x_3(|X|)\}\$ . The image produced by using CLAHE is graphically represented in Figure [4.](#page-8-0)

<span id="page-8-0"></span>

**Figure 4.** After applying CLAHE on KOA images. **Figure 4.** After applying CLAHE on KOA images.

Third, we cropped the KOA images to remove the text at the margin areas and reduce Third, we cropped the KOA images to remove the text at the margin areas and reduce the size of the KOA images. Thus, we obtain the cropped dataset  $(X_4)$  by using Equation (5).

$$
X_4 = C(X_3[h_r, h_m, h_j, h_k] = \{x_4(1), x_4(2), \dots, x_4(v), \dots, x_4(|X|)\}
$$
(5)

where C represents crop operation. Parameter  $(h_r, h_m, h_j, h_k)$  means the crop values in units of pixels from the top, bottom, left, and right. We set  $h_r = h_m = h_j = h_k = 256$ . Now the size of each image size  $[x_4(v)] = W_4 \times H_4 \times C_4$ . We can have  $W_4 = H_4 = 256$  and  $C_4 = 1$ . Fourth, we down-sampled each image to the size of  $[W_5, H_5]$ , and now obtain the resized image set  $(X_5)$  as mentioned in Equation (6).

$$
X_5 = \Downarrow (X_5[W_5, H_5]) = \{x_5(1), x_5(2), \dots, x_5(v), \dots x_5(|X|)\}
$$
(6)

The  $X_5$  represents the down-sampling (DS), where  $b$  is the down-sampled version of the original image *a*, and denotes this fact  $\Downarrow$ :  $a \rightarrow b$  original image. In this study,  $W_5 = H_5 = 150$  and  $C_5 = 1$ . There are two aspects to DS's benefit: (i) it can reduce storage needs and (ii) it avoids overfitting with a smaller dataset as demonstrated in Table [3.](#page-8-1) The reason why we set  $W_5 = H_5 = 150$  is based on the trial-and-error method. We found that larger size will bring in overfitting which impairs the performance, and meanwhile, the smaller size will make the images blurry which also decreases the classifier's performance.

<span id="page-8-1"></span>Table 3. Image storage and size per preprocessing step.



We compare the size and storage of each KOA image  $x_s(v)$ ,  $s = 1, \dots, 5, v = 1, \dots$ , |*X*| at every preprocessing step. Here, following the preprocessing step, we can observe that the storage or size requirements for each image have been reduced to approximately 2.08%. Visual representations of the final state's compression ratios (CRs)  $X_5$  to original stage *X*<sub>1</sub> were calculated as *CR*  $_{\text{Stronge}}(v) = \text{byte}[x_5(v)] / \text{byte}[x_1(v)] = 62,011/10,456,121,$ and *CR*  $_{Size}(v) = size[x_5(v)]/size[x_1(v)] = 31,256/2,034,617$ . Hence, we can obtain  $CR_{Size}(v) = CR_{Size}(v) = 2.083\%, \forall v = 1, 2, \ldots, |X|.$ 

### *3.3. Implementation of SMOTE Tomek*

From Table [2,](#page-7-0) it has been observed that the KOA dataset has an uneven distribution of knee images in each class. The imbalance number of knee images affects the performance of the model. Therefore, the SMOTE Tomek [\[67\]](#page-31-24) method is used to synthetically balance the knee images in each class of the KOA dataset. SMOTE is the technique for oversampling which balances class distribution in a KOA dataset. Tomek links are selected pairs of instances from the same class and in SMOTE new instances may be created at random [\[68\]](#page-31-25). Therefore, this study combines SMOTE and Tomek to lower the chance of overlap. The pseudocode of SMOTE Tomek is outlined in Algorithm 1.

**Algorithm 1**: Balancing knee images of the KOA dataset using the SMOTE Tomek algorithm

**Input:**  $S =$  Set for training,  $M =$  instances of minority set,  $U \& q =$  No of nearest neighbors, *C* = The number of synthetic examples required to compensate for the number of original KOA images in the specified class. **Output:** A group of synthetic samples from the minority: *O*′ 1.  $ST = \Phi$  //*ST* is a collection of samples that are considered as Smote Tomek 2. for all *O<sup>i</sup>* in *O* do 3.  $N_{oi} \leftarrow k$  nearest neighbors of  $O_i$  in *S* 4. *n* ← The number of samples in *N*<sub>*oi*</sub> and not in O<br>5. if  $k/2 \le n < k$  then //*o<sub>i</sub>* is a borderlin if  $k/2 \leq n < k$  then  $// o_i$  is a borderline sample 6. add *o<sup>i</sup> to ST* 7. end if 8. end for 9.  $Q' = \Phi$  $110'$  is a set containing synthetic samples 10. for all  $st'$  *i* in *ST* do 11. *N*<sub>sti</sub> $\leftarrow$  *q* nearest neighbors of *st i* in *O* 12. *for i* = 1 *to* C do 13.  $o \leftarrow \text{choose a random sample from } N_{sti}$ <br>14.  $st' : \leftarrow st' : + i * (st' : - o)$  //*i* is a 14.  $st'_{i} \leftarrow st'_{i} + j * (st'_{i})$ *i* − *o* //*j* is a random number in (0, 1), *st' i* is a synthetic sample 15. add  $st'$ <sub>*i*</sub> to  $O'$ 16. end for 17. end for 18.  $O' = O U O'$  $110'$  is the union of minority samples and synthetic samples 19. return *O*′

Figure [5](#page-10-0) presents the synthetic images generated by the SMOTE Tomek up-sampling method. Additionally, the detailed description of the KOA dataset after using SMOTE Tomek and pre-processing methods such as  $X_1$  to  $X_5$  are presented in Table [4.](#page-10-1)

<span id="page-10-0"></span>

**Figure 5.** Synthetic image sample of KOA dataset after using SMOTE Tomek. **Figure 5.** Synthetic image sample of KOA dataset after using SMOTE Tomek.

<span id="page-10-1"></span>**Table 4.** Summary of the enhanced KOA dataset after applying the up-sampling method of  $\Omega$  discrete computer computer vision, and face detection, and face detection, and face detection are computed vision are computed vision are computed vision are computed vision of  $\Omega$ SMOTE Tomek.

No. of	Class Name	No. of Images <b>After SMOTE</b>	Data Splitting			
<b>Classes</b>			Training $(70\%)$	Validation (20%)	Testing $(10\%)$	
$\theta$	Healthy	2520	1764	504	252	
	Doubtful	2314	1621	462	231	
2	Minimal	2900	2030	580	290	
3	Moderate	2372	1661	474	237	
4	Severe	2565	1797	512	256	
Total		12,671	8873	2532	1266	

### *3.4. Proposed KOC\_Net Model*

Disease classification, image segmentation, and face detection are computer vision applications that benefit greatly from the CNN architecture, which incorporates the anatomy of the human brain as its primary source of inspiration. Translation invariance, also referred to as geographical invariance [\[67](#page-31-24)[–70\]](#page-32-0), signifies the ability of a CNN to recognize the identical feature in multiple images independently of its visual location. For this study, we designed a novel KOC\_Net model based on CNN for the classification of KOA using KL severity grading X-rays. The architecture of the KOC\_Net is illustrated in Figure [6,](#page-11-0) which includes five convolutional (ConvL) blocks, one dropout layer, two dense layers, and a SoftMax classification layer.



**Figure 6.** Proposed KOC\_Net architecture for KOA classification. **Figure 6.** Proposed KOC\_Net architecture for KOA classification.

#### 3.4.1. Convolutional Blocks of KOC\_Net

<span id="page-11-0"></span>and a Software control of Max classification layer.

3.4.1. Convolutional Blocks of KOC\_Net The ConvL block of the proposed KOC\_Net model contains a convolutional2D (ConvL\_2D) and a pooling2D (Pool\_2D). To allocate weights to the various kernel layers, the LecunUniformV2 kernel initializer is designed. Through the utilization of the activation function of ReLU, we prevent the model from the issue of gradient-vanishing.<br>Lecture is defined in the activa-lecture of the activa-lecture of the internal state of the state of the state of the state of the st the knee X-ray images. This layer, sometimes called the kernel, initiates the process by the knee X-ray images. This layer, sometimes called the kernel, initiates the process by activating filters. The filter size of the proposed KOC\_Net model is demonstrated in knee X-ray images. The kernel, in initiate the kernel, in initiate the process by action (7). In KOC\_Net, the initial ConvL\_2D layers apply the filter to extract the information from

$$
F_{Filter\_size} = f_x \times f_y \tag{7}
$$

\_ = × (7) Suppose, *I* is the input image, *FFilter*\_*size* is the kernel size, and *O* is the output feature map. where  $f_x$  and  $f_y$  represent the filter width and height, respectively. For this study, we used the filter size of  $3 \times 3$ . Equation (8) presents the ConvL\_2D operation of the KOC\_Net.

$$
O(x, y) = \sum a \sum b \times I(x + a, y + b) \times F_{Filter\_size}(a, b)
$$
\n(8)

used the filter size of 3 × 3. Equation (8) presents the ConvL\_2D operation of the KOC\_Net. where  $O(x,y)$  is the value at position  $(x,y)$  in the output feature map,  $I(x + a, y + b)$  is the value at position  $(x + a, y + b)$  in the input image.  $F(x + a, y + b)$  is the value at position (*a*,*b*) in the kernel. An output feature map was produced through the use of a ConvL\_2D. Equation (9) for the ConvLs reveals the input feature maps are combined to produce each<br>output feature map value at position  $(x + a, y + b)$  in the input image.  $F_{Filter\_size}(a, b)$  is the value at position output feature map.

$$
X\frac{v}{k} = I\left[\sum_{i \in Mb} X\frac{v-1}{k} * R\frac{v}{ij} + M\frac{v}{k}\right]
$$
(9)

where,  $X^v_k$  is the output of the present layer,  $(Xv - 1) \times (k - 1)$  is the previous layer's  $\sum_{i=1}^{\infty}$  for the Cancil and  $\sum_{i=1}^{\infty}$  for the input  $\sum_{i=1}^{\infty}$  are are called to processed by a PoLU function a collection of input maps. After that, the ConvL results are processed by a ReLU function.<br>. output,  $R^{\frac{v}{l}}_{ij}$  is the current layer's kernel,  $M^v_{\bar{k}}$  are the current layer's biases, and  $M$  represents

#### 3.4.2. Flatten Layer

∶ r atten Eayer<br>The utilization of the flatten layer (*FTL*) allowed for the transformation of the 2D visual representation into a 1D input as presented in Equation (10). The image produced by using<br>FTL is graphically represented in Figure 7 *FTL* is graphically represented in Figure [7.](#page-12-0)

$$
FTL_{2D} = T_{1D} \tag{10}
$$

where *T* represents the input tensor. This reshaping essentially flattens the spatial dimensions of the input tensor, transforming it into a vector that fed into a fully connected layer (FCL) for the final stages of a KOC\_Net to classify the knee image into their respective classes.

<span id="page-12-0"></span>

**Figure 7.** Structure of the flatten layer for KOC\_Net. **Figure 7.** Structure of the flatten layer for KOC\_Net.

#### 3.4.3. Dropout Layer of KOC\_Net Model 3.4.3. Dropout Layer of KOC\_Net Model

For this study, the incorporation of the dropout layer into the KOC\_Net model to For this study, the incorporation of the dropout layer into the KOC\_Net model to lessen the possibility of overfitting [\[71\]](#page-32-1). The dropout value of 0.5 is used for the KOC\_Net model. This layer aimed to alleviate training time constraints and model complexity. Equation (11) is used for employing the dropout process in the proposed model.

$$
Y = \text{Dropout}(X) \tag{11}
$$

Here, *Y* is the output of the dropout layer. Each element of *Y* is computed by using Equation (12). Equation (12).

$$
Yi = \frac{X_i}{1 - p} \tag{12}
$$

where  $X_i$  is the corresponding element in the input  $X$ , and  $p$  is the dropout probability. During training, each neuron's output is set to zero with probability *p* and scaled by (1 − During training, each neuron's output is set to zero with probability *p* and scaled by (1 − *p*) to account for the dropped-out neurons. During inference, the dropout layer is deactivated, and the output is scaled by  $1 - p$  to ensure that the expected output remains the same.

# 3.4.4. Dense Block of the KOC\_Net

The proposed KOC\_Net model contains two dense blocks, with an activation function comprising each block. The detailed description of these blocks is stated below:

 $t_{\text{t}}$  and the detailed description of the description of the description of these blocks is stated below: **ReLU Function** 

The ReLU activation function determines the movement of KOC\_Net output from one the relation function function function determines the movement of the movemen battering with a value of EUC and feaves positive values anothings at the introduces field<br>linearity to the network, allowing it to learn complex patterns and relationships in the KOC tive outcome with a value of zero and leaves positive values unchanged. It introduces non-image data during the training process of the KOC\_Net. The following Equation (12) is  $\frac{1}{2}$  and to perform the ReLU operations. layer to another. ReLU activation is achieved through the substitution of every negative

$$
ReLU(x) = max(0, x)
$$
\n(13)

• Dense Layer

The dense layer generates output that is consistent with the characteristics of the input matrix, which is a singular matrix. This output is produced by the dense layer. The final output of the KOC\_Net model is generated by a dense layer comprising five neurons, which employs the SoftMax activation function [\[11\]](#page-29-10). SoftMax is an activation function that operates based on probability, where the quantity of neurons is equivalent to the total number of classes. The 1,150,037 parameters make up the total amount of parameters, with 1,150,037 of them being trainable and zero of them being non-trainable.

#### *3.5. Model Evaluations*

The confusion matrix is generated for evaluating the performance of the proposed KOC. Net model and other baseline models. The initial phase in the process of training the proposed model and baseline models consisted of dividing the dataset into two distinct sets: a training set and a test set [\[72](#page-32-2)[,73\]](#page-32-3). Using the test set, the performance of the model was evaluated in terms of several parameters such as accuracy (ACC), precision (PRE), recall (REC), and F1-Score. Equations (14)–(17) are used to measure these parameters.

#### 3.5.1. Accuracy (ACC)

The ACC is used to calculate the proportion of correct prediction of the KOA made by the KOC\_Net model. Equation (14) is used to calculate the ACC.

$$
ACC = \frac{TP + TN}{TP + FN + FP + TN}
$$
\n(14)

#### 3.5.2. Precision (PRE)

The PRE is used to evaluate the accuracy of positive prediction carried out by the proposed KOC\_Net and other baseline models. Equation (15) is used to measure the PRE.

$$
PRE = \frac{\text{TP}}{\text{TP} + \text{FP}}
$$
 (15)

3.5.3. Recall (REC)

REC is TPR, which measures the ability of a KOC\_Net model and baseline models used in this work to identify all relevant positive instances. Equation (16) is applied to calculate the REC.

$$
REC = \frac{TP}{TP + FN}
$$
 (16)

#### 3.5.4. F1-Score

The harmonic mean of REC and PRE is called F1-Score. The following Equation (17) is used to measure the F1-Score.

$$
F1-score = 2 \times \frac{PRE \times REC}{PRE \times REC}
$$
 (17)

#### *3.6. Proposed Algorithm*

Algorithm 2 presents the pseudocode of the proposed KOC\_Net model. Algorithm 2 consists of input, output, and five sections such as  $[H_1, H_2, H_3, H_4, H_5]$ .  $H_1$  demonstrates the pre-processing of knee X-rays. The steps for synthetically balancing the size of the KOA dataset are presented in  $H_2$ . The structure of the proposed KOC\_Net model is discussed in *H*3. The training and validation of the proposed KOC\_Net on the enhanced dataset are described in  $H_4$ . The last section  $H_5$  computes the performance of the model.



#### <span id="page-14-0"></span>**4. Experimental Results and Discussions**

This section presents the experimental results obtained by using the KOC\_Net model. Additionally, the results of the proposed KOC\_Net are also compared with baseline models.

#### *4.1. Experimental Setup and Hyperparameters*

Tensor flow (TF) and Keras library were used to implement the proposed KOC\_Net model and other baseline models used in this work. Additionally, the Python programming language is used to implement the operations that are not linked with CNN. The proposed KOC\_Net model and baseline models are executed up to 30 epochs with a batch size of 16. The momentum and learning rate of the KOC\_Net is 0.9 and 0.0001, respectively. The experiment is performed on a Windows 10 operating system having 32 GB of RAM and an 11 GB NVIDIA GPU.

#### *4.2. Results Analysis*

This section presents the detailed results of the KOC\_Net and other baseline models in terms of many performance evaluation metrics.

#### 4.2.1. Results of KOC\_Net Model in Terms of Accuracy

After enhancing the dataset by using SMOTE Tomek, we compared the proposed KOC\_Net model and baseline models such as Vgg-19, XceptionNet, DenseNet-169, and Inception-V3. We also observed the outcomes obtained by using the proposed KOC\_Net model without applying SMOTE Tomek. Table [5](#page-15-0) presents the detailed results obtained

by using the KOC\_Net model with and without using SMOTE Tomek, and the other four baseline models.

<span id="page-15-0"></span>**Table 5.** Results obtained by the proposed model and other baseline models in terms of many performance metrics.

<b>Classifiers</b>	<b>ACC</b>	<b>PRE</b>	<b>REC</b>	F <sub>1</sub> -Score	<b>AUC</b>
$Vgg-19$	81.08%	88.91%	$82.66\%$	81.46%	84.24%
DenseNet-169	84.97%	89.17%	89.93%	88.73%	85.21%
Xception	87.06%	88.73%	85.41%	81.11%	85.58%
Inception-V3	83.62%	89.60%	81.96%	83.37%	80.53%
KOC Net without SMOTE Tomek)	79.89%	77.85%	79.47%	72.28%	77.99%
<b>KOC Net with SMOTE Tomek</b>	$96.51\%$	90.25%	91.95%	96.70%	95.71%

From Table [5,](#page-15-0) it has been observed that the proposed KOC\_Net model with SMOTE Tomek achieved the highest classification accuracy of 96.51% as compared to other baseline approaches. The Vgg-19 achieved a classification ACC of 81.08%, PRE of 88.91%, REC of 89.93%, F1-Score of 81.46%, and AUC of 84.24%. The DenseNet-169 model attained an ACC of 84.97%, PRE of 89.17%, REC of 82.66%, and F1-Score of 88.73%. The XceptionNet model achieved an ACC of 87.06%, PRE of 88.73%, REC of 85.41%, AUC of 85.58%, and F1-Score of 81.11%. Additionally, the Inception-V3 attained an ACC of 83.62%, PRE of 89.60%, REC 81.96%, and F1-Score of 83.37%. The proposed KOC\_Net model without SMOTE Tomek achieved the outcomes of 79.89% ACC, 77.85% PRE, 79.47% REC, 72.28% F1-Score, and 77.99% AUC. However, the proposed KOC\_Net model with SMOTE Tomek attained the highest results of 96.51% ACC, 90.25% PRE, 91.95% REC, 96.70% F1-Score, and 95.71% AUC. Figure [8](#page-16-0) shows the graphical representation of the proposed model with and without SMOTE Tomek, and other baseline models.



**Figure 8.** *Cont*.

<span id="page-16-0"></span>

Figure 8. Representation of results in terms of accuracy; (a) Vgg-19, (b) XceptionNet, (c) DenseNet-169, (**d**) Inception-V3, (**e**) KOC\_Net model without SMOTE Tomek, and (**f**) KOC\_Net model with 169, (**d**) Inception-V3, (**e**) KOC\_Net model without SMOTE Tomek, and (**f**) KOC\_Net model with SMOTE Tomek. SMOTE Tomek.

## 4.2.2. Results of the KOC\_Net Model in Terms of AUC 4.2.2. Results of the KOC\_Net Model in Terms of AUC

For this study, the AUC is used to measure the ability of the model to distinguish For this study, the AUC is used to measure the ability of the model to distinguish between the KOA classes. The high value of AUC shows that the model is performing between the KOA classes. The high value of AUC shows that the model is performing significantly while distinguishing the positive and negative classes. Thus, to determine significantly while distinguishing the positive and negative classes. Thus, to determine the efficacy of the proposed KOC\_Net model, a comparison has been performed. The Vgg-19, XceptionNet, DenseNet-169, and Inception-V3 attain the AUC of 84.24%, 85.21%, 85.58%, and 80.53%, respectively. The proposed KOC\_Net model without SMOTE Tomek achieves the AUCH of 77.99%. The highest AUC of 95.71% was achieved by the proposed KOC\_Net with SMOTE Tomek. The results reveal that the proposed KOC\_Net model with SMOTE Tomek performs better than other approaches discussed in this study. The detailed results of the AUC of these models are presented in Figure [9.](#page-17-0)

<span id="page-17-0"></span>

Figure 9. Representation of results in terms of AUC; (a) Vgg-19, (b) XceptionNet, (c) DenseNet-(**d**) Inception-V3, (**e**) KOC\_Net model without SMOTE Tomek, and (**f**) KOC\_Net model with 169, (**d**) Inception-V3, (**e**) KOC\_Net model without SMOTE Tomek, and (**f**) KOC\_Net model with SMOTE Tomek. SMOTE Tomek.

## 4.2.3. Results of the KOC\_Net Model in Terms of Precision 4.2.3. Results of the KOC\_Net Model in Terms of Precision

The parameter precision is used to calculate positive predictions made by the model. The higher the value of precision shows that the model makes fewer false positive predic-tions. Figure [10](#page-18-0) shows the graphical representation of the precision value obtained by the tions. proposed KOC\_Net model and other baseline models. The results show that Vgg-19 attains a precision of 88.91%. The DenseNet-169 and XceptionNet achieved a precision of 89.17% and 88.73%, respectively. The inception-V3 attains 89.60% precision. Additionally, the result obtained by the KOC\_Net model without SMOTE Tomek is 77.85%. The higher precision value of 90.25% was attained by the proposed KOC\_Net model with SMOTE Tomek.

<span id="page-18-0"></span>

Figure 10. Representation of results in terms of precision; (a) Vgg-19, (b) XceptionNet, (c) DenseNet-169, (**d**) Inception-V3, (**e**) Proposed KOC\_Net model without SMOTE Tomek, and<br>(f) Proposed KOC\_Net model with SMOTE Tomek. (f) Proposed KOC\_Net model with SMOTE Tomek.

## 4.2.4. Results of the KOC\_Net Model in Terms of Recall 4.2.4. Results of the KOC\_Net Model in Terms of Recall

The metric recall is used to measure the correct identification of true positives from all  $\overline{a}$ the actual positive knee image samples of the KOA dataset. Figure [11](#page-19-0) illustrates the recall curve data that were employed in the process of evaluating the proposed KOC\_Net model in comparison to Vgg-19, Inception-V3, XceptionNet, and DenseNet-169. The proposed KOC\_Net model without SMOTE achieves a recall of 79.47%. The Vgg-19, DenseNet-169, XceptionNet, and Inception-V3 attains the recall of 82.66%, 89.93%, 85.41%, and 81.96%, respectively. The highest recall of 91.95% was attained by the proposed KOC\_Net model with SMOTE Tomek.

<span id="page-19-0"></span>

Figure 11. Outcomes of recall; (a) Vgg-19, (b) XceptionNet, (c) DenseNet-169, (d) Inception-V3, (e) Proposed KOC\_Net model without SMOTE Tomek, and (**f**) Proposed KOC\_Net model with SMOTE Tomek.

4.2.5. Results of the KOC\_Net Model in Terms of F1-Score

The metric F1-Score is used to measure the harmonic means of precision and recall. The high F1-Score represents that the model performs significantly in classifying five classes of KOA. The highest F1-Score of 96.70% was achieved by the proposed KOC\_Net model with SMOTE Tomek. The other models Vgg-19, DenseNet-169, XceptionNet, and Inception-V3 attains the F1-Score of 81.46%, 88.73%, 81.11%, and 83.37%, respectively. The lowest 72.28% F1-Score was achieved by the KOC\_Net model without SMOTE Tomek. The results obtained by these models in terms of F1-Score are depicted in Figure [12.](#page-20-0)

<span id="page-20-0"></span>

12. Composed models; (c) DenseNet-169, (d) Inception-V3, (e) KOC\_Net model without SMOTE Tomek, and (f) KOC\_Net model with SMOTE Tomek. Figure 12. Comparison of the F1-Score of the proposed model with baseline models; (a) Vgg-

#### 4.2.6. Results of the KOC\_Net Model in Terms of Loss

The loss function represents the numerical difference between the actual and prethe loss. The Vgg-19, DenseNet-169, XceptionNet, and Inception-V3, produced the loss values of 0.6321%, 0.6501%, 0.6155%, and 0.8537%, respectively. The proposed  $\text{KOC\_Net}$ model with SMOTE Tomek produces a loss of 0.5885%. The graphical representation of the loss curve obtained by these models is presented in Figure [13.](#page-21-0) dicted values. The categorial cross-entropy loss function is used in this study to calculate



**Figure 13.** *Cont.*

<span id="page-21-0"></span>

Figure 13. Loss of proposed and baseline models; (a) Vgg-19, (b) XceptionNet, (c) DenseNet-169, (d) Inception-V3, (e) KOC\_Net model without SMOTE Tomek, and (f) KOC\_Net model with SMOTE Tomek.

## 4.2.7. Results of the KOC\_Net Model in Terms of ROC 4.2.7. Results of the KOC\_Net Model in Terms of ROC

ROC curves are graphs showing the performance of the proposed KOC\_Net model and baseline models by plotting the  $TP$  rate and  $FP$  rate. The ROC values for the proposed  $\overline{P}$ KOC\_Net with and without SMOTE Tomek were 1.00 and 0.7105, respectively. The Vgg-19, 19, DenseNet-169, XceptionNet, and Inception-V3 were 0.7587, 0.7365, 0.7423, and 0.6817, DenseNet-169, XceptionNet, and Inception-V3 were 0.7587, 0.7365, 0.7423, and 0.6817, respectively. The ROC curve in Figure [14](#page-22-0) demonstrates that the suggested KOC\_Net model performs much better than other competitive approaches used in this study. model performs much better than other competitive approaches used in this study.



is illustrated in Figure 15 through the extension of the ROC curve. As shown in Figure 15 **Figure 14.** *Cont.*

<span id="page-22-0"></span>

**Figure 14.** Representation of results in terms of ROC; (a)  $Vgg-19$ , (b) XceptionNet, (c) DenseNet-169,  $\mathbb{Z}^2$  (**e**) Proposed KOC\_Net model without SMOTE Tomek, and (**f**) Proposed KOC (**d**) Inception-V3, (**e**) Proposed KOC\_Net model without SMOTE Tomek, and (**f**) Proposed KOC\_Net model with SMOTE Tomek.

#### $\frac{1}{2}$ . 2.8.  $\frac{1}{2}$   $\frac{1$ 4.2.8. AU(ROC) for Multi-Class Evaluation Using Proposed KOC\_Net Model

A comparison between the proposed KOC\_Net model and four baseline deep models is illustrated in Figure [15](#page-23-0) through the extension of the ROC curve. As shown in Figure [15](#page-23-0) demonstrated a significant enhancement when the dataset was balanced utilizing the SMOTE Tomek method. The proposed KOC\_Net model demonstrated a significant effect on the AUC for all classes. When there is an increase in AUC, it indicates that the feature selection that was carried out by KOC\_Net has reached a high level of accuracy.

To validate our proposed KOC\_Net model, we conducted a comparison with four other models utilizing a confusion matrix. The KOC\_Net model is significantly improved through the integration of SMOTE Tomek, as depicted in Figure [16.](#page-26-0)

The proposed KOC\_Net model correctly classifies the 154 images as Healthy, 152 cases as Doubtful, 111 images as Minimal, 202 cases as Moderate, and 229 cases are Severe. Out of a total of 209 images, the XceptionNet correctly categorizes 92 images as Healthy cases, misclassifying 80 images as Doubtful, 34 images as Minimal, and 3 images as Moderate. Additionally, 172 Doubtful images out of 235 total images were correctly classified as Doubtful, while 35 were incorrectly identified as Healthy, 25 as Minimal, and 3 as Moderate. As presented in Figure [16d](#page-26-0), the proposed KOC\_Net model without SMOTE Tomek correctly classifies 5 cases as Healthy and inaccurate classifying 72 cases as Doubtful and 19 cases as Minimal. Additionally, 203 cases of Doubtful were accurately classified, and 29 and 01 cases as Minimal and Healthy, respectively were misclassified. However, the proposed KOC\_Net model without SMOTE Tomek correctly classifies the 50 cases as Moderate and 12 cases as Severe. Next, we visualize the output of the proposed KOC\_Net model with SMOTE Tomek using the Grad-CAM heatmap technique. The goal of the heatmap is to highlight the KOA area based on KL severity grading. Figure [17](#page-27-0) demonstrates the heatmap of the proposed KOC\_Net.



<span id="page-23-0"></span>selection that was carried out by KOC\_Net has reached a high level of accuracy.

**Figure 15.** Representation of results in terms of AU (ROC); (a) Vgg-19, (b) XceptionNet, (c) DenseNet-Net-169, (**d**) Inception-V3, (**e**) Proposed KOC\_Net model without SMOTE Tomek, and (**f**) Proposed 169, (**d**) Inception-V3, (**e**) Proposed KOC\_Net model without SMOTE Tomek, and (**f**) Proposed KOC\_Net model with SMOTE Tomek. KOC\_Net model with SMOTE Tomek.







**Figure 16.** *Cont*.



**Figure 16.** *Cont*.

<span id="page-26-0"></span>





**Figure 16.** Confusion Matrix; (a) Proposed KOC\_Net model with SMOTE Tomek, (b) Vgg-19, (c) XceptionNet, (d) KOC\_Net model without SMOTE Tomek, (e) Inception-V3, and (f) DenseNet-169.

<span id="page-27-0"></span>

**Figure 17.** Visualization of the infected region of KOA using GRAD-CAM. The first rows represent **Figure 17.** Visualization of the infected region of KOA using GRAD-CAM. The first rows represent  $\frac{1}{\sqrt{2}}$  the rows images and the Grade 1 to Grade 4 highlight the infected region of of KOA by using the proposed KOC\_net model. the Healthy images and the remaining rows from Grade 1 to Grade 4 highlight the infected region of KOA by using the proposed KOC\_net model.

## *4.3. Comparison of Proposed KOC\_Net Model with State-of-the-Arts 4.3. Comparison of Proposed KOC\_Net Model with State-of-the-Arts*

This section presents a comprehensive comparison of the proposed KOC\_Net model This section presents a comprehensive comparison of the proposed KOC\_Net model with recent studies  $[14,43-46,64-66]$  $[14,43-46,64-66]$  $[14,43-46,64-66]$  $[14,43-46,64-66]$  $[14,43-46,64-66]$ . The comparison of the proposed model has been formed in terms of several metrics as presented in Table 6. performed in terms of several metrics as presented in Table [6.](#page-27-1)



<span id="page-27-1"></span>**Table 6.** Performance comparison of the proposed KOC\_Net model with prior studies. **Table 6.** Performance comparison of the proposed KOC\_Net model with prior studies.

#### *4.4. Discussions*

X-ray images are commonly used in the detection and categorization of an extensive range of KOAs. Several studies [\[11,](#page-29-10)[13](#page-29-12)[,14,](#page-29-13)[33](#page-30-16)[,62,](#page-31-19)[65](#page-31-22)[,66,](#page-31-23)[74](#page-32-4)[–76\]](#page-32-5) use knee X-rays for the identification of KOA severity. Due to KOA severity grading, the diagnosis of KOA is a time-consuming process. If KOA is not diagnosed in its initial grading, a patient may face Severe complications. Therefore, this study proposed a KOC\_Net model that automatically classifies the KOA into their respective grades by using the KL grading severity system. For this work, two publicly benchmark KOA datasets were used for training the proposed KOC\_Net model. The imbalance classes of the dataset were balanced by the SMOTE Tomek method. The pseudocode of the SMOTE Tomek was presented in Algorithm 1. Several pre-processing methods were employed to enhance the KOA dataset as shown in Figure [3.](#page-7-1) The CLAHE method was also applied to increase the contrast of the image. The proposed

KOC\_Net model was trained on the enhanced dataset generated after pre-processing and the SMOTE Tomek method. The steps for executing the proposed KOC\_Net model are presented in Algorithm 2.

The performance of the proposed KOC\_Net model with and without using SMOTE Tomek was compared with four baseline models, i.e., Vgg-19, DenseNet-169, XceptionNet, and Inception-V3. The proposed KOC\_Net model with SMOTE Tomek achieved the highest classification accuracy of 96.51%, while other models, Vgg-19, DenseNet-169, XceptionNet, and Inception-V3, attained accuracy of 81.08%, 84.97%, 87.06%, and 83.62%. A detailed comparison of the proposed model and baseline model is presented in Table [5.](#page-15-0) The results of Table [5](#page-15-0) show that the proposed KOC\_Net with SMOTE Tomek is more capable of identifying the KOA and extracting dominant discriminative patterns from knee X-rays, with the highest classification accuracy of 96.51%. Additionally, the results of the four baseline models were also presented in Table [4,](#page-10-1) and we also provide a detailed description of why recent studies show less performance in classifying the KOA-based KL grading severity. The reason is that the classification performance of four baseline pre-trained model has been restricted by their final ConvL due to their deep network [\[14,](#page-29-13)[66\]](#page-31-23). The filter size in these baseline classifiers is inadequate because neurons connected to the input are so large it ignores the major elements from the KOA image. Additionally, the vanishing gradient problem occurred while training these four-baseline model due to their large number of layers. All these issues are resolved by using the KOC\_Net model with SMOTE Tomek. A simplified structure of CNN layers is introduced in the KOC\_Net model which prevents the model from gradient vanishing. Moreover, fewer training parameters are generated by the proposed KOC\_Net model which also reduces the complexity of the model.

Table [6](#page-27-1) presents the comprehensive comparison of the proposed KOC\_Net model with state-of-the-art classifiers. Cueva et al. [\[65\]](#page-31-22) designed a CNN model for the classification of KOA and they achieved the classification accuracy of 61.00%. The study [\[14\]](#page-29-13) developed a CNN model for the diagnosis of KOA. Their model achieved a classification accuracy of 95.12% in identifying the KOA of three grades. It is also observed that recall attained in this work is lower compared to the findings [\[14\]](#page-29-13). The reason for this is the study [\[14\]](#page-29-13) focused on 03 classes, while we increased the number of classes to 05. Recall measures the ability to identify positive instances, and as we expanded the number of classes, the recall value decreased in our case. Additionally, Kumar et al. [\[46\]](#page-31-3) and Touahema et al. [\[43\]](#page-31-0) designed a CNN model and achieved an accuracy of 91.03% and 94.94%, respectively. The proposed KOC\_Net model with SMOTE Tomek attains a classification accuracy of 96.51%, which is superior to state-of-the-art classifiers.

#### <span id="page-28-0"></span>**5. Conclusions and Future Work**

KOA is rated by a grading system according to the extent of joint degeneration. The KL grading scale is used to identify the stage of KOA. Therefore, this study proposed the KOC\_Net model for the classification of KOA using KL grading X-rays. For this work, each convolutional block of the KOC\_Net model contained multiple layers to classify the KOA. Several pre-processing steps such as [*X*1, *X*2, *X*3, *X*4, *X*5] were applied to enhance the KOA dataset. Moreover, the imbalance distribution of the images in the KOA dataset was resolved by using SMOTE Tomek. Grad-CAM shows a heat map of class activation to demonstrate the operation of the proposed KOC\_Net model with SMOTE Tomek. The proposed KOC\_Net model with SMOTE Tomek achieved 96.51% ACC, 96.51% REC, 96.70% F1-Score, 90.25% PRE, and 95.71% AUC. Thus, it is concluded that the proposed model with SMOTE Tomek provides great assistance to orthopedics in making diagnoses of KOA. A limitation of the study is that the KOC\_Net model is not suitable for other medical imaging such as CT, MRI, sonography, etc. Therefore, in the future, we will train and test the KOC\_Net on CT scans and MRI images. Additionally, we would also use a federated learning method to preserve patient data privacy while performing the classification of KOA.

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**Data Availability Statement:** The original contributions presented in the study are included in the article, further inquiries can be directed to the corresponding authors.

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